ENHANCEMENT OF THE DISSOLUTION RATE OF NATEGLINIDE TABLETS USING LIQUISOLID COMPACT TECHNIQUE

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ABSTRACT

Objective: The main objective of this work is to develop new formulation to enhance the solubility of a highly permeable and a poorly soluble oral drug antihyperglycemic agent, nateglinide by liquisolid compacts.

Methods: The liquisolid compact technique is based on dissolving the insoluble drug in propylene glycol, polyethylene glycol 400, tween-80 as non-volatile solvents to improve dissolution rate of the drug. liquisolid compacts of nateglinide (NTG) using various non-volatile solvents to improve dissolution rate of the drug. The present study was planned with the objective to prepare the liquisolid compacts. Among all formulations, liquisolid system prepared by propylene glycol was considered as best formulation which release drug up to 98% in 60 minutes and in comparison to marketed formulation, optimized formulation showed better dissolution profile.

Result: Higher drug release profiles due to increased wetting property and surface area of the drug available for dissolution was obtained in case of liquisolid compacts. Among all formulations, liquisolid system prepared by propylene glycol was considered as best formulation which release drug up to 98% in 60 minutes and in comparison to marketed formulation, optimized formulation showed better dissolution profile.

Conclusion: It can be concluded that liquisolid compact technique could be a promising strategy in improving the dissolution of poor water soluble drugs.

Keywords: Antihyperglycemic agent, Liquisolid compact technique, Nateglinide, Propylene glycol.

INTRODUCTION

One of the novel methods for promoting dissolution is the formation of liquisolid compacts. Liquisolid compact formulation mainly includes non-volatile solvent, disintegrant, drug candidate, carrier material, and coating material [1].

In this technique, liquid may be transformed into a free flowing, readily compressible, and apparently dry powder with the liquisolid technology by simple physical blending with selected excipients named as carrier and coating material. The liquid portion, which can be a liquid drug, a drug suspension or a drug solution in suitable non-volatile liquid vehicles, is incorporated into the porous carrier material [2]. Preferably, water-miscible organic solvent systems with high boiling point such as propylene glycol, liquid polyethylene glycols (PEGs), or glycerine are best suitable as liquid vehicles. Once, the carrier is saturated with liquid, a liquid layer is formed on the particle surface which is instantly adsorbed by the fine coating particles. Thus, an apparently dry, free flowing, and compressible powder is obtained. Usually, microcrystalline cellulose (MCC) is used as carrier material and amorphous silicon dioxide (colloidal silica) as coating material. Fig. 1 represents the schematic representation of a liquisolid system [3].

Practically water-insoluble liquid and solid drugs can be formulated into liquisolid systems using the new formulation-mathematical model.

The present study was planned with the objective to prepare the liquisolid compacts of nateglinide (NTG) using various non-volatile solvents to improve dissolution rate of the drug.

NTG has been exploited as a new class of oral antidiabetic agent used in the management of Type 2 diabetes mellitus [4] (non-insulin-dependent diabetes mellitus) (Fig. 2). It belongs to the meglinitide class of short-acting insulin secretagogues. NTG is an amino acid derivative of D-phenylalanine which stimulates the secretion of insulin by binding to the adenosine triphosphate potassium channels in pancreatic beta cells. It induces an early insulin response to meals decreasing postprandial blood glucose levels [5]. It should only be taken with meals and meal-time doses should be skipped with any skipped meal. Its empirical formula is C_{19}H_{23}NO, and molecular weight is 317.4226. Literature survey was performed on different liquisolid compacts such as repaglinide [6,7], famotidine [8], fenofibrate [9], gliburide [10], and efavirenz [11].

MATERIALS AND METHODS

Materials
NTG was gift sample from Glenmark Pharmaceuticals. Propylene glycol and PEG 400 were obtained from India glycols limited, Hyderabad. Tween 80, aerosol, MCC, crospovidone, and magnesium stearate were procured from S.D. Fine Chemicals Ltd.

Methods
Pre-formulation studies
Drug-excipient compatibility studies [12,13]
In the preparation of tablet formulation, drug and excipients may interact as they are in close contact with each other, which could lead to the instability of drug. Fourier-transform infrared (FT-IR) spectroscopy (FT-IR spectroscopy, Shimadzu, Japan) was employed to ascertain the...
compatibility between drug and the selected excipients. The pure drug and drug with excipient were scanned separately.

