

FORMULATION AND DEVELOPMENT OF *IN SITU* FORMING GEL FOR THE TREATMENT OF ORAL THRUSH

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ABSTRACT

Objective: The objective of the present work was to develop an *in situ* gel composed of Pluronic F-127, Carbopol 934, and methylparaben and loaded with fluconazole using DoE software to sustain the delivery of drug in the buccal cavity.

Methods: *In situ* gels were prepared by temperature-induced method, by employing DoE and characterized by Fourier transform infrared (FTIR), differential scanning calorimeter (DSC), and evaluated for gelation temperature, gelation time, adhesive force, and *in vitro* diffusion studies.

Results: Both FTIR and DSC studies suggested that there were no chemical interactions present between both drug and polymers. The formulated gels S1, S3, and S9 showed gelation at a body temperature. The viscosity, gel strength, and mucoadhesive force for the formulated *in situ* gels were found to be within the ranges of 375–738 cps, 35–62 s, and 4650–5210.32 dynes/cm², respectively. The *in vitro* diffusion studies indicated that optimized *in situ* gel S3 exhibited the improved ability to sustain the drug compared to other formulations.

Conclusion: Thus, developed *in situ* gel system was determined to be effective in terms of eradication of oral thrush.

Keywords: *In situ* gel, Pluronic F-127, Carbopol 980, Fluconazole, Oral thrush.

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INTRODUCTION

Oral thrush is defined as a yeast or fungal infection caused by *Candida albicans*, generally observed in oral cavities of babies and elderly people with dentures [1]. These fungal organisms are present in oral cavity within a wide range of population; changes in the environment of oral cavity lead to these fungal infections, other factors that trigger these fungal infections are hyposalivation, usage of immune suppressants, and radiation therapy to cure diseases [2]. To treat these fungal infections, conventional formulations such as gels, torches, creams, mouth paints, rinses, and suspensions are used to deliver the drug locally into the oral cavity. These formulations are also used to treat various conditions such as bacterial infections, fungal infections, periodontal disease, toothache, and dental caries [3].

Degradation of drugs in the oral cavity salivary fluid causes incomplete eradication of candidiasis. The delivery of drugs locally in the oral cavity will result in improved efficacy to eliminate the infection. The antifungal drugs with enhanced stability and more residence time will permit to penetrate through the tissue membrane of buccal cavity to act on *Candida* species for extended period [4,5]. To deliver the drug locally in the buccal cavity in this research work, *in situ* gel was selected as vehicle to deliver the drug due to its various advantages such as reduced dose frequency, and enhanced patient comfort and compliance [6,7].

Fluconazole is a wide-spectrum antifungal drug belonging to the class of imidazole derivatives. Fluconazole shows its action by bonding with lanosterol 14- α -dimethylase and inhibits the production of ergosterol, in turn, leading to loss of integrity in the fungal cell membrane. In addition to this, it also decreases the binding of fungal cells to the host tissue and prohibits the multiplication and growth of fungi [8].

The main interest of the current study is to formulate thermoreversible *in situ* gels using Carbopol-934 and Pluronic F-127, for release of Fluconazole to treat candidiasis in the oral cavity. Hence, the systemic side effects can be reduced, improve the therapeutic efficacy and patient acceptance.

MATERIALS AND METHODS

Materials

Fluconazole was obtained as a gift sample from Bayer Pharmaceutical Pvt., Ltd, Thane, India, and Pluronic F-127 was obtained as a gift sample from Triveni Interchem Pvt., Ltd, Vapi, India.

Methods

Formulation and optimization of temperature-induced *in situ* gel loaded with fluconazole.

Experimental design

A 3² randomized full factorial design for the study of *in situ* gel at two factors and three levels. Factors included in the study Pluronic F-127 and Carbopol-934 are used as independent variables, whereas levels -1 and +1 were used as low and high, respectively. Viscosity, pH, and gelation time were used as dependent variables. Best fit model for statistical analysis was considered significant when p value was <0.05. Design-Expert software (DX11) State-Ease Inc., USA, was used to study the effect of different variables dependent on the properties of viscosity, pH, and gelation time [9].

