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**Review Article** 

# **MESOPOROUS MATERIAL, MCM- 41: A NEW DRUG CARRIER**

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## ABSTRACT

Nanotechnology is a fast-growing area, involving the fabrication and use of nano-sized materials and devices. Various nanocomposite materials play a number of important roles in modern science and technology including pharmaceutical science. Among these materials mesoporous materials covers large number of applications in drug delivery system. Mesoporous MCM-41 is one of the mesoporous materials, used now-a-days as a drug carrier. Since this kind of materials consist on a disordered network of siloxane bridges and free silanol groups, these latter could be the reacting sites against appropriate guest chemical species. In this review, the application of mesoporous MCM-41 as drug delivery system has been discuss from the host guest interaction point of view. This article reviews the fabrication and chemistry of mesoporous MCM- 41 for biomedical applications, and also the potential advantages of mesoporous MCM- 41 in drug delivery.

Key words: Mesoporous material MCM-41, Drug delivery, Chemistry, Applications.

#### INTRODUCTION

Mesoporous materials with regular geometries are generating a lot of attention owing to their great potentials in practical applications such as catalysis, adsorption, sensing, medical usage, ecology, nanotechnology <sup>1-15</sup>, Chemical and biological separations, chromatography, photonic and electronic devices, drug delivery, and energy storage<sup>16</sup>. Mesoporous materials are classified under porous material and these porous materials are classified according to their pore diameter <sup>17</sup> (table-1). Researchers had taken great efforts to synthesize mesoporous materials such as silicas <sup>18</sup>, transitional aluminas <sup>19</sup> and pillard clays. In fact, in 1990, Yanagisawa and coworkers <sup>20, 21</sup>, described the preparation of mesoporous silicas with uniform pore size. However, the pores in these materials were generally irregularly spaced and broadly distributed in size.

Types of	Diameter of	Examples
porous material	pores (nm)	
Micrporous	Diameter < 2	Zeolites, AlPO <sub>4</sub>
Mesoporous	2 < Diameter < 50	HMS,MCM-41,SBA-15
Macroporous	Diameter > 50	Porous gel, Porous
		glasses

In 1992, a research team from Mobil Oil Company synthesized a new family of materials, the so-called M41S [22-25] that presents ordered pore distributions, with homogeneous sizes ranging between 2 nm -10 nm, including different materials like hexagonal-MCM-41, cubic-MCM-48, and lamellar-MCM-50.The mesoporous materials were basically prepared through silica formation around template micelle [26, 27] assemblies followed by template removal by appropriate methods such as calcination and solvent evaporation. Different mesoporous materials are listed in table. 2.

**Table 2: Different mesoporous materials** 

Mesoporous material	Full name
MSU	Michigan State University
SBA	Santa Barbara Amorphous
MCM	Mobil Crystalline Matter/ Mobil
	Composite Matter
HMS	Hollow Mesoporous Silica
OMS	Ordered Mesoporous Silica
TUD	Technische Universiteit Delft
MCF	Meso Cellular Form
FSM	Folded Sheet Mesoporous

These pioneering findings were followed by various kinds of mesoporous materials. For example, hexagonal mesoporous silica (HMS) prepared using neutral amine as template possesses slightly disordered hexagonal structure and thicker walls, superior thermal stability upon calcination in air, and a smaller crystallite size, which affords complementary textural mesoporosity for improved access to the framework-confined mesopores<sup>28</sup>. Michigan State University (MSU-1) synthesized by using polyethylene oxide (PEO) as a structure directing agent also has a disordered channel structure <sup>29</sup>.

This material possesses large wall thickness and small particle size with considerable textural mesoporosity due to pores formed between the relatively small particles.

The widely used material is Santa Barbara Amorphous-15 (SBA-15), having highly orderd pores with thicker pore walls and two dimensional hexagonal structure, by using amphiphilic triblock-copolymer of poly(ethylene oxide) and poly(propylene oxide) (Pluronic P123) as the structure directing reagent in highly acidic media <sup>30</sup>.

In addition to preparation of various mesoporous silica structures, incorporation of heteroatoms such as Cu, Zn, Al, B, Ga, Fe, Cr, Ti, V Sn etc. into mesoporous silica framework has been widely investigated <sup>31-49</sup>. Methodology to prepare mesoporous silica via the template synthesis is extended to preparation of a various mesoporous metal oxides <sup>50-63</sup> such as TiO<sub>2</sub>, Ta<sub>2</sub>O<sub>5</sub>, Nb<sub>2</sub>O<sub>5</sub>, ZrO<sub>2</sub>, Al<sub>2</sub>O<sub>3</sub>, V<sub>2</sub>O<sub>5</sub> etc. as well as synthesis of mesoporous aluminophosphate <sup>64-67</sup>.

In recent years, mesoporous materials, which have unique pore size, higher surface area and pore volume, have been widely employed as carriers for drug delivery.

Compared with amorphous colloidal and porous silica, mesoporous silicas exhibit higher loading of drugs and provide a controlled drug release if modified by functionalisation. Numerous interesting drug delivery applications of mesoporous materials have been demonstrated. Different Mesoporous material like MCM- 41, SBA- 15, TUD, MCM- 50, HMS, TMS etc have many important properties advantageous to drug delivery applications.