FT-IR spectroscopy
The functional group analysis for the excipients is done using the FT-IR method analysis. Initially, the samples were made into pellets using a pelletizer under a pressure of 100 kg/cm$^2$. A blank potassium bromide (KBr) pellet is made, and then, a few mg of sample is mixed with KBr and made into pellet. All the pellets are analyzed by FT-IR instrument, and the data are processed using FT-IR system in the wave number range of 4000-400 cm$^{-1}$.

Analytical method development
Preparation of phosphate buffer pH 6.8 solution
50 ml of the 0.2 M monobasic potassium phosphate solution was taken in a 200 ml volumetric flask and 22.4 ml of 0.2 M sodium hydroxide solution was added to it, and then, water was used to make up the volume.

Determination of $\lambda_{\text{max}}$ of NTG in phosphate buffer pH 6.8 solution
Working standard
100 mg of NTG was weighed and dissolved in 5 ml methanol, and then, the volume was made up to 100 ml with phosphate buffer pH 6.8 solution to give 1000 µg/ml concentrated stock solution.

Dilution 1: From the working standard solution 10 ml was diluted to 100 ml with phosphate buffer pH 6.8 solution to give 100 µg/ml concentrated solutions.

Dilution 2: From dilution-1, 10 ml solution was diluted to 100 ml with phosphate buffer pH 6.8 solutions to give 10 µg/ml concentrated solutions.

This solution was scanned at a range of 200-400 nm wavelengths. The corresponding scan spectrum curve was noted and the wavelength having highest absorbance is noted as $\lambda_{\text{max}}$, 217 nm.

Construction of calibration curve of NTG in phosphate buffer pH 6.8 solution
From dilution-1, 0.2, 0.4, 0.6, 0.8, and 1 ml of solutions were taken and were made up to the mark in 10 ml volumetric flask to obtain 2, 4, 6, 8, and 10 µg/ml concentrated solutions. The absorbance of these solutions was noted at $\lambda_{\text{max}}$, 217 nm.

Formulations of NTG liquisolid compacts are shown in Table 1.

Pre-compression studies [14]
Bulk density
An accurately weighed sample of powder was carefully added to the measuring cylinder with the aid of funnel. The level was observed without compacting and noted as apparent volume ($V_a$). The bulk density ($D_b$) was calculated by the formula as given below:

$$D_b = \frac{M}{V_0}$$

Where, $M$=Mass of powder taken, $V_0$=Apparent untapped volume.

Tapped density
It is the ratio of total mass of powder to the tapped volume of powder. The volume was measured by tapping the powder for 500 times. Then, the tapping was done for 750 times and the tapped volume was noted (the difference between these two volumes should be <2%). If it is more than 2%, tapping is continued for 1250 times and tapped volume was noted. It is expressed in g/cc and is given by formula:

$$\text{Tapped density} = \frac{\text{Weight of powder}}{\text{tapped volume}}$$

Carr’s index
The percentage compressibility of powder is direct measure of the potential of powder arch or bridge strength. It is calculated according to the equation given below:

$$\text{Compressibility index} = (\text{Tapped density} - \text{bulk density})\times100/\text{Tapped density}$$

Table 1: Composition of nateglinide liquisolid compacts

<table>
<thead>
<tr>
<th>Ingredients</th>
<th>Formulations (mg/tab)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>F1</td>
</tr>
<tr>
<td>Nateglinide</td>
<td>60</td>
</tr>
<tr>
<td>Propylene glycol</td>
<td>40</td>
</tr>
<tr>
<td>Tween 80</td>
<td>-</td>
</tr>
<tr>
<td>PEG 400</td>
<td>-</td>
</tr>
<tr>
<td>MCC</td>
<td>225</td>
</tr>
<tr>
<td>Aerosil</td>
<td>10</td>
</tr>
<tr>
<td>MCC</td>
<td>50</td>
</tr>
<tr>
<td>Crospovidone</td>
<td>10</td>
</tr>
<tr>
<td>Magnesium stearate</td>
<td>2</td>
</tr>
<tr>
<td>Tablet weight (mg)</td>
<td>397</td>
</tr>
</tbody>
</table>

NTG: Nateglinide, PEG: Polyethylene glycol, MCC: Microcrystalline cellulose
Bulk density

disintegration test for prepared dissolution of NTG

weight variation = was within permissible limits or not. The weight was then compared with average weight to assure whether it from the collective weight, average weight was calculated. Each Twenty Weight variation [16]

evaluation of formulated table ets. Main advantages of direct compression are low manufacturing cost and high mechanical integrity of the tablet [15].