Formulation of temperature-induced *in situ* gel loaded with fluconazole

Thermoreversible *in situ* gels were prepared using cold technique; this process involves slow addition of Pluronic F-127 and methylparaben in a sufficient quantity of cold distilled water. The required quantity

of Carbopol 934 was taken in another beaker and allowed it to swell for overnight. Polymer solutions were stirred until uniform solutions were obtained using a magnetic stirrer (Remi, India). The mixture was then kept at room temperature for 24 h. To adjust the pH to 7, a little quantity of triethanolamine was added. Fluconazole was weighed and solubilized in dimethylsulfoxide by stirring continuously until a uniform drug solution was formed. Drug solution was incorporated into gel before *in vitro* studies [1]. The different variables and compositions of thermoreversible gels obtained from DoE were given in Tables 1 and 2.

Characterizations

Fourier transform-infrared (FTIR) studies

The nature of drug-excipient interacting forces during gelation process was characterized using FTIR by employing potassium bromide pellet method [10].

Differential scanning calorimetry

All differential scanning calorimeter (DSC) studies of pure drug and physical mixture were done using Shimadzu DSC-TSW 60. A few mg of sample were entirely sealed into aluminum crimp pan cells. Under nitrogen atmosphere, it was heated at constant temperature of 10°C/min [10].

Evaluation of prepared *in situ* gels

Visual appearance and clarity

The formulated gels were examined for visual appearance and clarity by observing the formulated *in situ* gels against a white and black background to check the presence of any particulate matter [11].

pH

The most accurate common means of measuring pH are through a laboratory device called a probe pH meter. Measurement is made by submerging the probe in the liquid until a reading is registered by the meter [12,13].

Viscosity

Viscosity of all formulated *in situ* gels was done using Brookfield viscometer using spindle no. 6 at 30 rpm, at two different temperatures, namely 8±1°C and 37±1°C [12,14].

Gelation temperature and gelation time

Evaluation of gelation temperature and gelation time was done by taking required quantity of gelling a thin-walled test tube and places it in a thermostatically controlled water bath with frequent shaking until it got converted to gel. Complete gelation was confirmed by tilting the test tube upside down, where the gel does not flow out. The gel formation was evaluated visually and gelation time was observed [12,15].

Determination of mucoadhesive force

Mucoadhesive force can be termed as strength required to disconnect the formulated gel from oral mucosa. Mucoadhesive force was determined using modified balance technique. This method was done using chicken mucosa and two vials. Tissue specimen with appropriate thickness and surface area was taken from chicken mucosa and tied to each side of vial using thread and stored at 32–34°C for about 15 min. Weighing balance was attached to one of the vials and specified quantity of gel was positioned between the tissue specimens attached to bottom of the vials. The force required to detach the gel from mucosa was measured [16].

In vitro diffusion studies

The *in vitro* diffusion study of the formulated *in situ* gel was performed by modified USP dissolution apparatus-1. A Whatman filter paper was taken in the basket and wetted by dipping in simulated lacrimal fluid for a time period of at least 1 min to ensure the contact of release

medium with formulation. 100 µl of the formulation was applied to the Whatman filter paper and 50 ml of simulated lacrimal fluid was filled in a beaker and basket was rotated over its surface. At regular intervals, 3 ml samples were withdrawn replaced with an equal amount of fresh simulated lacrimal fluid. The samples were analyzed spectrophotometrically for fluconazole content using ultraviolet (UV)-visible spectrophotometer (Shimadzu UV-1800) at 286 nm [17,18].

