

**FORMULATION OF IBUPROFEN LOADED ETHYL CELLULOSE NANOPARTICLES BY NANOPRECIPITATION TECHNIQUE****P.SWATHI<sup>1</sup>, A.KRISHNA SAILAJA<sup>2</sup>,****<sup>1</sup> Project Assistant, RBVRR Women's College of Pharmacy, Barkathpura, Hyderabad-27, <sup>2</sup>Associate Professor, RBVRR Women's College of pharmacy, Osmania University, Hyderabad-27.  
Email: pamulapartiswathi@gmail.com****Received: 15 May 2014, Revised and Accepted: 5 June 2014****ABSTRACT**

**Objective :** The present study was undertaken to prepare and characterize drug loaded Ethyl cellulose nanoparticles using nanoprecipitation technique. The model drug chosen was Ibuprofen.

**Methods:** These nanoparticles were prepared using nanoprecipitation technique in which the organic phase containing varied proportions of drug and the polymer was added drop wise to the aqueous phase having the stabilizer with continuous stirring. This resulted in the formation of precipitate in the aqueous phase. The stirring was continued for about 2 hours further. Then, the precipitate was collected by subjecting the sample to vacuum filtration and was air-dried.

**Results:** The best formulation among all the three was determined by comparing the particle size, stability and invitro drug release of all the formulation. F3 was considered as the best formulation with average particle size as 251.1 nm, zeta potential as -25.2 mV, and 86.02 % drug release which was sustained till 8 hours.

**Conclusion:** F3 formulation i.e.; in which concentration of drug and polymer bears a ratio of 1:2 was concluded as the best because of their smaller particle size and greater stability.

**Keywords:** Acetone, Ethyl cellulose(EC), Ethanol, Ibuprofen, Nanoparticles, Nanoprecipitation.

**INTRODUCTION**

The major focus on Novel drug delivery systems during the past two decades is to improve the therapeutic efficacy and safety profile of the drug substances. Colloidal drug delivery systems are considered to be more popular than the matrix or reservoir drug delivery systems. Among all the colloidal systems, Nanoparticles hold promise as drug delivery through various routes due to their greater stability and easier manufacturing ability. These systems are used for specific drug delivery, controlled drug delivery and also for the improvement of bioavailability of the hydrophobic drugs[1].

Nanoparticles are colloidal particles having size below 1  $\mu\text{m}$ . The production of these nanoparticle systems can be categorized in to two, based on the specific characteristics in the materials used. First category involves reactive synthesis from solubilized small molecular precursors and the second involves the fabrication of bulk materials into nanostructures. Nanoprecipitation is one of the method that is included under second category. It is widely applicable technique that is less energy consuming and less complex method. The principle behind this technique is the interfacial deposition that occurs due to the displacement of a solvent with the non-solvent. The parameters that influence the formation of the nanoparticles in this method are miscibility of the solvents and the presence of the dilute polymer solutions. The various polymers undergoing this method are macromolecules that can form complexes in the nanoscale range called as Polyplexes, when come in contact with oppositely charged molecules such as genes and proteins.[2]

This method is considered to be the most sensitive and low energy consuming one as it requires low energy costs and no special equipment requirements. The various polymers involved in this technique are not only Poly(lactide), Poly(lactide-co-glycolide) and Poly caprolactone but also other lactones, cellulose ethers and esters like cellulose butyrate acetate, ethyl cellulose, hydroxyl methylpropylcellulose phthalate, cellulose acetophthalate, naturally

occurring polymers(gelatin, Arabic gum), poly(vinyl alcohol acetophthalate), copolymers of acrylate acrylate and methacrylate (Eudragit), poly(vinyl pyrrolidone-vinyl acetate), maleic acid derivatives, etc.

It is most suitable method for hydrophobic drugs and the problem arises when a hydrophilic drug has to be encapsulated in the polymeric matrix by this method. The problem can be minimized by adjusting the pH value or by choosing appropriate solvent/non-solvent.[3],[4]

Ethyl cellulose is a semi synthetic material having properties like biocompatibility and degradation to non toxic and readily excreted products. It is a very useful polymer for the preparation of nanoparticle drug delivery system, as is water-insoluble, wall-forming polymer.[5]

The model drug selected for this work was Ibuprofen. It is a non-steroidal anti-inflammatory drug that is used to relieve symptoms of pain of arthritis. Other uses includes primary dysmenorrhoea, alleviating fever and reducing inflammation, also helping in showing analgesic, anti-platelet and vasodilation effect.