The small size of the pores confines the space of a drug and engages the effects of surface interactions of the drug molecules and the pore wall. The size of the pores and the surface chemistry of the pore walls may be easily changed and controlled. Depending on the size and the surface chemistry of the pores, increased or sustained release of the loaded drug can be obtained. Sensitive therapeutic compounds susceptible to degradation, like peptides and proteins are also effectively loaded with mesoporous material. This article reviews the fabrication and chemistry of mesoporous MCM- 41 for biomedical applications, and also the potential advantages of mesoporous MCM- 41 in drug delivery.

# DRUG AND MESOPOROUS MATERIAL

Following oral administration, dissolution of the drug molecule in the gastrointestinal (GI) milieu is a prerequisite for the absorption process. Up to 40 per cent of new chemical entities (NCEs) discovered by the pharmaceutical industry today are poorly soluble or lipophilic compounds. The solubility issues complicating the delivery of these new drugs also affect the delivery of many existing drugs. Low drug solubility often manifests itself in a host of in vivo consequences, including decreased bioavailability, increased chance of food effect, more frequent incomplete release from the dosage form and higher interpatient variability.

Poorly soluble compounds also present many in vitro formulation obstacles, such as severely limited choices of delivery technologies and increasingly complex dissolution testing with limited or poor correlation to the in vivo absorption. These in vivo and in vitro characteristics and the difficulties in achieving predictable and reproducible in vivo/in vitro correlations are often sufficiently formidable to halt development on many newly synthesized compounds due to solubility issues.

Developing strategies to overcome this handicap and to enable oral delivery of these new chemical entities now constitutes one of the greatest challenges to scientists active in pharmaceutical research <sup>68</sup>. Although several formulation approaches including solid dispersions <sup>69</sup>, emulsion based systems <sup>70</sup> and nanosizing <sup>71</sup> have led to promising in vitro results, the number of marketed applications of these technologies remains very limited. Together with the growing number of poorly water soluble compounds, this emphasizes the need to explore new types of approaches.

Ordered mesoporous silica materials have recently attracted much attention because of their emerging applications in drug delivery <sup>72</sup>. Since their first appearance in materials science in the 1990s, these inorganic carriers have been successfully used in other research areas such as catalysis, purification <sup>73</sup> and adsorption <sup>74</sup>.

The majority of ordered mesoporous materials have a two dimensionally ordered array of cylindrical pores of uniform size disposed parallel to each other and separated by thin walls <sup>26, 27</sup>. MCM-41 (Mobil Composition of Matter number forty one) and SBA-15 (Santa Barbara Amorphous number fifteen) are probably the most investigated materials of this type. Mesoporous materials based on silica are currently a field of intensive activity because of their high potential in a very broad range of applications. A series of inorganic mesostructures, like MCM41, HMS, SBAn etc, have been synthesized with different templating schemes <sup>26, 27</sup>, Amongst different such materials some are listed in table.3 with their structural characteristics.

Tab	le 3: 1	Structural	Cha	aractei	istics	of	f meso	porous	mater	ial	ls
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Types	of	mesoporous	Structural characteristics
materials			
	MCI	M-41	Hexagonal 1 D
	MC I	M- 48	Bicontinuous 3 D
	SB.	A- 1	Cubic- 3 D
	SB	A-3	Hexagonal 2 D
	SBA	A-15	Hexagonal 1 D
	SBA	A- 16	Cage like arrangement
	М	SU	Hexagonal 2 D
	Н	MS	Hexagonal

The operating tool in mesoporous MCM- 41 is the presence of micropores and these micropores are located in the walls between adjacent mesopores and do not bridge the wall; they constitute dead end pores <sup>75</sup>. Due to their open and well-defined pore system in combination with high surface area, ordered mesoporous MCM- 41 is potential carrier for therapeutic molecules <sup>76</sup>. During the last

few years, a number of interesting drug delivery applications of mesoporous materials has been demonstrated. Table. 4

#### **CHEMISTRY OF MESOPOROUS MATERIAL MCM-41**

In 1990, Yanagisawa and colleague reported the synthesis of the mesoporous materials which shows the characteristic of MCM-41. Through intercalation of long-chain alkyltrimethylammonium cations into the layered silicate kanemite followed by calcination to remove the organic species, a mesoporous material was obtained. The silicate layers condensed to form a three-dimensional structure with "nanoscale pores".

Studies related to MCM-41 began in 1992 when a group of scientists employed by the Mobile Corporation published a paper entitled "A New Family of Mesoporous Molecular Sieves Prepared with Liquid Crystal Templates" <sup>25</sup>. The paper described the synthesis and characterization of a new family of mesoporous molecular sieves to which they gave the name M41S. MCM-41 is a material belonging to this family. The material was an improvement over other mesoporous materials of the time, which were generally amorphous solids with irregularly spaced, non-uniform sized pores<sup>25</sup>. A successful synthesis of MCM-41 produces a pure silica material composed by a hexagonal array of tubular channels of nearly uniform diameter.

