DEVELOPMENT AND EVALUATION OF TIOCONAZOLE LOADED EMULGEL

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ABSTRACT

Objective: The objective of the present work was to develop, characterize and evaluate the tioconazole loaded emulgel and to prove that emulgel can be the best alternative for delivery of hydrophobic drug topically.

Methods: for the preparation of stable Emulgel, firstly gels were prepared using different polymers as carbopol 934 and xanthan gum, followed by preparation of emulsions and finally mixed together (table 1). Emulgel was evaluated for physical appearance, pH, spreadability, extrudability, viscosity, swelling index, dilution test, centrifuge test, drug content, in vitro release study, kinetic analysis of release data, antifungal activity and stability study for 3 mio. A comparative study was also performed between prepared emulgels with available marketed antifungal cream.

Results: All evaluation parameters were in acceptable range with good physical appearance and the pH in the range of 5.5 to 6.8. The results show that the extrudability was in the range 15.63 to 35.27 g/cm²; with spreadability in range of 6.6 to 8833 cm. swelling index of F3 was seen a maximum in 3 h of about 75.13%. The viscosity was in the range of 15240 to 56340 cps at 10 RPM. During in vitro release of all formulations, F1 and F5 showed a maximum in vitro drug release of 59.11% and 55.11% respectively in 8 h. The kinetic analysis of fitting the data in different model shows that the best formulation of F1 fits in the Higuchi model with regression coefficient (R²) of 0.998 and show non-fickian diffusion. The formulations were found stable. F1 and F5 provide a similar zone of inhibition like to market cream.

Conclusion: Tioconazole emulgel provide the better platform for delivery of hydrophobic drug for topical route and so able to produce better patient compliance.

Keywords: Emulgel, Tioconazole, Hydrophobic drug, Topical drug delivery

INTRODUCTION

Topical drug delivery is the potential route to deliver the drug producing low side effect in comparison with any other dosage forms. Drug concentration can be optimized to low concentration due to lack of metabolic elimination of drug before reaching the targeted site [1]. There are various conventional dosage forms for topical applications as cream, ointment, gel, but they shows fluctuation in bioavailability of drugs and are associated with other limitation as gel is limited to deliver the hydrophilic drugs, similarly ointment are limited for hydrophilic drug, so recently there have been novel approaches in the topical delivery to control the fluctuation of drug and deliver it in a controlled manner as per our need and to reduce the limitation associated with conventional preparation also to improve their properties for patient compliance [2]. The new approach in the field of topical drug delivery is introduced to deliver the hydrophilic drug that can enjoy the gelling property and whose rate can be controlled named Emulgel. It is simply where emulsion of the drug is prepared and that are incorporated in the gel [3].

Several antifungal agents are available in the market as cream, ointment, gel, powders, lotions etc. for dermatological preparations. Tioconazole is an antifungal agent of imidazole class which is used to treat infections caused by a fungus or yeast. Imidazoles having broad spectrum activity against dermatophytes, Candida and other fungi involved in deep mycosis, some gram-positive and anaerobic bacteria. Tioconazole has considerably greater fungicidal activity than clotrimazole, econazole, ketoconazole, and miconazole against Candida albicans and other Candida species. Tioconazole is highly hydrophobic in nature that lies in Biopharmaceutics classification system (BCS)-II class [4, 5].

Taking above consideration, tioconazole was selected to formulate as emulgel, the aim of this study was to develop an emulgel formulation of tioconazole using two polymers, natural polymer-xanthan gum and synthetic polymer-carbopol 934 in different concentration. The effect of using different polymer for gelling and its concentration variation on the release of the drug from the emulgels was investigated. Others parameters as physical properties, spreadability, rheological properties, extrudability, swelling index, antifungal activity of the emulgel were also evaluated and compared with the marketed cream of sertaconazole nitrate (Onabé™) of the same imidazole class antifungal to justify that the emulgel can be the alternative for cream or they can be better dosage form to deliver the drug than other conventional semi-solid preparations for hydrophobic drugs in topical treatment.