The objective of the present study includes formulation of nanoparticles containing Ibuprofen using ethyl cellulose as the retardant polymer which will release the drug at the gastrointestinal tract for a prolonged duration to promote patient compliance and to evaluate the effect of various process variables on mean particle size, percentage yield, percentage encapsulation efficiency of the formed Ibuprofen nanoparticles.

**MATERIALS**

Drug : Ibuprofen (Gift Sample)

Polymer : Ethyl Cellulose, obtained from SD Fine Chem. Limited, Mumbai.

Stabilizer : Tween - 20, obtained from SD Fine Chem. Limited, Mumbai.

Solvents : Ethanol, Acetone, obtained from SD Fine Chem. Limited, Mumbai.

## METHODOLOGY

Nanoprecipitation technique was adopted for the preparation of Ibuprofen loaded Ethyl Cellulose nanoparticles. The processing parameters like concentration of the drug, polymer and amount of solvents chosen were varied and three different formulations were prepared [6],[7],[8]. In the first formulation (F1), equal quantities of drug and polymer were dissolved in water miscible solvents i.e.; 6ml of Ethanol and 6ml of Acetone respectively. Tween-20 (0.1%) which acts a stabilizer was added to the aqueous phase. Above prepared organic phase was added drop-wise to the aqueous phase with continuous stirring. The appearance of precipitate in the solution was considered as the end point. After the attainment of endpoint, the solution was kept for stirring for about 2 hours. The precipitate was separated from the solution by means of filtration. The obtained precipitate was air-dried to remove the moisture content.

Similarly, in the second formulation (F2), drug and polymer were taken at the ratio of 1:1.5 and were dissolved in 6ml of Ethanol and 10ml of acetone respectively. Further the above steps were repeated. In the third formulation (F3), the amount of polymer taken was doubled when compared to that of the drug. They were dissolved in 6ml of Ethanol and 12 ml of Acetone respectively.

The dried free flowing powder obtained for all the formulations (F1, F2, F3) were then characterized for particle size distribution and zeta potential to ensure that they were within nanosize range and possessed optimum stability respectively. Further, they were evaluated for following parameters like entrapment efficiency, loading capacity and invitro drug release.

### Characterization of Nanoparticles

#### Drug Content and Drug Entrapment Efficiency

Drug content was determined as follows

50 mg from each formulation of prepared drug loaded EC nanoparticles prepared by nanoprecipitation technique, were dissolved in 50 ml of methanol and kept for stirring at 600 rpm for 3 hours respectively. The total amount of the drug in each formulation was determined spectrophotometrically at 221 nm.

Entrapment efficiency and Loading capacity were determined as follows

50 mg from each formulation of prepared drug loaded EC nanoparticles prepared by nanoprecipitation technique, were dissolved in 50 ml of 7.2 pH phosphate buffer and were kept for ultracentrifugation for 40 minutes respectively. Entrapment efficiency and loading Capacity of each formulation was determined using the formula :

$$\text{Entrapment Efficiency} = \frac{\text{Total amount of the drug entrapped}}{\text{Total amount of the drug initially taken}} \times 100$$

$$\text{Loading Capacity} = \frac{\text{Total amount of the drug entrapped}}{\text{Total weight of the nanoparticles taken}} \times 100$$

#### Particle Size Analysis and Zeta Potential Measurement

The average particle size and size distribution of Ibuprofen loaded EC NP's were determined by dynamic light scattering (DLS), using Horiba Zetasizer.

The Zeta potential (Surface Charge) which indicates the stability of the NP's can be defined as electrokinetic potential that is determined by electrophoretic mobility. Samples were prepared by diluting with

water and corresponding zeta potential were measured using Horiba Zeta Sizer.