RESULTS AND DISCUSSION

Characterization

FTIR studies

The IR spectra of pure drug Fluconazole were compared with the IR spectra of physical mixture. The comparison between two spectra

Table 1: Variables in 3² factorial design of fluconazole loaded *in situ* gels

Variables	Low (%)	High (%)
Pluronic F-127 (X1)	12	15
Carbopol 934 (X2)	0	0.04

Table 2: 3² factorial design layout for fluconazole loaded *in situ* gels

Run	Pluronic F-127 (X1)/factor 1 (ml)	Carbopol 934 (X2) factor 2 (mg)
1	15	0.02
2	15	0
3	15	0.04
4	13.5	0
5	13.5	0.04
6	13.5	0.02
7	12	0.02
8	12	0.04
9	12	0

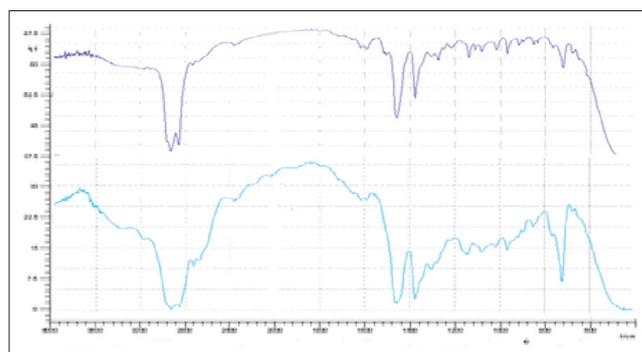


Fig. 1: Fourier transform-infrared spectra of pure drug and drug-excipient mixture

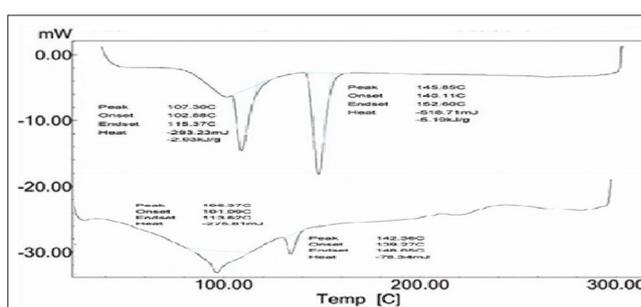


Fig. 2: Differential scanning calorimeter of pure drug and physical mixture

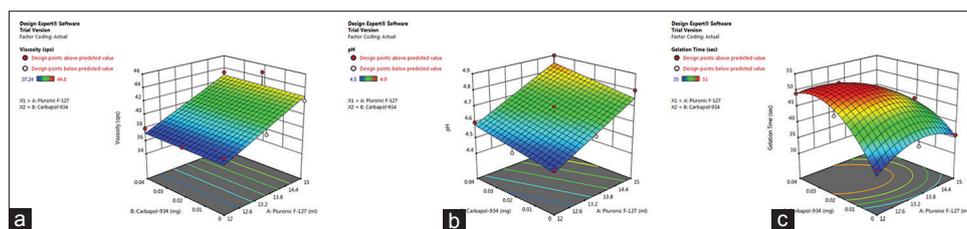


Fig. 3a-c: Three-dimensional response surface plot depicting the impact of factors over responses

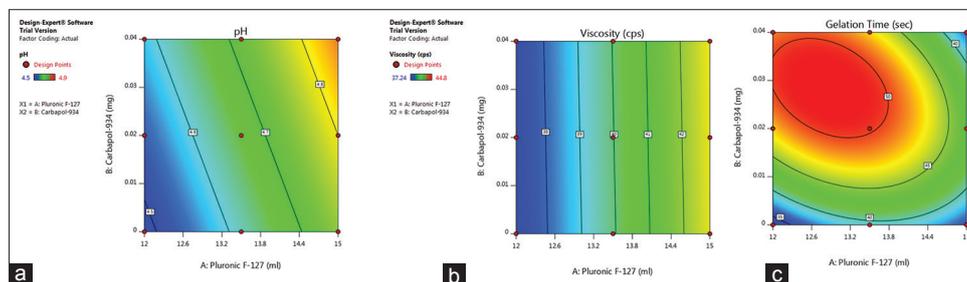


Fig. 4a-c: Contour plot showing the impact of the impact of factors over responses

Table 3: Observed response in 3² factorial design for temperature-induced *in situ* gel loaded with fluconazole