MATERIALS AND METHODS

Materials
Tioconazole was received as gift from Themis Medicare Pvt. Ltd. Haridwar (India). All other excipients were of analytical grade procured from Central drug house Pvt. Ltd. Delhi (India). Distilled water was used throughout the studies. Onabé™ cream [sertaconazole nitrate 2% w/w] of Glenmark Pharmaceuticals Ltd was procured from Pharmacy shop.

Methods

Drug-polymer compatibility studies
Drug–polymer compatibility studies were done for selection of polymer by Fourier Transform Infrared spectroscopy (FTIR) [6].

Infrared spectroscopy

Infrared spectra were recorded in the region of 4000 to 400 cm⁻¹ by Perkin Elmer Spectrum Two™ Spectrophotometer.

Formulation and evaluation

Preparation of emulgel formulation in different polymer

The composition of emulgel formulations is given in table 1. Emulgel was prepared in two steps, the first formation of emulsion and that are incorporated in the gel [3].
addition of emulsion into the gel. In formulations F1, F2, F3 gel base were prepared by dispersing carbopol 934 in distilled water and the pH was adjusted to 6 to 6.5 using triethanolamine (TEA). In formulations F4, F5, F6 xanthan gum was dispersed in cold water to form a gel. Oil phase of the emulsion was prepared by heating liquid paraffin and cetostearyl alcohol to 70 °C to 80 °C and dissolving span-80 into it, then isopropyl myristate was added to oil phase. The aqueous phase is prepared by dissolving tween-80 and addition of propylene glycol to it, further tioconazole dissolved in alcohol was added to same. Both the oil and aqueous phase was heated to 70 °C to 80 °C and then the aqueous phase was added to oil under constant stirring until the temperature reaches to room temperature. The obtained emulsion was then added to gel under stirring in the ratio of 1:1 to obtain the Emulgel [7].

Table 1: Composition of tioconazole emulgel formulations

<table>
<thead>
<tr>
<th>Ingredients (%w/w)</th>
<th>Formulations</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>F1</td>
</tr>
<tr>
<td>Xanthan gum</td>
<td>7</td>
</tr>
<tr>
<td>Light liquid paraffin</td>
<td>1</td>
</tr>
<tr>
<td>Xylitol</td>
<td>3</td>
</tr>
<tr>
<td>Tioconazole</td>
<td>1</td>
</tr>
<tr>
<td>Propylene glycol</td>
<td>5</td>
</tr>
<tr>
<td>Water</td>
<td>q.s</td>
</tr>
</tbody>
</table>

Evaluations of emulgel and marketed cream

Physical appearance

The prepared Emulgel and the marketed cream Onabet™ were inspected visually for their color, homogeneity, grittiness, phase separation [8].

pH

pH of 1% dispersion of Emulgel and the marketed cream Onabet™ in distilled water was measured with digital pH meter. Measurement was done in triplicate and averages were calculated [8].

Extrudability (tube test)

Here the weight required extruding 0.5 cm ribbon of Emulgel and the marketed cream Onabet™ in 10 s from the lacquered collapsible aluminum tube is determined. The test was repeated and the average values were used for the calculation [8].

Formula for extrudability calculation

Extrudability = weight applied to extrude emulgel from tube(g) /Area(cm²)

Swelling index

1 g of Emulgel formulations and the marketed cream Onabet™ were taken on porous aluminum foil and then placed in the petri dish containing 10 ml distilled water. The samples were taken from the petri dish at a different time interval and left undisturbed in a dry place for some time so that the external liquid is removed and weighed. Swelling index is then calculated by using below formula [8].