Determining the size and morphology of the nanoparticles:

Scanning Electron Microscopy is used to determine the shape, size and surface morphology of the nanoparticles. Nanoparticulate suspension is made to obtain Photomicrographs of the drug loaded ethyl cellulose nanoparticles using this SEM. In Vitro Drug Release Studies:

The invitro drug release studies were carried out using Arbitrary Shaker. The prepared nanoparticles of each formulation were placed in conical flask each and were dispersed using 50 ml of 7.2 pH buffer. The entire system was kept at  $37 \pm 0.5$  °C with the continuous stirring at 100 rpm. The samples were withdrawn at predetermined intervals and replaced by fresh medium simultaneously. The amount of drug released for each formulation at specific time interval was determined with UV spectrophotometrically at 221 nm. [9], [10]

## RESULTS AND DISCUSSIONS

The yield obtained for all the formulation for Drug loaded EC nanoparticles prepared by nanoprecipitation technique were optimum. They were evaluated for above mentioned characters and results obtained were as follows:

**Drug Content of the formulations:** The drug content for all the formulations were evaluated. It was observed that the NPs of F1 showed a higher drug content value i.e; 93.11%. NPs of F2 and F3 showed drug content values as 84.52% and 88.56% respectively.

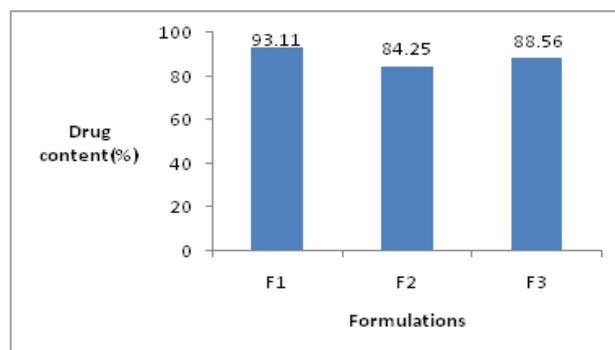


Fig. 1: It shows Drug Content of NPs of various formulations prepared by nanoprecipitation technique.

**Entrapment Efficiency and Loading Capacity of the formulations :** Entrapment efficiency and loading capacity were found to be more for Nanoparticles having higher polymer concentration when compared to drug. The entrapment efficiencies were found to be 77.58%, 88.81% and 95.8% for F1, F2, F3 respectively.

The loading capacities of these formulations i.e; F1, F2, F3 were observed as 56.25%, 35.75%, 43.15% respectively.

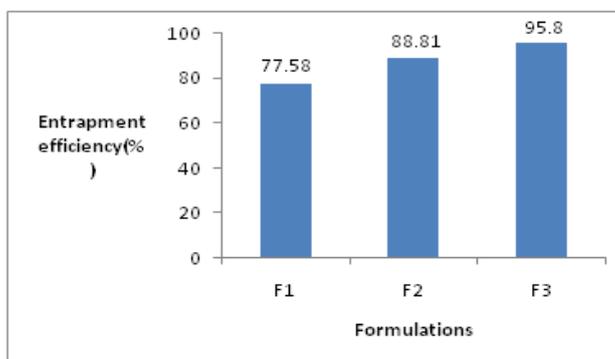


Fig. 2: It shows Entrapment Efficiency of NPs of various formulations prepared by nanoprecipitation technique.

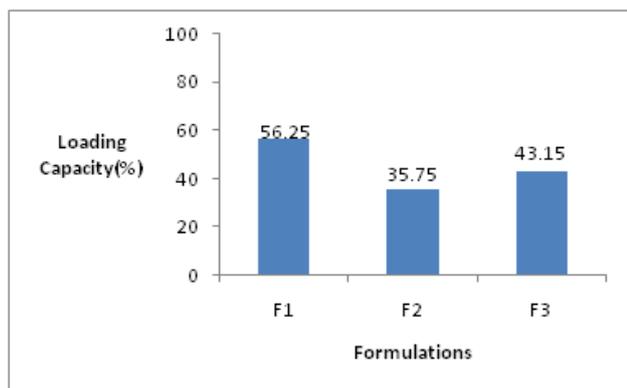


Fig. 3: It shows Loading Capacity of NPs of various formulations prepared by nanoprecipitation technique.