Std.	Run	Pluronic F-127 (X1)/factor 1 (ml)	Carbapol-934 (X2) Factor 2 (mg)	Response Y1 pH	Response Y2 viscosity (cps)	Response Y3 gelation time (s)
6	1	15	0.02	4.7	44.8	36
3	2	15	0	4.8	42.1	44
9	3	15	0.04	4.9	43.3	35
2	4	13.5	0	4.6	39.09	37
8	5	13.5	0.04	4.7	38.3	49
5	6	13.5	0.02	4.7	39.02	51
4	7	12	0.02	4.5	37.24	46
7	8	12	0.04	4.6	37.92	49
1	9	12	0	4.5	38	35

Table 4: Results of regression analysis for responses

Responses	Value	F-value	p-value
pH			
R ²	0.8690	19.91	<0.0022
Adjusted R ²	0.8254		
Predicted R ²	0.7016		
Adequate precision	11.4891		
Viscosity			
R ²	0.8211	13.77	0.0057
Adjusted R ²	0.7615		
Predicted R ²	0.6223		
Adequate precision	7.5647		
Gelation time			
R ²	0.9489	11.15	0.0374
Adjusted R ²	0.8638		
Predicted R ²	0.3955		
Adequate precision	8.4959		

was studied, and it was observed that there was no interaction between pure drug and drug-excipients mixture which was depicted in Fig. 1.

Differential scanning calorimetry

It was evident that DSC of physical mixture and pure drug showed endothermic peak corresponding to fluconazole around 145.85°C as depicted in Fig. 2. Hence, from the results, it was inferred that there was no interaction between the pure drug and physical mixture.

Formulation and optimization of temperature induced *in situ* gel loaded with fluconazole

From the results depicted in Table 3, it was evident that variables that have chosen have a strong impact on responses. On application of factorial design, the following regression equations were obtained. In which negative values indicate negative effect of a specific variable on the response factor and positive value indicates positive effect of a specific variable.

$$pH = +3.41667 + 0.088889 \text{ Pluronic F-127} + 2.5 \text{ Carbapol-934}$$

$$\text{Viscosity} = +14.35944 + 1.89333 \text{ Pluronic F-127} + 2.75000 \text{ Carbapol-934}$$

$$\text{Gelation Time} = -363.52778 + 58.83333 \text{ Pluronic F-127} + 2579.16667 \text{ Carbapol-934}$$

ANOVA studies suggested that all the models were significant for the responses shown which were depicted in Table 4, and polynomial regression results were expressed using three-dimensional graphs and contour plots which were depicted in Figs. 3a-c and 4a-c.

Optimization

To design the optimized *in situ* gel, required response values were depicted in Table 5. The combination which resulted in achieving the required specifications was done using the design expert software. To validate the obtained model, the obtained results were overlapped with predicted results.

Table 5: Optimization of temperature-induced *in situ* gel loaded with fluconazole

Value	Pluronic F-127 (ml)	Carbapol-934 (mg)	Response pH	Response viscosity (cps)	Response gelation time (s)
Predicted	14.932	0.03	4.9	43.3	35
Actual	14.82	0.03	4.9	43.1	36
% error	0.112	-	-	0.2	1

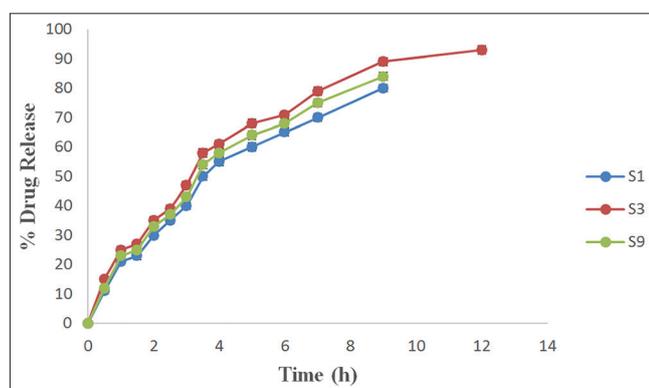
Table 6: Results of evaluated physicochemical parameters