Interconnections between the pores of MCM-41 are energetically unfavourable and the pore walls are made of an amorphous arrangement of silica tetrahedral <sup>97</sup>. The mesoporous structure can be controlled by a sophisticated choice of templates (surfactants), adding auxiliary organic chemicals, and changing reaction parameters (e.g., temperature, pressure, crystallization time, water content, pH, compositions).

A notable aspect of MCM-41 is that the diameter of the pores can be controlled through the carbon chain length of the surfactant used during synthesis <sup>98-100</sup>. Pore size may also be controlled through the addition of auxiliary organic reagents during synthesis <sup>25</sup>. The addition of some auxiliary compound like 1, 3, 5trimethylbenzene and triisopropylbenzene is effective in increasing the size of micelles <sup>25,67</sup>. Alkanes such as n-pentane, nhexane, n-heptane, n-octane and n-dodecane and N,Ndimethylhexadecylamine which can interact with the micelles of cationic surfactants, lead to the enlargement of the mesopores <sup>2,101</sup>. The specific hydrothermal treatment of mesoporous materials is an another method of obtaining stable and enlarged mesopores <sup>102,103</sup>.

Numerous studies of this novel material have been published since its discovery. However, a multiple review on MCM-41 has never been published except the brief report <sup>104</sup>.

This paper is intended to provide a comprehensive overview on synthesis, formation mechanisms, modification, and applications of MCM-41 in order to its potential applications in drug delivery. MCM-41 is a relatively straightforward material to produce under controlled laboratory conditions. Some common reagents used for synthesis of MCM- 41 are given in and table. 5.

	Table 5:	Reagents	for the	synthesis	of Mcm	41
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Common reagent	Chemical formula
Fumed silica	SiO2
Tetramethyl ammonium silicate	(CH3)4NOH.2SiO2
Tetraethyl orthosilicate	Si(OC2H5)4
Cetyl trimethyl ammonium chloride	C16H33N(CH3)3Cl/ OH
/ hydroxide	
Ammonium hydroxide	NH4OH
Sodium silicate	Na2SiO3
Cetyl trimethyl ammonium bromide	C16H33N(CH3)3Br
Dodecyl trimethyl ammonium bromide	C12H25N(CH3)3Br
Tetramethylammonium hydroxide	(CH3)4NOH
Sodium hydroxide	NaOH

Table 4: Differe	nt mesoporous	s materials	s as d	rug	carrier
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Mesoporous material	Drug	Category	Modification	Comment	Ref
MCM- 41	Ibuprofen, Piroxicam	NSAID		Faster release of drug and increase dissolution of drug	77
TUD- 1	Ibuprofen	NSAID		Faster release of drug and increase dissolution of drug	78
Mesoporous- silica sphere	Gentamicin	Antibiotic	Coating with pH sensitive polyelectrolyte multilayer	Controlled drug release	79
SBA- 15, MCM- 41	Ibuprofen	NSAID		Faster release of drug and increase dissolution of drug	80
Mesoporous- silica powder	Gentamicin	Antibiotic	Hybridization with biodegradable polymer	Sustained release of drug	81
Mnesoporous- silica- nanoparticles	Camptothecin, Taxol	Anticancer	Fluorescent nanoparticles	Effectively targeted to human cancer cells	82
Mesoporous- silica- nanoparticles	Hydralazine	Neuroprotector	functionalizing polyethylene glycol	Significant neuroprotection to damage cells	83
Mesostructured- cellular form	Ibuprofen Vancomycin	NSAID Antibiotic	Modified with hydrophobic polyisoprene	Significantly increase dissolution rate	84
Mesoporous- silica- nanoparticles	Gene	Protein	Surface -functionalization	Effective penetration in cell membranes of animal and plant cells	85
SBA- 15	Atenolol	Antihypertensive	Modified synthesis temperature	Sustained delivery of drug	86
SBA- 15, MCM- 41	Sodium- alendronate	Anti-psoriatic	Surface modification by amine group	Enhanced release rate of drug	87
SBA- 15, MCM- 41	Amoxicillin Erythromycin	Antibiotic "	Use of aqueous and non- aqueous solvents respectively for drug loading	Significantly increase dissolution rate	88
SBA- 15	Itraconazole	Antifungal	-	Faster release of drug and	89
MCM- 41	Atenolol	Antihypertensive	Prepared with hydroxyapatite	Slow drug release	90
MCM- 41	Ibuprofen	NSAID	With different morphology & variable pore geometry	Controlled release	91
Hybrid mesoporous silica	Folic acid, Cisplatin	Vitamin, Anticancer	Functionalization with amino group	Targeting drug delivery	92
Hollow mesoporous silica	Ibuprofen	NSAID	Prepared with polyvinylpyrolidone	Sustained release	93
MCM- 48	Erythromycin	Antibiotic		Delayed release	94
SBA- 15 Mesoporous orgenosilica sphere	Bovine serum Tetracycline	Protein Antibiotic		Controlled release Sustained release	95 96