**Average Particle size and Zeta Potential:** The size distribution of the prepared nanoparticles along the mean diameter were measured using particle size analyser. The average particle size of the prepared drug loaded Ethyl Cellulose nanoparticles were recorded. It was found minimum for F3 formulation i.e.; 251.1 nm.

**HORIBA SZ100 Z**

**Measurement Results**  
 Date : 14 May 2014 13:37:13  
 Measurement Type : Particle Size  
 Sample Name : Ibu-EC (1-2)  
 Scattering Angle : 90  
 Temperature of the holder : 25.0 deg. C  
 T% before meas. : 31848  
 Viscosity of the dispersion medium : 0.895 mPa.s  
 Form Of Distribution : [Standard]  
 Representation of result : Scattering Light Intensity  
 Count rate : 73 kCPS



**Calculation Results**

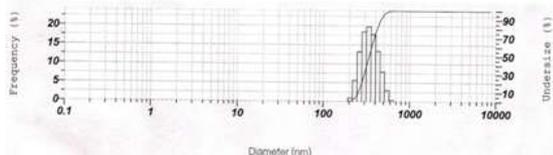
Peak No.	S.P.Area Ratio	Mean	S. D.	Mode
1	1.00	350.5 nm	79.2 nm	334.4 nm
2	---	---	---	---
3	---	---	---	---
Total	1.00	350.5 nm	79.2 nm	334.4 nm

**Histogram Operations**

% Cumulative (1) : 10.0 (%) - 255.2 (nm)  
 % Cumulative (2) : 50.0 (%) - 339.4 (nm)  
 % Cumulative (3) : 90.0 (%) - 463.2 (nm)  
 Mean : 350.5 nm