1. NTG drug was initially dispersed in the non-volatile solvent systems (tween-80, PEG 400) termed as liquid vehicles with the different drug: Vehicle ratio.

2. Carrier, MCC was added to the above liquid preparation by continuous mixing for 10-20 minutes in a mortar to evenly distribute liquid medication into powder.

3. To the above mixture aerosil, as coating material and remaining quantity of MCC was added and mixed thoroughly.

4. Mixture of crospovidone, disintegrant, and other remaining additives such as lubricant, magnesium stearate are added, and mixed in a mortar.

5. The final mixture was punched into tablet using 10 mm diameter punch.

Direct compression method

Direct compression method was used for the formulation of NTG tablets. The Hausner’s ratio is calculated by the formula as given below: Hausner’s ratio = Tapped density / Bulk density

Angle of repose

It is defined as the maximum angle possible between the surface of a pile of powder and the horizontal plane. Angle of repose was calculated using the following formula.

\[ \theta = \tan^{-1} \left( \frac{h}{r} \right) \]

Where, \( \theta \) = Angle of repose, \( h \) = Height (cm), \( r \) = Radius (cm).

The angle of repose has been used to characterize the flow properties of solids. It is a characteristic related to inter particulate friction or resistance to movement between particles.

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5. The final mixture was punched into tablet using 10 mm diameter punch.

Evaluation of formulated tablets

Weight variation [16]

Twenty tablets were selected and weighed collectively and individually. From the collective weight, average weight was calculated. Each tablet weight was then compared with average weight to assure whether it was within permissible limits or not.

\[ \% \text{ weight variation} = \frac{\text{Average weight} - \text{weight of each tablet}}{\text{Average weight}} \times 100 \]

Thickness

Thickness of the tablets was determined using vernier calipers.

Hardness test

Hardness of the tablet was determined using the Monsanto hardness tester. The lower plunger was placed in contact with the tablet and a zero reading was taken. The plunger was then forced against a spring by turning a threaded bolt until the tablet fractured. As the spring was compressed a pointer rides along a gauge in the barrel to indicate the force.

Friability [17]

Friability of the tablets was checked using Roche Friabilator. The device subjects a number of tablets to the combined effect of abrasions and shock by utilizing a plastic chamber that revolves at 25 rpm dropping the tablets from a height of 6 inches with each revolution. Pre-weighed sample tablets were placed in the friabilator, which was then operated for 100 revolutions. Tablets were dusted and reweighed. The difference in the weight is noted and expressed as percentage.

It should be preferably between 0.5% and 1.0%.

Friability = \( \frac{[(W_s - W_f)/W_s] \times 100}{100} \)

Where, \( W_s \) = Weight of tablets before test, \( W_f \) = Weight of tablets after test.

Content uniformity test [18]

Ten tablets were weighed and powdered, a quantity of powder equivalent to 10 mg of NTG was transferred to a 100 ml volumetric flask and 10 ml methanol is added. The drug is extracted in methanol by vigorously shaking the stopped flask for 15 minutes. Then, the volume is adjusted to the mark with phosphate buffer pH 6.8 and the liquid is filtered. From prepared solution take 0.1 ml solution in 10 ml volumetric flask and makeup to mark with phosphate buffer pH 6.8. The NTG content was determined by measuring the absorbance at 217 nm after appropriate dilution. The drug content was calculated using the standard calibration curve. The mean percent drug content was calculated as an average of three determinations.

In vitro disintegration study [19-21]

The in vitro disintegration test for prepared tablets was carried out using USP disintegration test apparatus. Six tablets were placed individually in each tube of disintegration test apparatus, and discs were placed over each tablet. Distilled water was used as the medium which is maintained at 37±2°C and the time taken for each tablet to disintegrate completely was recorded.

In vitro dissolution rate [22]

In vitro dissolution of NTG tablets was studied in USP XXIII Type 2 dissolution apparatus employing a paddle stirrer at 50 rpm. 900 ml of phosphate buffer pH 6.8 was used as dissolution medium. The temperature of dissolution medium was maintained at 37 ± 0.5°C throughout the experiment. Samples of dissolution medium (5 ml) were withdrawn by means of syringe fitted with pre-filter at known intervals of time (5, 10, 15, 20, 30, 40, 45, and 60 minutes) and analyzed for drug release by measuring the absorbance at 217 nm. The volume withdrawn at each time interval was replaced with fresh quantity of dissolution medium. Cumulative percent NTG released was calculated and plotted against time.