#### Table 6: Synthesis strategies for MCM-41

Characteristic of Synthesized Mesoporous MCM- 41	Molar ratio of different components	Temperature (°C)	Time (h)	Ref
Prepared with liquid crystal mechanism	2.6 OH: 30 SiO2 : Al2O3: 6.3 CTA: 8.4 TMA: 382H2O	150	48	22
Simple preparation	30 SiO2: 0.4 Al2O3: 2.6 CTA: 4.5 TMAOH: 500 H2O	70	24	126
Prepared in acidic médium	26.9 H: 30 SiO2: 3.5 CTA: 3800 H2O	Ambient	05-24	26
Prepared with primary amine, in acidic medium	0.6 H: 30 SiO2: 192 C2H5OH: 8DA: 1060 H2O	Ambient	18	28
Synthesis of V- MCM-41	5.1 Na20: 30 SiO2: 0.6 VO2: 15 CTMA: 900 H20	100	144	127
Prepared in alkali free medium	4 (NH4)20: 30 SiO2: Al2O3:6 CTA: 700 H2O	100	72	30
Ordered MCM-41 with acetic acid addition	15 OH: 30 SiO2: Al2O3:5 CTMA:1125 H2O	100	72	128
Synthesis of Fe- MCM-41	15 OH: 30 SiO2: 0.3 Fe2O3: 6CTA	150	168- 240	129
Synthesis of B- MCM-41	2.5 Na20: 30 SiO2: x BO2: 4.8 CTA: 1890 H2O	100	24	130
Synthesis of Mn- MCM-41	(4.7 - 14.3) OH: 30 SiO2: (0.01-2.6) MnO:3.5 CTA: 4000 H2O	21-100	72	131

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This paper is intended to provide a comprehensive overview on synthesis, formation mechanisms, modification, and applications of MCM-41 in order to its potential applications in drug delivery. MCM-41 is a relatively straightforward material to produce under controlled laboratory conditions. Some common reagents used for synthesis of MCM- 41 are given in and table. 5. The morphology of the MCM-41 particles depends on the reagents and synthesis procedure used.

Freshly prepared MCM-41 presents as a loose, agglomerated white powder with low mechanical stability <sup>27</sup>. It is the structure and properties of the material at the nanometer scale which have generated a great deal of interest in it and its many potential applications. The uniform size and shape of pores, large surface areas, and high thermal and hydrothermal stability are advantages of MCM-41 with respect to its potential use as a drug carrier and catalyst support <sup>105</sup>.

Various morphologies can be achieved for mesoporous silica using either the templating method or the phase transformation approach. This usually involves order or shape in the micron scale. In addition to the normal particulate form, different shapes are also observed like fibers, gyroids and discoids <sup>106, 107</sup>, ropes <sup>108</sup>, hollow <sup>109</sup>, spheres <sup>110, 111</sup>, films supported <sup>112</sup> or free-standing <sup>113</sup>, tubular <sup>114</sup>, and pillar-within-spheres <sup>115</sup>.

The surfaces of MCM-41 particles are dominated by silanol groups. These silanol groups may be classified as being one of three different varieties: single, (SiO) 3Si-OH-9, geminal, (SiO) 2Si (OH)2; or hydrogen bonded, (SiO) 3Si-OH-OH-Si (SiO)3. The surface density of these groups is approximately 2.5 to 3.0 groups/ nm2 and depends on the surfactant removal technique <sup>116</sup>. Under ambient humidity levels, all silanol groups become involved in hydrogen bonding with drug molecules <sup>117</sup>. If drugs have to be placed into pores, a material with a homogeneous ordered pore distribution should be specially designed. In such material, the drug adsorption and subsequent delivery will be more regular and reproducible than that coming from a disordered pore distribution. A step forward to this type of systems is the transition from nondesigned materials to specially designed porous matrices (ordered mesoporous materials).

The fundamental reasons for such rich morphological behaviors are:

 The silicate ions act as counterions to the cylindrical micelles to organize into soft hexagonal liquid crystalline phase.

- The rich organization of lyotropic surfactant system can be exploited to form many meso- structures.
- Control of higher hierarchical order of size above the nanometer scale can be achieved by fine tuning the interface curvature, either by changing composition or reaction condition.
- Silica condensation reaction can be controlled as in the late stage of the reaction.
- The self- organization and siloxane bond formation processes can be separately controlled.

The composition and pore structures are thoroughly studied with various spectroscopic and microscopic methods such as IR, TGA, SEM, TEM, BET (gas sorption measurements), XRD and solid state NMR. Following synthesis, the materials are characterized to determine particle and pore morphology, structure and surface details. The main characterizing techniques used on most mesoporous materials are low angle powder X-ray diffraction (XRD), nitrogen adsorption/desorption, scanning electron microscopy (SEM), transmission electron microscopy (TEM), and, recently induced coupled plasma atomic emission spectroscopy (ICP-AES), diffuse reflectance ultraviolet-visible spectroscopy (DRUVVIS), and fluorescence spectroscopy, solid state nuclear magnetic resonance (NMR). Adsorption analysis gives information about the porosity and surface area of the materials, while SEM gives particle size and morphology. Diffraction techniques and TEM supply insight to the degree of structural order whereas; solid state NMR measurements provide details regarding the surfaces of MCM-41 materials. Chemical composition of mesoporous particles can be examined by energy dispersive spectrometry (EDS). Many a times the obtained materials are characterized by thermal analysis like thermogravimetric (TG) and Differential scanning calorimetry (DSC).