**Cumulant Operations**

Z-Average : 251.1 nm



No.	Diameter	Frequency	Cumulation	No.	Diameter	Frequency	Cumulation	No.	Diameter	Frequency	Cumulation
1	0.100	0.000	0.000	101	100.000	0.000	100.000	201	10000.000	0.000	100.000
2	0.125	0.000	0.000	102	112.200	0.000	100.000	202	11220.000	0.000	100.000
3	0.156	0.000	0.000	103	125.900	0.000	100.000	203	12590.000	0.000	100.000
4	0.195	0.000	0.000	104	142.400	0.000	100.000	204	14240.000	0.000	100.000
5	0.248	0.000	0.000	105	161.900	0.000	100.000	205	16190.000	0.000	100.000
6	0.311	0.000	0.000	106	184.800	0.000	100.000	206	18480.000	0.000	100.000
7	0.391	0.000	0.000	107	211.500	0.000	100.000	207	21150.000	0.000	100.000
8	0.494	0.000	0.000	108	242.400	0.000	100.000	208	24240.000	0.000	100.000
9	0.628	0.000	0.000	109	278.000	0.000	100.000	209	27800.000	0.000	100.000
10	0.799	0.000	0.000	110	320.000	0.000	100.000	210	32000.000	0.000	100.000
11	1.012	0.000	0.000	111	369.000	0.000	100.000	211	36900.000	0.000	100.000
12	1.280	0.000	0.000	112	426.400	0.000	100.000	212	42640.000	0.000	100.000
13	1.616	0.000	0.000	113	493.600	0.000	100.000	213	49360.000	0.000	100.000
14	2.031	0.000	0.000	114	572.400	0.000	100.000	214	57240.000	0.000	100.000
15	2.560	0.000	0.000	115	664.400	0.000	100.000	215	66440.000	0.000	100.000
16	3.241	0.000	0.000	116	771.200	0.000	100.000	216	77120.000	0.000	100.000
17	4.121	0.000	0.000	117	895.600	0.000	100.000	217	89560.000	0.000	100.000
18	5.250	0.000	0.000	118	1040.000	0.000	100.000	218	104000.000	0.000	100.000
19	6.681	0.000	0.000	119	1208.000	0.000	100.000	219	120800.000	0.000	100.000
20	8.481	0.000	0.000	120	1403.200	0.000	100.000	220	140320.000	0.000	100.000
21	10.791	0.000	0.000	121	1630.400	0.000	100.000	221	163040.000	0.000	100.000
22	13.761	0.000	0.000	122	1895.200	0.000	100.000	222	189520.000	0.000	100.000
23	17.561	0.000	0.000	123	2204.000	0.000	100.000	223	220400.000	0.000	100.000
24	22.361	0.000	0.000	124	2563.200	0.000	100.000	224	256320.000	0.000	100.000
25	28.361	0.000	0.000	125	3000.000	0.000	100.000	225	300000.000	0.000	100.000
26	35.861	0.000	0.000	126	3531.200	0.000	100.000	226	353120.000	0.000	100.000
27	45.361	0.000	0.000	127	4176.000	0.000	100.000	227	417600.000	0.000	100.000
28	57.361	0.000	0.000	128	4956.000	0.000	100.000	228	495600.000	0.000	100.000
29	72.361	0.000	0.000	129	5904.000	0.000	100.000	229	590400.000	0.000	100.000
30	89.861	0.000	0.000	130	7064.000	0.000	100.000	230	706400.000	0.000	100.000
31	111.361	0.000	0.000	131	8480.000	0.000	100.000	231	848000.000	0.000	100.000
32	137.361	0.000	0.000	132	10208.000	0.000	100.000	232	1020800.000	0.000	100.000
33	168.361	0.000	0.000	133	12304.000	0.000	100.000	233	1230400.000	0.000	100.000
34	205.361	0.000	0.000	134	14832.000	0.000	100.000	234	1483200.000	0.000	100.000
35	250.361	0.000	0.000	135	17856.000	0.000	100.000	235	1785600.000	0.000	100.000
36	314.361	0.000	0.000	136	21440.000	0.000	100.000	236	2144000.000	0.000	100.000
37	390.361	0.000	0.000	137	25760.000	0.000	100.000	237	2576000.000	0.000	100.000
38	483.361	0.000	0.000	138	30976.000	0.000	100.000	238	3097600.000	0.000	100.000
39	598.361	0.000	0.000	139	37264.000	0.000	100.000	239	3726400.000	0.000	100.000
40	740.361	0.000	0.000	140	44800.000	0.000	100.000	240	4480000.000	0.000	100.000
41	915.361	0.000	0.000	141	53760.000	0.000	100.000	241	5376000.000	0.000	100.000
42	1130.361	0.000	0.000	142	64320.000	0.000	100.000	242	6432000.000	0.000	100.000
43	1392.361	0.000	0.000	143	76720.000	0.000	100.000	243	7672000.000	0.000	100.000
44	1710.361	0.000	0.000	144	91200.000	0.000	100.000	244	9120000.000	0.000	100.000
45	2094.361	0.000	0.000	145	108080.000	0.000	100.000	245	10808000.000	0.000	100.000
46	2554.361	0.000	0.000	146	127840.000	0.000	100.000	246	12784000.000	0.000	100.000
47	3102.361	0.000	0.000	147	150960.000	0.000	100.000	247	15096000.000	0.000	100.000
48	3750.361	0.000	0.000	148	176960.000	0.000	100.000	248	17696000.000	0.000	100.000
49	4512.361	0.000	0.000	149	206400.000	0.000	100.000	249	20640000.000	0.000	100.000
50	5400.361	0.000	0.000	150	240000.000	0.000	100.000	250	24000000.000	0.000	100.000

Fig. 4: It shows Particle Size analysis of F3 formulation

**Zeta Potential:** Zeta potential of the prepared drug loaded Ethyl cellulose nanoparticles were measured using zeta meter. NPs of F3 formulation showed higher stability, bearing a value of -25.2 mV.

**Invitro Drug Release Studies :** Invitro drug release studies were performed to determine the sustained release nature of the formulations. In F2 and F3 formulations, the drug release was continued upto 8 hours. In a period of 8 hours 86.012% and 79.95% of drug has been released from F2 and F3. In F1, the drug release continued upto 4 hours. 98.2% of the drug has been released within a time period of 4 hours. From the various plots mentioned, it can be concluded that the drug release from the nanoparticles of the F1 and F3 formulations obeyed zero order kinetics and F2 formulation

obeyed first order kinetics, all following fickian diffusion mechanism.