Tests	S1	S2	S3	S4	S5	S6	S7	S8	S9
Visual appearance	Clear								
pH	4.7	4.8	4.9	4.6	4.7	4.7	4.5	4.6	4.5
Viscosity (Cps)	44.8	42.1	43.3	39.09	38.3	39.02	37.24	37.92	38

Table 7: Results of prepared formulations for gelation temperature and time

Formulation	Gelation temperature (°C)	Gelation time (s)
S1	35±0.99	36±0.97
S2	33±1.24	44±1.02
S3	24±1.12	35±1.15
S4	22±1.25	37±1.23
S5	26±1.29	49±1.56
S6	32±1.02	51±1.58
S7	37±1.58	46±1.63
S8	41±1.25	49±1.35
S9	46±1.65	35±1.53

*Mean±SD, n=3. SD: Standard deviation

Fig. 5: *In vitro* diffusion profile of S1, S3, and S9

Evaluation of formulated *in situ* gels

Clarity

The visual appearance of formulated gel (S1-S11) was found to be clear when observed against a white and black background, and the results were depicted in Table 6.

pH

The optimal pH range for any *in situ* gel is 4.7–4.9 and the formulated gels loaded with Fluconazole had shown within the range of 4.6–4.9 as depicted in Table 6. From the results obtained, it can be inferred that pH of the formulated *in situ* gels was within the range.

Viscosity

The viscosities of the formulated gels were found to be within the range of 38–45 cps which was depicted in Table 6. From the results, it can be inferred that as the concentration of Pluronic F-127 increases there was an increase in viscosity, due to decreased distance between micelles which, in turn, lead to increased interactions between them and resulting in developing viscous gels.

Gelation temperature and time

As depicted in Table 7, all the formulated *in situ* gels had shown gel-like viscosity within a temperature range of 22–59°C and the formulations showed gelation within 35–51 s depending on the concentrations of Pluronic F-127 and Carbapol-934. From the results obtained, it was inferred that S1, S3, and S9 had shown gelation at body temperature, whereas formulation S3 and S9, i.e. 35 s had shown gelation faster when compared with other formulations and every addition of 0.1% w/w CP 934 into the formulations led to 5°C increase in gelation temperature.

Mucoadhesive force

Results obtained from mucoadhesive force study suggested that adhesive property of Pluronic F-127 increases with increase in concentration of Carbapol-934. Formulation S3 had shown more strength (5210.32 dynes/cm²) when compared with S1 (4650.29 dynes/cm²) and S9 (5123 dynes/cm²). From the results, it can be inferred that more the mucoadhesive force, more it can prevent fallout of the gelled solution from mucosa.

In vitro diffusion studies

The formulated gels S1, S3, and S9 retarded drug release from *in situ* gel for 10–12 h as depicted in Fig. 5. Results suggested that S3 formulation has sustained the release of drug up to 12 h, while formulations S1 and S9 had completely diffused the drug within 8 h. From the results obtained, it can be inferred that as the concentration of polymers increased, release of drug from *in situ* gel was retarded.

CONCLUSION

Thermoreversible *in situ* gels loaded with fluconazole were formulated and optimized successfully by cold technique by employing DoE software. FTIR and DSC studies suggested that there was no chemical interaction present between the pure drug and physical mixture. Among different formulations S1, S3, and S9 have shown gelation at body temperature. From the data obtained from *in vitro* studies and mucoadhesive study as S3 was considered as optimum formulation as it sustained the release of the drug up to 12 h and shown a mucoadhesive strength of 5210.32 dynes/cm², while other formulations diffused the drug completely by 6–8 h and shown a mucoadhesive strength of 4650.29 dynes/cm² and 5123 dynes/cm². From the results, it can be concluded that formulated *in situ* gel can be used as an alternative approach to treat candidiasis.

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AUTHOR'S CONTRIBUTIONS

Author is a faculty in division of pharmaceuticals and the work contributed on faculty development program in the institution.

CONFLICTS OF INTEREST

The author confirms that this article content has no conflicts of interest.

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