RESULTS

Pre-formulation studies

Construction of standard calibration curve of NTG in phosphate buffer pH 6.8

The absorbance of the solution was measured at 217 nm, using UV spectrophotometer with phosphate buffer pH 6.8 as blank. A graph
of absorbance versus concentration was plotted which indicated in compliance to Beer’s law in the concentration range 2-10 µg/ml.

Standard plot of NTG was plotted by taking absorbance on Y-axis and concentration (µg/ml) on X-axis; the plot is shown in Fig. 3.

The standard calibration curve of NTG pH 6.8 phosphate buffers showed good correlation with regression value of 0.999.

**Drug excipient compatibility studies (FT-IR spectroscopy) (Figs. 4 and 5)**

The FTIR spectrum of pure NTG showed an absorption band at 2924 cm⁻¹ (aliphatic -H stretching, asymmetric), 2859 cm⁻¹ (aliphatic CH stretching, symmetric), 1636 cm⁻¹ (C=O stretching for ketone), and 3086 cm⁻¹ (aromatic C–H stretching). Drug and excipients absorption bands were identified and interpreted in the spectra. The FT-IR spectra of physical mixtures of drug and excipients reveal no interaction between drug and excipients. The FT-IR studies from the spectra confirmed the absence of any chemical interaction between the drug and the excipients.

**Pre-compression studies**

The prepared powders were evaluated for their flow properties; the results for the blends of compression tablets were shown in Table 2.

The bulk density for all formulations was found to be in range 0.82-0.96 kg/cm³ and the tapped density for all formulations was found to be in range 0.88-1.11 kg/cm³.

The Carr’s index and Hausner’s ratio were found to be in the range of <16 and 1.07-1.18, respectively, indicating good flow and compressibility of the blends.

The angle of repose for all the formulations was found to be 25.3-35.6 which indicates passable flow (i.e., incorporation of glidant will enhance its flow). Hence, prepared powders were compressed into tablets and evaluated.

**Post-compression studies (Table 3)**

The variation in weight was within the limits complying with pharmacopeia specifications of USP. The hardness for different formulations was found to be between 2.9 and 3.2 kg/cm², indicating satisfactory mechanical strength. The friability was <1.0% for all the formulations, which is an indication of good mechanical resistance of the tablet.

The drug content was found to be within limits 98.2-101.2%. Disintegration time for all the formulations was found to be 21-34 seconds.

### Table 2: Pre-compression studies of nateglinide liquisolid formulations

<table>
<thead>
<tr>
<th>Formulation code</th>
<th>Bulk density (g/cc)</th>
<th>Tapped density (g/cc)</th>
<th>Carr’s index</th>
<th>Hausner’s ratio</th>
<th>Angle of repose (°)</th>
</tr>
</thead>
<tbody>
<tr>
<td>F1</td>
<td>0.96±0.52</td>
<td>1.06±0.14</td>
<td>9.6±3.8</td>
<td>1.11±0.3</td>
<td>27.3±2.9</td>
</tr>
<tr>
<td>F2</td>
<td>0.86±0.23</td>
<td>0.98±0.13</td>
<td>12.1±0.4</td>
<td>1.14±0.8</td>
<td>31.2±1.2</td>
</tr>
<tr>
<td>F3</td>
<td>0.85±0.36</td>
<td>0.98±0.24</td>
<td>13.6±0.9</td>
<td>1.16±0.17</td>
<td>35.6±1.4</td>
</tr>
<tr>
<td>F4</td>
<td>0.94±0.44</td>
<td>1.11±0.33</td>
<td>15.1±0.8</td>
<td>1.18±0.28</td>
<td>29.6±2.6</td>
</tr>
<tr>
<td>F5</td>
<td>0.89±0.52</td>
<td>1.04±0.52</td>
<td>14.3±0.6</td>
<td>1.17±0.6</td>
<td>25.3±2.8</td>
</tr>
<tr>
<td>F6</td>
<td>0.82±0.66</td>
<td>0.88±0.29</td>
<td>6.6±1.4</td>
<td>1.07±0.1</td>
<td>29.2±1.9</td>
</tr>
<tr>
<td>F7</td>
<td>0.85±0.39</td>
<td>0.96±0.28</td>
<td>11.9±0.5</td>
<td>1.13±0.5</td>
<td>31.6±1.7</td>
</tr>
<tr>
<td>F8</td>
<td>0.91±0.64</td>
<td>1.02±0.76</td>
<td>10.9±0.34</td>
<td>1.12±0.5</td>
<td>29±1.5</td>
</tr>
<tr>
<td>F9</td>
<td>0.89±0.48</td>
<td>1.04±0.85</td>
<td>14.3±0.8</td>
<td>1.17±0.2</td>
<td>25.3±1.3</td>
</tr>
</tbody>
</table>