**HORIBA SZ100 Z**

**Ibu-EC(1-2).nzt**  
**Measurement Results**  
 Date : 14 May 2014 14:44:34  
 Measurement Type : Zeta Potential  
 Sample Name : Ibu-EC(1-2)  
 Temperature of the holder : 25.0 deg. C  
 Viscosity of the dispersion medium : 0.895 mPa.s  
 Conductivity : 0.217 mS/cm  
 Electrode Voltage : 3.3 V



**Calculation Results**

Peak No.	Zeta Potential	Electrophoretic Mobility
1	-25.2 mV	-0.000195 cm <sup>2</sup> /Vs
2	---	---
3	---	---
Zeta Potential (Mean)	-25.2 mV	---
Electrophoretic Mobility mean	---	-0.000195 cm <sup>2</sup> /Vs

Fig. 5: It shows Zeta Potential of F3 formulation

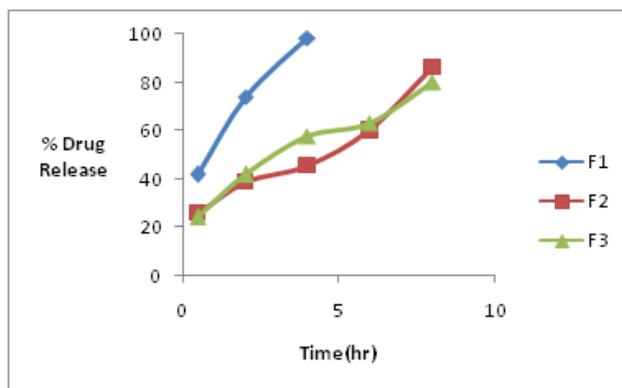


Fig. 6: It shows invitro drug release pattern of NPs of various formulations prepared by nanoprecipitation technique.

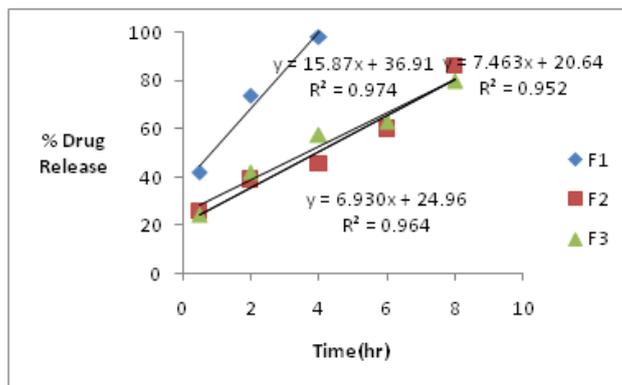


Fig. 7: It shows Zero Order plot of NPs of various formulations prepared by nanoprecipitation technique.

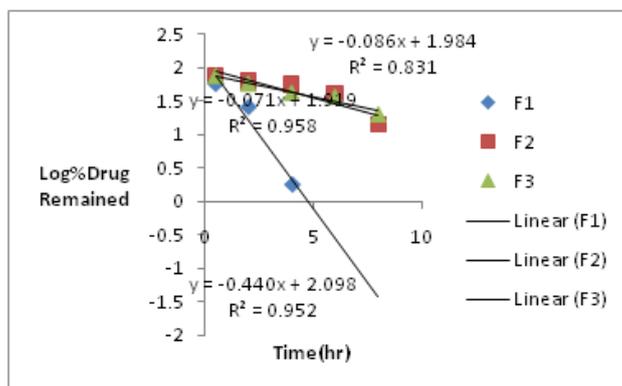


Fig. 8: It shows First Order plot of NPs of various formulations prepared by nanoprecipitation technique.