Swelling Index (SW)% = [(Wt - Wo) / Wo] × 100

Where (SW)% = Equilibrium percent swelling,
Wt = Weight of swollen emulgel after time t,
Wo = Original weight of emulgel at zero time

Spreadability

It expresses the extent of the area to which formulation readily spreads to the affected part on the application. The therapeutic efficacy of the product depends on its spreading value. For determination of spreadability, 1 g of Emulgel formulations and the marketed cream Onabet™ was placed within the circle of 1 cm diameter pre-marked on a glass plate of 20 x 20 cm, on which a second glass plate was placed. A 500 g weight was allowed to rest on the upper glass plate for 5 min. The increase in the diameter due to gel spreading was noted [9].

Drug content

1% dilution of Emulgel formulations was done with a suitable solvent and filtered through Whatman filter paper. 1 ml filtrate is further diluted to 10 ml, then the sample was analyzed in UV spectrophotometer against blank that is solvent without drug and absorbance was noted. The absorbance was fitted in the line of equation obtained from the calibration curve to obtain the concentration of drug [10].

Dilution test

1% aqueous dilution of Emulgel and the marketed cream Onabet™ was done by adding Continuous phase and visually checked for phase separation and clarity [11].

Centrifuge test

6 g of Emulgel was taken in 10 ml graduated centrifuge tubes and were subjected to spin at 4000 RPM for 10 min. The sample was observed for any phase separation occurrence [12].

Viscosity

The viscosity of prepared emulgel and Onabet™ marketed cream was measured by Brookfield DVE viscometer (AMETEK) with spindle 64. The preparation whose viscosity was to be determined was placed in the viscometer and the receptor compartment was filled with phosphate buffer pH 7.4. The medium was continuously stirred with the magnetic bead at 50 rpm. The viscosity in centipoises was observed and reported [13].

In vitro drug release

In vitro releases of emulgel were calculated out using Franz diffusion cell (effective diffusion area 4.9 cm² and 14 ml cell volume). Semi permeable egg membrane was clamped to the donor compartment and the receptor compartment was filled with phosphate buffer pH 5.5+metanol [9:1] which was the dissolution media. The temperature of the cell was maintained at 37±2 °C. The medium was continuously stirred with the magnetic bead at 50 rpm. The emulgel (500 mg) were spread uniformly on the membrane. The sample 1 ml aliquots were withdrawn from the receptor at regular interval and replace with the equal amount of fresh dissolution media. The samples withdrawn were diluted to required and analyzed under UV-spectrophotometry. The cumulative percentage drug released were calculated with time [14].

Kinetic analysis of drug release

Kinetic analysis of the drug release was done by fitting the release data to the different release model given below to describe the proper release model:
Zero order release (cumulative % drug release vs. time)

\[ Q = K_0t \]

Where \( Q \) is the amount of drug released at time \( t \), \( K_0 \) is the zero-order release rate.

First order release (log cumulative % drug retained vs. time)

\[ \ln(100-Q) = \ln 100 - K_1t \]

Where \( Q \) is the percent of drug released at time \( t \), \( K_1 \) is the first-order release rate constant.

Higuchi model (cumulative % drug retained vs. square root of time)

\[ Q = K_2\sqrt{t} \]

Where \( Q \) is the percent of drug released at time \( t \), \( K_2 \) is the Higuchi square root of time release constant.

Korsmeyer-peppas model (log cumulative % drug release v/s. log time)

\[ F = \left( \frac{M_t}{M} \right) = K_m t^n \]

Where \( F \) is fraction of drug released at time \( t \), \( M_t \) is drug release at time \( t \), \( M \) is the total amount of drug in dosage form, \( K_m \) is a constant dependent on the geometry of the dosage form, \( n \) is diffusion exponent indicating the mechanism of drug release, if the value of \( n \) is 0.5 it indicates fickian diffusion and if between 0.5 to 1 it is anomalous transport or Non-fickian diffusion [14].