The use of mesoporous materials as drug carrier has been extensively studied in an attempt to make use of their uniform mesopores and large surface areas. The drug loading is performed by direct impregnation methods. The mesoporous matrix is placed either as powder particles with regular sizes or as compacted pieces into the solution of the drug with a given concentration. In this impregnation procedure several factors have to be considered like the solution pH, temperature, drug solubility and polarity and generally its chemical nature. The release process is then carried out placing the drug-loaded mesoporous matrices into a solution and monitoring the drug concentration along the test time. In particular, a good election is a simulated body fluid. The selection of the loading solvent will have an effect on the amount of loaded drug. Thus when polar drug molecules such as amoxicillin <sup>118</sup> or gentamicin <sup>119</sup> are targeted, a polar solvent like water have to be used to enhance the concentration of drug into the pores. Sodium alendronate <sup>120, 121</sup> is a water-soluble salt, so an aqueous saline solution buffered at pH 4.8 was used to load this drug into mesoporous matrices. On the other hand, when a non-polar drug is aimed like ibuprofen, the chosen solvent also needs to be non-polar like hexane. Intermediate cases can also be found like erythromycin 122 that has to be loaded using acetonitrile. The drug loading into the mesoporous matrices is controlled by the chemical nature of the pore walls. The inorganic network of silica-based ordered mesoporous materials is plenty of silanol groups (Si-OH) that would interact with the functional groups of the drug. Depending on the strength of this attracting interaction, the drug retention will be modulated. Thus, ibuprofen that has a carboxylic acid group would form hydrogen bonds with the silanol groups and consequently drug molecules would be retained into the mesopores 123.

The release kinetics of drugs from OMS carriers is dependent on several material characteristics including pore size <sup>100</sup>, pore connectivity <sup>124</sup> and the chemical composition of the silica surface <sup>125</sup>. Initially, the focus of mesoporous silica materials has been on the development of slow release formulations; but the applicability has recently been expanded towards dissolution enhancement of poorly water soluble compounds. Numerous research papers have revealed

the use of mesoporous material as drug carrier; some are listed in table. 4.

#### **MECHANISM OF SYNTHESIS OF MESOPOROUS SILICA MCM-41**

The synthesis of mesoporous material is one of the most important subjects in modern pharmaceutical science. The synthesis and applications of mesoporous materials prepared using surfactant as templates have attracted great attention since the discovery of the M41S family of mesoporous molecular sieves by scientists at the Mobil Corporation. The main characteristics of MCM-41 materials are their high thermal stability, large surface area and narrow pore size distribution.

Different synthesis strategies have been proposed and successfully used, some reported synthesis for mesoporous MCM -41 are given in table. 6. However, there is one thing all these procedures have in common next to the obvious presence of a source of silica, viz. a templating agent. A template is a structure-directing agent, which is usually a relatively simple molecule or ion, around which a framework is built up. The most common templates for the synthesis of MCM-41 are quaternary ammonium ions with long alkyl chain, generally a hexadecyl group.

The energetically most favourable form of micelles is spherical, because in this geometry the surface energy is minimised most efficiently. Moreover, this conformation allows the largest number of micelles to be formed out of a certain amount of template, which is attractive considering the entropy of the system.

Nevertheless, it is observed that at increasing amounts of template in water different micelle geometry evolves: the spherical micelles gradually transform into long tubes, often denoted as rod-like micelles. Increasing the template concentration even further results in aggregation of the rod-like micelles into a hexagonal liquid crystalline structure, resembling the MCM-41 structure. If the template concentration is increased further this hexagonal liquid crystalline phase first transforms into a cubic liquid crystalline phase and eventually, at the highest template concentrations, into a lamellar liquid crystalline phase. The cubic liquid crystalline phase resembles the structure of mesoporous MCM-48, whereas the lamellar phase is the structural analogue of MCM-50 (an unstable material, which consists of platelets of amorphous silica). Because of the resemblances between the liquid crystalline phases and the MCM structures it is often assumed that the liquid crystalline structures are the actual templates of MCM-41 and MCM-48.

According to Myers <sup>132</sup>, the particular phase present in a surfactant aqueous solution at a given

concentration depends not only on the concentrations but also on the nature of itself (the length of the hydrophobic carbon chain, hydrophilic head group, and counterion) and the environmental parameters (pH, temperature, the ionic strength, effect of stirring, effect of addition of silica source and other additives).

Once MCM-41 has been formed its pores are filled with template and in order to obtain a completely mesoporous support material the micelles must be removed. The most elegant solution to this demand is removal by means of repeated washing with (slightly acidified) mixtures of organic solvent and water, resulting in extraction of the template. The resulting solutions, containing the template, can be evaporated to dryness, which leads to recovery of the template. If the synthesis conditions were relatively mild the template will not have decomposed and can be re-used for a next synthesis. A simpler method for template removal is calcination. During this process template is decomposed into CO2, some NOx and steam.