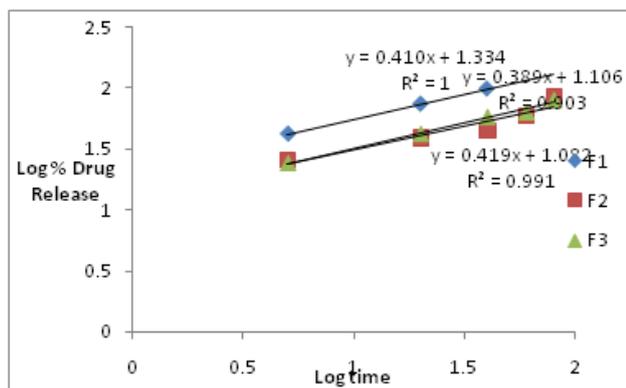


Fig. 9: It shows Peppas plot of NPs of various formulations prepared by nanoprecipitation technique.

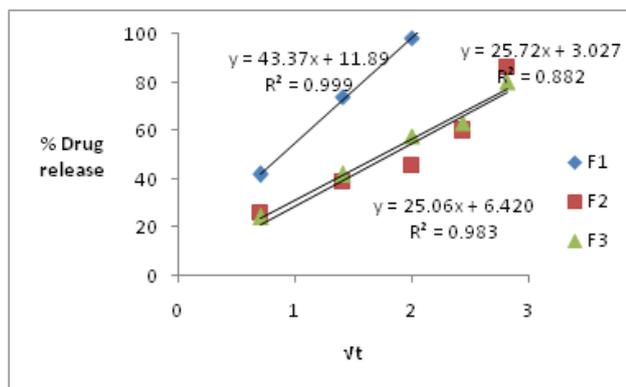


Fig. 10: It shows Higuchi plot of NPs of various formulations prepared by nanoprecipitation technique.

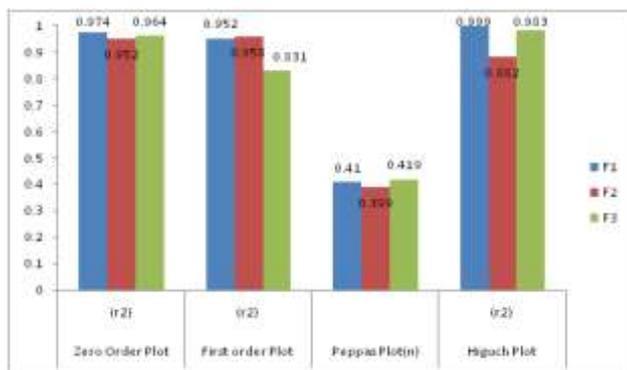


Fig. 11: It shows the parameters determined from the Invitro Release Studies performed on Drug loaded Ethyl cellulose NPs of three different formulations :

## DISCUSSION

In this present study attempts have been made to prepare Ibuprofen loaded EC nanoparticles by nanoprecipitation technique. Ibuprofen is a non-steroidal anti-inflammatory drug used in the treatment of Rheumatoid arthritis and Ankylosing spondylitis. In order to obtain the best formulations, the concentration of polymer and solvents were varied by keeping the concentration of drug constant. Three formulations were prepared by varying the concentration of the polymer and organic solvents. The drug, polymer ratio was maintained as 1:1, 1:1.5, 1:2 in formulation 1, 2, 3 respectively. The effect of the polymer concentration on nanoparticle size, stability, drug content, entrapment efficiency, loading capacity was studied.

On comparing the invitro drug release profile of all the formulations, F1 was showing maximum drug release(98.20%) in a time period of 4 hours. The maximum drug release was may be because of the poor entrapment of the drug. Initial burst release indicated the presence

of the free drug in higher concentrations. In F2 and F3, the drug release was continued upto 8 hours indicating its sustained release properly. When F2 and F3 formulations were compared, maximum amount of drug has been released from F3(86.012%). In F2 and F3, amount of polymer taken was more when compared to drug. The sustained release nature is thought to be mainly because of the higher concentration of polymer to that of drug. Entrapment efficiency was improved by increasing the polymer concentration from 1:1 to 1:1.5 to 1:2.

## CONCLUSION

From the results, it can be concluded that F3 formulation i.e.; in which concentration of drug and polymer bears a ratio of 1:2, is considered to be better than F1 and F2 because of smaller particle diameter(251.1 nm), greater stability(-25.2 mV) and maximum entrapment efficiency(95.8%).

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