Antifungal activity

19.5 g of Potato dextrose agar (PDA) was transferred in a 500 ml of conical flask and 500 ml of purified water and heat is applied to dissolve completely. Sterilization was done for 15 min at 121 °C at 15 lbs pressure in an autoclave. Agar well method was used to determine the zone of inhibition for antifungal activity of emulgel formulations. Aspergillus strain was obtained from the Department of Microbiology, self-cultured in SGRRITS, Dehradun. The medium was poured into the three petridish and cooled for few minutes at room temperature until it forms solidifies at room temperature and then the three cups are bored in each petridish with the help of sterile steel boarer of 6 mm and fungal strain was swabbed on the PDA plate and similar concentration of the standard formulation (0.125 g) and emulgel formulations (0.25 g) were placed in the bores with help of 18 gauges needles and the petri plates were incubated for 24 to 48 h at 25 °C in incubators. The zone of inhibition was measured in mm [15].

Stability studies

The optimized formulation was subjected to accelerated stability for 3 mo as per ICH guidelines by keeping at 40+2 °C/75+5% RH and Samples were withdrawn on at a regular interval of 1, 2 and 3 mo for evaluation of physical appearance, pH, viscosity, centrifuge test and drug content [16].

RESULTS AND DISCUSSION

Drug-polymer compatibility studies

FTIR study of pure Drug (fig. 1), Drug with carbopol 934 (fig. 2) and drug with xanthan gum (fig. 3) was performed. The evaluation was based on shifting of the fingerprint region as the experimental result shows there was no significant deviation between drug and drug with polymers which confirm the compatibility. So these polymers were selected for formulations [6].

Evaluation of emulgel and marketed Cream

Physical appearance

Physical appearances of the formulations are shown in fig. 4 and described in table 2.
Table 2: Physical characteristics

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Colour</th>
<th>Phase separation</th>
<th>Grittiness</th>
</tr>
</thead>
<tbody>
<tr>
<td>F1</td>
<td>White</td>
<td>No</td>
<td>None</td>
</tr>
<tr>
<td>F2</td>
<td>White</td>
<td>No</td>
<td>None</td>
</tr>
<tr>
<td>F3</td>
<td>White</td>
<td>No</td>
<td>None</td>
</tr>
<tr>
<td>F4</td>
<td>White</td>
<td>No</td>
<td>None</td>
</tr>
<tr>
<td>F5</td>
<td>White</td>
<td>No</td>
<td>None</td>
</tr>
<tr>
<td>F6</td>
<td>White</td>
<td>No</td>
<td>None</td>
</tr>
<tr>
<td>Onabet™</td>
<td>White</td>
<td>No</td>
<td>None</td>
</tr>
</tbody>
</table>

*p=3, Average of three determinations

The formulations were white viscous creamy preparation with a smooth, homogeneous texture and glossy appearance with no grittiness and phase separation. That indicates the physical stability of the prepared formulations with acceptable features [7].

Table 3: pH of emulgel formulation and marketed cream

<table>
<thead>
<tr>
<th>Formulation</th>
<th>F1</th>
<th>F2</th>
<th>F3</th>
<th>F4</th>
<th>F5</th>
<th>F6</th>
<th>Onabet™</th>
</tr>
</thead>
<tbody>
<tr>
<td>pH</td>
<td>5.733±0.057</td>
<td>5.867±0.057</td>
<td>5.733±0.057</td>
<td>6.767±0.057</td>
<td>6.733±0.057</td>
<td>6.667±0.057</td>
<td>6.767±0.057</td>
</tr>
</tbody>
</table>

*p=3, mean±SD, The pH of the formulations was in the range 5.5 to 6.8 which match with the normal pH range of the skin and thus do not produce any skin irritation [1].