Certain factors greatly affect the properties and characteristics of mesoporous MCM- 41, some of the factors are discussed below.

The most frequently used template for the synthesis of MCM-41 is hexadecyl (cetyl) trimethyl ammonium bromide (or chloride), i.e. a template with an alkyl chain containing sixteen -CH2 moieties. This template yields MCM-41 with a uniform pore size. Using templates with longer or shorter alkyl chains the pore size of MCM- 41 can be influenced. Different research articles revealed the use of cationic surfactant for the synthesis of mesoporous silica, though several articles imposed the use of anionic surfactant as well as non ionic surfactant also 133, <sup>134</sup>. The variation in the sizes and shapes of the templates leads to the formation of mesoporous materials with different pore sizes and structures. The mesoporous materials that are prepared using anionic surfactants show chiral properties in their pores, and thus, they attract much attention as adsorbents that are useful in the separation of chiral drug molecules <sup>135, 136</sup>. Cationic surfactants with increased carbon chains length show increase in the size of micelles <sup>137, 138</sup>. Although the increase in the length of the carbon chains of anionic surfactants definitely results in the enlargement of the mesopores, the extent of the enlargement is not sufficient due to the difficulty in the preparation of long chain surfactants. Furthermore, the addition of alkylbenzenes and amines to the synthetic mixtures of mesoporous materials containing anionic surfactants is usually ineffective in enlarging their pore sizes. One research article imparts that, when ordered mesoporous materials have been synthesized using mixture of surfactants such as cationic/nonionic 139 and cationic/anionic surfactants <sup>140</sup>, give rise to mesoporous materials with well defined pore sizes and morphologies. Mixtures of surfactants with different charges allow a wide variety of silica sources and synthetic conditions for the preparation of mesoporous materials. The surface properties of the pore walls is also different according to the type of surfactant used.

Silanol groups on the pore walls are also susceptible of undergoing a chemical modification with a large variety of organic groups through a functionalisation process. Indeed, the pore-wall modification would be performed depending on the functional groups of the drug molecules to be adsorbed. For example, sodium alendronate, a drug employed for osteoporosis treatments, has two phosphonate groups that would undergo stronger attracting interactions with amine groups than with silanols <sup>120</sup>. Therefore, if the pore wall surface is covered by amine groups, there would be a larger alendronate loading than in unmodified materials. The result shows that drug loading increased from 14% (unmodified) to 37% (modified) for amine-grafted materials MCM-41.

The pH of the synthesis procedure also has influence on pore size and volume of MCM-41. Cheng and his colleague studied the postsynthesis structural modulation of silica by the treatments with the ammonia solution of NH40H and the aqueous solution of H2SO4. Their investigation revealed that NH40H treated silicas generally have smaller unit cell parameters, smaller mesopores sizes and lower pore volumes, while the H2SO4 treatment gave materials with larger mesopores sizes and pore entrances but very low pore volumes<sup>141</sup>.

# ORDERED MESOPOROUS MATERIALS: IMMEDIATE VS CONTROL RELEASE

Conventional dosage forms have the disadvantage of not being able to control either the rate of drug delivery or the target area of drug administration and provide a rapid and an immediate drug release. Thus, frequent administration is necessary in order to maintain a therapeutic level, which in turn causes drug concentration in blood and tissues to fluctuate widely. Polymeric cross-linked carrier matrices, such as hydrogels and supra-molecular polymer aggregates as well as different types of microencapsulation vehicles, are typical examples of common drug delivery devices. Depending on the delivery system and the pharmaceutical in use, different release mechanisms are applied. However, there are three primary ways by which active agents can be released from such system: diffusion, degradation, and swelling followed by diffusion. Any or all of these mechanisms may occur in a given release system. Diffusion occurs when a drug or other active agent passes through the system (a ceramic or polymer based matrix) that forms the controlledrelease device. The diffusion can occur on a macroscopic scale as through pores in the matrix or on a molecular level, by passing between, for instance, polymer chains. The diffusion controlled release could be activated by several means, including ionic strength, pH and thermal, magnetic or chemical changes. The ability to control over the drug delivery can be an important factor especially at times when traditional oral or injectable drug

formulations are difficult to distribute. In some cases there might be a need of a slow release of a water soluble drug or a fast release of low-solubility drugs. It might also be convenient for drug delivery to specific sites, drug delivery using nanoparticulate systems, delivery of two or more agents with the same formulation, and also systems based on carriers that can dissolve or degrade and be readily eliminated. The ideal drug delivery system should be inert or biodegradable, biocompatible, mechanically strong, comfortable for the patient, capable of achieving high drug loading, safe from accidental release, simple to administer and remove, and easy to fabricate and sterilize.