**Fig. 3: Calibration curve for nateglinide in 6.8 phosphate buffer**

**Fig. 4: Fourier-transform infrared spectra of nateglinide**

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*Mamatha and Sultana*  
Dissolution tests were performed for formulations F1-F9. From in vitro release study, it has been observed that the formulations F2, F3 showed higher drug release indicating that increase in non-volatile solvent concentration increases the dissolution of drug (Fig. 6). From in vitro release study for tween 80 used formulations, it has been observed that the formulation F6 showed higher drug release indicating that increase in non-volatile solvent concentration increases the dissolution of drug (Fig. 7).

The results indicated that the increase in concentration of solubility enhancing agent will increase the dissolution of drug. Among all the formulations, F2 was selected as an optimized formulation because it shows higher drug release at less concentration of propylene glycol than other formulations. Based on mathematical data, it was concluded that the release data were best fitted with first order kinetic and follows Higuchi model.

The optimized formulation dissolution profile was compared with market formulation dissolution profile (Fig. 9).

From in vitro release study of PEG 400 used formulations, it has been observed that the formulations F9 showed higher drug release indicating that increase in non-volatile solvent concentration increase the dissolution of drug (Fig. 8).

The results indicated that the increase in concentration of solubility enhancing agent will increase the dissolution of drug. Among all the formulations, F2 was selected as an optimized formulation because it shows higher drug release at less concentration of propylene glycol than other formulations. Based on mathematical data, it was concluded that the release data were best fitted with first order kinetic and follows Higuchi model.

The optimized formulation dissolution profile was compared with market formulation dissolution profile (Fig. 9).

From dissolution data, it was observed that more than 90% of the drug were released from both liquisolid and marketed formulation in 60 minutes in phosphate buffer pH 6.8.

DISCUSSION

Liquisolid compact technology is one of the advanced methods of formulation for poor dissolving drugs. This type of formulation includes drug candidate, non-volatile solvent, disintegrant, carrier, and coating material. Liquisolid compact technology produces dry, free flowing, and compressible powders. Like glibenclamide, NTG also belongs to Biopharmaceutical Classification System Class II [23].

**Table 3: Post-compression studies of nateglinide liquisolid compacts**

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Weight variation</th>
<th>Hardness (kg/cm²)±SD</th>
<th>Thickness (mm)±SD</th>
<th>Friability (%)±SD</th>
<th>Drug content (%)±SD</th>
<th>Disintegration time (s)±SD</th>
</tr>
</thead>
<tbody>
<tr>
<td>F1</td>
<td>Pass</td>
<td>2.9±0.8</td>
<td>4.3±0.18</td>
<td>0.82±0.07</td>
<td>99.1±0.21</td>
<td>34±0.028</td>
</tr>
<tr>
<td>F2</td>
<td>Pass</td>
<td>3.2±0.16</td>
<td>4.7±0.2</td>
<td>0.48±0.04</td>
<td>98.5±0.13</td>
<td>25±0.042</td>
</tr>
<tr>
<td>F3</td>
<td>Pass</td>
<td>3.1±0.9</td>
<td>4.4±0.7</td>
<td>0.67±0.08</td>
<td>98.1±0.45</td>
<td>21±0.031</td>
</tr>
<tr>
<td>F4</td>
<td>Pass</td>
<td>2.9±0.4</td>
<td>4.6±0.5</td>
<td>0.33±0.04</td>
<td>101.2±0.37</td>
<td>28±0.014</td>
</tr>
<tr>
<td>F5</td>
<td>Pass</td>
<td>3.0±0.24</td>
<td>4.3±0.7</td>
<td>0.95±0.03</td>
<td>99.5±0.67</td>
<td>24±0.018</td>
</tr>
<tr>
<td>F6</td>
<td>Pass</td>
<td>3.2±0.31</td>
<td>4.6±0.6</td>
<td>0.34±0.02</td>
<td>100.2±0.12</td>
<td>30±0.035</td>
</tr>
<tr>
<td>F7</td>
<td>Pass</td>
<td>3.1±0.5</td>
<td>4.4±0.4</td>
<td>0.82±0.04</td>
<td>98.6±0.31</td>
<td>32±0.045</td>
</tr>
<tr>
<td>F8</td>
<td>Pass</td>
<td>3.0±0.32</td>
<td>4.7±0.9</td>
<td>0.65±0.06</td>
<td>98.2±0.67</td>
<td>28±0.062</td>
</tr>
<tr>
<td>F9</td>
<td>Pass</td>
<td>3.1±0.22</td>
<td>4.4±0.3</td>
<td>0.42±0.08</td>
<td>99.3±0.45</td>
<td>31±0.035</td>
</tr>
</tbody>
</table>