Table 4: Extrudability of emulgel formulations and marketed cream

<table>
<thead>
<tr>
<th>Formulation</th>
<th>F1</th>
<th>F2</th>
<th>F3</th>
<th>F4</th>
<th>F5</th>
<th>F6</th>
<th>Onabet™</th>
</tr>
</thead>
<tbody>
<tr>
<td>Extrudability (g/cm²)</td>
<td>20.67±0.473</td>
<td>31.2±0.656</td>
<td>35.27±1.201</td>
<td>15.63±0.727</td>
<td>17.8±0.3</td>
<td>23.5±0.53</td>
<td>19.8±0.7</td>
</tr>
</tbody>
</table>

*p=3, mean±SD

Formulation F1 and F4 with polymers carbopol 934 and xanthan gum respectively having low concentration among their respective formulations shows the low requirement of extrusion pressure and the extrudability rises with the increase in viscosity of the formulation. The formulation with xanthan gum requires low extrusion pressure in comparison with that of carbopol and all the
results were acceptable in comparison to the marketed cream Onabet™ [2].

**Swelling index**

The swelling index of all formulations and marketed cream is represented in fig. 5.

Formulations with carbopol 934 showed maximum swelling index in comparison with xanthan gum and were comparable to that of marketed cream. Among all the formulation, F3 emulg el with carbopol 934 (1.5%) showed the highest swelling index. Variation in swelling index value may be dependent on the water uptake nature and chain strength of the polymer [1].

**Spreadability**

Spreadability of emulg el and marketed cream are shown in table 5. Spreadability is carried out for all the formulations. It indicates how easily the emulgel will be spread on the affected area by the small amount of shear. Spreadability of emulgel formulation lies between 1-8.833. F1 shows good spreadability among the carbopol polymer and F4 shows good spreadability among the xanthan gum polymer [9].

**Drug content**

Drug content of prepared formulations are shown in table 6.

The drug content of the formulations is determined by UV-spectrophotometer at a wavelength of 230 nm, all the formulations shows the drug content in between the limit of 95% to 102% and there is no major effect of a change in polymers and its concentrations [10].

**Dilution test**

All prepared formulations and marketed cream were diluted with water and result indicated no phase separation upon dilution [11].

**Centrifuge test**

All prepared formulations and marketed cream showed no phase separation that indicates the stability of product on high shear rate [12].

**Viscosity**

The viscosity of emulgel formulation and marketed cream was determined using Brookfield Viscometer. Emulgel with carbopol 934 shows high viscosity in comparison to that of emulgel with xanthan gum. Results show the ascending viscosity of emulgel with an increase in the concentration of polymer in order F3>F2>F1 for carbopol 934, and a similar increase in viscosity was seen for the formulation with xanthan gum the amount of drug released after 8 h was 59.11%, 40.77%, 35.18% respectively, and for the formulations with xanthan gum the drug release in descending order F5>F4>F6 where the amount of drug released after 8 h was 55.14%, 50.68%, 42.83% respectively. It has been concluded that the carbopol 934 emulgel with low concentration of polymer F1 shows maximum release. The release...
pattern with carbopol 934 emulgel was better than that of xanthan Gum. It shows carbopol 934 is better polymer than xanthan gum for formulating emulgel. Formulation F1 from carbopol polymer and formulation F5 from xanthan gum polymer shows the best result. The cumulative % drug release profile of all the formulation batches has been shown in fig. 7 [16].

**Fig. 6: Viscosity of emulgels and marketed cream with effects of shear rate (rpm) on it**

**Fig. 7: In vitro cumulative % drug release profile of emulgel formulations**

**Kinetic analysis of drug release**

The results of *in vitro* release from formulations were plotted in different kinetic models like Zero order, First order, Higuchi plot and Korsmeyer Peppas plot and are represented in fig. 8, fig. 9, fig. 10, fig. 11 respectively. The regression coefficient value $R^2$ is reported for all formulations. The release data of best formulation F1 and F5 follows Higuchi model kinetics and first order kinetics respectively. All the formulation follows anomalous or non-fickian diffusion for drug release. The regression coefficients of all formulations are listed in table 7 [16].