Mesoporous silica has many important properties advantageous to drug delivery applications. The small size of the pores confines the space of a drug and engages the effects of surface interactions of the drug molecules and the pore wall. The size of the pores and the surface chemistry of the pore walls may be easily changed and controlled. Depending on the size and the surface chemistry of the pores, increased or sustained release of the loaded drug can be obtained. As the purely siliceous mesoporous materials have been shown to be biocompatible, or sometimes even bioactive, there is an increasing interest in this class of materials for applications in the field of bioceramics, especially as bone substitute materials. Furthermore, the highly organized porous silica matrix could be used as a potential controlled drug release system. Another attractive advantage is that amorphous silica is degradable in an aqueous solution, and thus problems related to the removal of the material after use can be avoided.

Numerous articles represent the use of mesoporous materials as pharmaceutical carrier systems for immediate as well as controlled drug release. Mesoporous materials can be used as medical devices because of the presence of larger pores and well-defined structure. They present high surface areas, above 1000 m2/g, and ordered mesopores ranging from 2.0 nm to tens nanometers, depending on the conditions of synthesis. It is observed that mesoporous materials exhibit high drug loading and the amount can be as high as 97 wt%. Several factoring can influence the drug loading such as pore structure, surface functionality, morphology, drug molecule size and solvent for drug loading. Generally, hollow mesoporous silica presents the highest loading for various drugs due to their hollowed pore structure. Higher surface area and pore size will favour the loading of drug. Grafting/ functionalisation of mesoporous silica change the pore size and the interaction between drug and substrate, resulting in lower drug loading and slow release rate.

Vallet-Regi and colleague were one of the first to explore the drug release properties of these materials in an attempt to prolong the release of ibuprofen using MCM-41 as a carrier <sup>85</sup>. Charnay showed a rapid and pH dependent release of ibuprofen from MCM-41 with a pore size of 3.5 nm 142. Later studies evidenced a high mobility of ibuprofen inside the pore system of MCM-41 at ambient temperature and pointed out the weak interaction of ibuprofen with the silica matrix. Cavallaro have investigated mesoporous silicate as devices for drug delivery. Four anti-inflammatory agents such as diflunisal, naproxen, ibuprofen and its sodium salt have been used. Drug release studies were also performed at pH 1.1 and 6.8 mimicking gastrointestinal fluids. Release data suggest that the matrix impregnated with diflunisal offers good potential as a system for the modified drug release 143. Qu recently studied a water-soluble drug captopril with mesoporous MCM-41 system <sup>144</sup>. The drugloading amount is correlated to the Brunauer-Emmett-Teller (BET) surface area and surface hydrophilicity and hydrophobicity of the mesoporous silica material, while drug release profiles could be controlled by tailoring the surface properties and pore size. Trewyn presented an investigation on preparation of mesoporous silica nanoparticle (MSN) materials with various particle morphologies, including spheres, ellipsoids, rods, and tubes, using roomtemperature ionic liquid (RTIL). By changing the RTIL template, the pore morphology was tuned from the MCM-41 type of hexagonal mesopores to helical channels, and to wormhole-like porous structures. These materials were then used as controlled-release delivery nanodevices to release antibacterial ionic liquids against Escherichia coli K12. The antibacterial activity was dependent on the rate of diffusional release of the pore encapsulated RTIL, which

was governed by the particle and pore morphology of the MSN materials  $^{\rm 145}\!.$ 

Mesoporous silica nanoparticles possess several attractive features such as large surface areas and porous interiors that can be used to store various molecules. In addition, their pore size and environment as well as their size and shape can be easily modified, making them a suitable choice as intracellular drug carriers. Jie prepared biocompatible mesoporous silica nanoparticles, containing the fluorescence dye fluorescein isothiocyanate; provide a promising system to deliver hydrophobic anticancer drugs paclitaxel to cancer cells. In this study, they have shown that fluorescent mesoporous nanoparticles (FMSN) are efficiently taken up by human cancer cells. They have also shown that a hydrophobic anticancer drug paclitaxel can be stored in FMSN and delivered to human cancer cells resulting in the inhibition of proliferation of these cells. These results point to the useful feature of FMSN as a valuable vehicle for anticancer drugs 82. Another important application of mesoporous nanoparticles also represented by Jie is that it acts as dissolution enhancer for poorly soluble anticancer drug camptothecin (CPT), that was successfully entrapped into the pores of fluorescent mesoporous silica nanoparticles (FMSN) and delivered CPT into a variety of human cancer cells to induce cell death, demonstrating that mesoporous silica nanoparticles are promising in overcoming the insolubility problem of anticancer drugs 82. Similar findings were mentioned by Wei Sun, when they prepared mesoporous silica nanoparticles (MSN) for lung cancer therapy, It revealed the three-dimensional distribution of the MSN inside the cell. MSNs can be a good drug delivery vector and have lots of applications in controlled drug release systems, as they may be selectively targeted to specific cellular organelles through surface modification. Therefore, drugs can be protected from enzymatic digestion in the cell cytoplasm by capping the channels in MSNs <sup>146</sup>. This approach can be employed to study real-time drug release events in living cells when MSNs or other nanoparticles are used as drug delivery vectors. Shenmin Zhu have explored the use of polymer with mesoporous silica with large pore seize for drug release. They were using hydrophobic polyisoprene (PI) through free radical polymerization in the pores network, and the resulting materials (MCF-PI) were investigated as matrices for drug storage. Ibuprofen (IBU) and vancomycin were selected as model drugs and loaded onto unmodified MCF and modified MCF (MCF-PI). The adsorption capacities of these model drugs on MCF-PI were observed increase as compared to that of on pure MCF, due to the trap effects induced by polyisoprene chains inside the pores. The delivery system of MCF-PI was found to be more favorable for the adsorption of IBU 147. Kamalakannan have reported the preparation of MCM-41 silica spheres via the pseudomorphic route. Subsequent surface modification of the mesoporous silica spheres was achieved by two silylating agents, noctadecyltrihydridosilane and noctadecyltrimethoxysilane, which provided different surface morphology and prepared MCM- 41 spheres are highly ordered and having practically uniform mesopores <sup>148</sup>. Some of the research articles have reported the post synthesis treatment which provides important information regarding the surface geometry and morphology of mesopores.