SD: Standard deviation
Solubility studies were conducted like that of Sirisha et al. for enhancement of dissolution of glibenclamide [23]. We have selected propylene glycol, tween 80, and PEG 400 as non-volatile solvents.

NTG was formulated in triplicate. F1-F3 used propylene glycol, F4-F6 used tween 80 whereas F7-F9 used PEG 400 as non-volatile solvents. It used MCC as carrier, aerosil as coating material, crospovidone as disintegrant and magnesium stearate as lubricant. Propylene glycol was used as surfactant/cosurfactant by Maghraby et al. [15] to increase the dissolution of repaglinide drug [7].

In the pre-formulation study, initially, NTG drug solution was checked for obeying Beer's law. It was observed that drug solution in the range of 2-10 µg/ml obeyed Beer's law at wavelength of 217 nm. To check drug-excipient compatibility, which is a major step in the process of formulating tablets FT-IR study was carried out. It was done in the wave number range of 4000-400 cm\(^{-1}\). From the FT-IR absorption bands, it was interpreted and confirmed that there is no interaction between drug NTG and other excipients.

Pre-compression studies for all the nine formulations, i.e., F1 to F9 were carried out. The results of bulk density, Carr's ratio, Hausner's ratio, and angle of repose for all the formulations were found to be within pharmacopeial specified limits. Hence, the prepared powders could be compressed and were further evaluated for post compression studies.

Post-compression studies included evaluation for weight variation, hardness, thickness, friability, and drug content along with assessment of disintegration time. All the above said post-compression parameters were found to be within specified pharmacopeial limits. Finally, tablets developed with minimum weight variation, sufficient mechanical strength, and less disintegration time.

Pre- and post-compression study was done similar to that of Rosuvastatin by Neelamma et al. [24] and glibenclamide by Sirisha et al. [23].

For all the 9 formulations in vitro dissolution study was carried out. Among the first three formulations which had used as non-volatile solvent F2 and F3 showed better results. In the next three formulations (F4-F6) using tween 80 as solvent, F6 was preferred. In the last three formulations (F7-F9) using PEG 400 as solvent, F9 was selected. From the above-selected formulations, it can be inferred that higher drug release can be achieved with increase in non-volatile solvent concentration.

From the above-preferred formulations, F2 was optimised for further study. Its dissolution profile was compared with that of the marketed formulation. From the dissolution profiles of optimized and marketed formulation it was concluded that optimized formulation was equally or better releasing the drug as to that of marketed formulation.

The reason for better dissolution rate of optimized formulation can be attributed to the drug presenting in a solubilized state in the formulation (liquisolid formulation), which contributes to increased wetting properties, thereby enhancing the dissolution rate. The results also hinted that with the increase in solubility enhancing agent, dissolution of the drug increases.

CONCLUSION

The research work done for the novel formulation of high permeable and low solubility antihyperglycemic drug NTG by liquisolid compact technology was successful. As the drug will be presented in a state of molecular dispersion, the formulation disintegrates in dissolution media. This will increase the effective surface area of the particles available for dissolution. Parison to marketed formulation our optimized formulation showed better dissolution profile. Hence, the liquisolid compact is the promising tool for enhancement of solubility of water insoluble drug.

ACKNOWLEDGMENT

The authors are thankful to Glenmark pharmaceuticals for providing the pure drug, NTG as gift sample and to the management of Sultan-ul-Uloom College of Pharmacy for providing necessary facilities to carry out the research work.

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