**Fig. 8: Zero order release plot of emulgel formulations**
Fig. 9: First order release plot of emulgel formulations

Fig. 10: Higuchi release plot of emulgel formulations

Fig. 11: Korsmeyer peppas release plot of emulgel formulations

Table 7: Release kinetic result of emulgel formulations

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Zero order</th>
<th>First order</th>
<th>Higuchi plot</th>
<th>Korsmeyer Peppas plot</th>
<th>Best fit model</th>
<th>mechanism of drug release</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>$R^2$</td>
<td>$R^2$</td>
<td>$R^2$</td>
<td>$R^2$</td>
<td>$n$</td>
<td></td>
</tr>
<tr>
<td>F1</td>
<td>0.970</td>
<td>0.996</td>
<td><strong>0.998</strong></td>
<td>0.986</td>
<td>0.845</td>
<td>Higuchi model</td>
</tr>
<tr>
<td>F2</td>
<td>0.918</td>
<td>0.957</td>
<td><strong>0.964</strong></td>
<td>0.890</td>
<td>0.746</td>
<td>Higuchi model</td>
</tr>
<tr>
<td>F3</td>
<td>0.980</td>
<td><strong>0.987</strong></td>
<td>0.975</td>
<td>0.951</td>
<td>0.887</td>
<td>First order</td>
</tr>
<tr>
<td>F4</td>
<td>0.966</td>
<td>0.987</td>
<td><strong>0.995</strong></td>
<td>0.983</td>
<td>0.787</td>
<td>Higuchi model</td>
</tr>
<tr>
<td>F5</td>
<td>0.969</td>
<td><strong>0.983</strong></td>
<td>0.980</td>
<td>0.961</td>
<td>0.664</td>
<td>First order</td>
</tr>
<tr>
<td>F6</td>
<td><strong>0.983</strong></td>
<td>0.977</td>
<td>0.953</td>
<td>0.973</td>
<td>0.730</td>
<td>Zero order</td>
</tr>
</tbody>
</table>

Table 10: Zone of inhibition of emulgel formulation and marketed cream

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Zone of Inhibition(mm)</th>
</tr>
</thead>
<tbody>
<tr>
<td>F1</td>
<td>18±1.732</td>
</tr>
<tr>
<td>F5</td>
<td>14.67±0.577</td>
</tr>
<tr>
<td>S (Onabet™ cream)</td>
<td>17.33±1.155</td>
</tr>
</tbody>
</table>

* $n=3$, mean±SD

Antifungal activity

The antifungal activity of best two formulations F1 and F5 were seen and compared with the Onabet™ marketed cream (S) by measuring the zone of inhibition. The Formulation F1 shows a maximum zone of inhibition 18 mm, whereas F5 and S shows the zone of inhibition of 14.67 and 17.33 respectively. The result indicates that the prepared emulgel F1 and F5 had a comparable antifungal activity to that of marketed cream (S) [17].
Thus the tioconazole emulgel can be the best approach for topical storage, the F1 and F5 formulation was observed in a stable form. From the stability studies, after the maximum drug release of 55.91% and 55.14% respectively in 8 h with good physical properties. From the stability studies, after storage, the F1 and F5 formulation was observed in a stable form. Thus the tioconazole emulgel can be the best approach for topical delivery.

CONCLUSION

Tioconazole Emulgel was formulated and compared with marketed cream and proved that emulgel can be, the better option than conventional as it minimizes the disadvantages associated with conventional semi-solid increasing the patient compatibility. The different gelling agent can be utilized such as carbopol 934 and xanthan gum. It can be novel approach to deliver the hydrophobic drug topically. It utilizes the two methods of formulating the emulsion and gel that facilitate to control the release of drugs. Various drugs can be formulated as emulgel and mostly the BCS class-II is efficient.

Stability studies

The optimized formulations F1 and F5 with acceptable drug release were observed in stability study, for 3 mo and all the parameters as physical appearance, pH, viscosity and drug content was found to be stable upon storage for 3 mo, no major changes were observed in their parameters, the slight changes were seen which was in acceptable limit that indicates, the formulations are stable whose shelf life can be predicted [16].

REFERENCES


How to cite this article