Ordered mesoporous silica has stable mesoporous structure, large surface area, good biocompatibility and tailored size of mesopores, all these requisites exhibited promising application as immediate and controlled drug delivery system. For applications in drug delivery systems , the development of mesoporous materials offer new possibilities for incorporating biological agents and different category of drugs such as anti-inflammatory agents, antibiotics, antifungal, chemotherapeutic drugs, steroids, hormones and vaccines, within a silica sample and for controlling the release kinetics from the matrix because of its well-arranged structure. The delivery of these molecules was once considered impossible because of the difficulty associated with the diffusion of large molecules through the materials of conventional drug delivery systems. These organic substances are normally very large in size, and one can anticipate that mesoporous silica would have a potential for encapsulating bioactive molecules by utilizing ordered mesopores. Plenty of drugs were evaluated for their loading and release characteristics with respect to mesoporous material and all have showed a very potential effect for its controlled and immediate

release pattern. List of such drugs and respective mesoporous materials provided in table.  $\mathbf 4$ 

## FUTURE POTENTIAL

Nanotechnology is a fast-growing area, involving the fabrication and use of nano-sized materials and devices. Various nanocomposite materials play a number of important roles in modern science and technology. Porous inorganic nanoparticles are of particular importance due to their broad range of potential applications. The synthesis of the mesoporous silicas MCM-41 and MCM-48 in 1992, using a supramolecular surfactant system as a template, provoked a boom in mesoporous materials.

Mesoporous materials (MCM-41), the basis for nano-technologies, are one of the fastest developing fields in pharmaceutical science. It has been shown that ordered mesoporous silica with stable mesoporous structure, large surface area, good biocompatibility and tailored size of mesopores and functionalisation has exhibited promising application as drug delivery system. The mesoporous silica demonstrates higher drug loading followed by controlled sustained release as well as immediate release. The drug release rate is governs by pore size and functional groups on the wall. Functionalisation of MCM-41 leads to cover the walls of silica resulting in pore size decrease and lower drug loading; however, it brings in controlled drug release. In most cases, drug release is a diffusion-controlled process and exhibits a two-stage profile. However, few investigations have been attempted to explore the drug release kinetics and more work should be focused because the understanding of kinetics will help in the achievement of controlled drug release. Surface functionalisation with various groups can change electrostatic, hydrophobic/hydrophilic forces, and the adhesive interactions of drug and matrix, inducing varying drug loading and delivery rate. Moreover, functionalisation with different groups will make the systems attached to cell and biological species such as proteins and enzymes. Future work should be directed to development of non-immunogenic polymer/mesoporous solid as drug carrier, which will show more advantages than glass-polymer systems. There are also many emerging biotechnologies that can benefit from the mesoporous materials-based drug delivery. Bone tissue engineering is an emerging area directed towards the design of materials that will help an organism to improve its ability of regeneration by recovering both the structure and also its function. Biocompatible and bioactive mesoporous materials with controlled drug delivery will favour the cellular growth and bone regeneration. Research should be directed towards finding suitable combination of bioactivity and controlled drug delivery kinetics. For direct drug delivery, nanosize particles have been attracted much attention. These nanoparticle carriers can effectively penetrate or pass through the cell membrane into cells, achieving controlled cellular delivery. Although a lot of inorganic nanoparticles have been produced, little work has been done in synthesis of nanosize mesoporous silica particles. The combination of the mesoporous characteristics and the properties of nanoparticles will provide a fascinating application of nanoparticles for biotechnology and biomedicine and more efforts should be attempted.

Many potential applications of mesoporous MCM-41 have been explored, from catalysis, separation, biology, environmental monitoring, and pharmaceuticals to clinical toxicology, but a gap in real industrial applications still exists. The great challenge facing the mesoporous materials community now is to transfer laboratory studies to industrial applications. Although the potential applications of such materials have been widely studied in many areas, more efforts are still needed for the continuing study of their practical applications to commercialize mesoporous materials in the future. The forthcoming practical applications in fields such as drug delivery, biotechnology, gene & protein therapy, new drug delivery system, catalysis, separation, adsorption, electronic devices, low dielectric constant materials and beyond will stimulate more research interests in this area, and more exciting and useful developments in mesoporous materials will also be delivered.

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