

PROPRANOLOL HYDROCHLORIDE TOPICAL GEL FOR THE TREATMENT OF INFANTILE HEMANGIOMA

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ABSTRACT

Objective: To formulate and evaluate propranolol hydrochloride topical gel for overcoming the limitations and low oral bioavailability associated with conventional therapy.

Methods: The propranolol hydrochloride topical gels were prepared by the cold mechanical method. The preliminary evaluation and further characterisation studies was conducted to find the optimised formulation. The *in vitro* release and *ex vivo* permeation studies were investigated. The histopathological studies and stability studies was also assessed.

Results: The propranolol hydrochloride topical gel was successfully prepared. The *in vitro* release of optimized topical propranolol hydrochloride gel formulation (G2) showed the highest cumulative percentage drug release that is, 95.55%±0.15 after 7.5 h. (G2) the formulation showed a higher flux value of 4.61µg/cm²/h. The histopathological study using pig skin revealed that the optimized formulation was found to be safe for topical application.

Conclusion: The formulated topical gel containing propranolol Hydrochloride seems to be a promising dosage form for enhanced skin delivery of propranolol hydrochloride in treating Infantile Hemangioma.

Keywords: Infantile Hemangioma, Propranolol hydrochloride, Topical gel

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INTRODUCTION

Infantile Hemangioma (IH) is benign vascular tumors or soft tissue tumors of childhood, characterized by endothelial cell proliferation. It is usually referred as "Strawberry Hemangiomas" because it appears as a red or blue raised lesion [1]. The prevalence of Infantile Hemangioma is about 1-10% across the world population and it is more frequently occur in low birth weight, female, premature infants and in twin birth. The tumours are commonly developed during infancy and only about 20% of them being present at birth. The main complications associated with Infantile Hemangiomas include risk of bleeding, tissue damage, ulceration, infection, pain, functional impairment, disfigurement of tissues etc. [2]. Congenital structural abnormalities are associated with some types of IH. IH are classified on the basis of morphological features into superficial, deep and mixed types [3]. Superficial hemangiomas are identified by bright red vascular nodules and plaques [4]. Deep hemangiomas are commonly characterized by subcutaneous, bluish vascular swellings and compressible lesions. Mixed hemangiomas are the combinations of both superficial and deep hemangiomas. Based on the distributions, IH are classified as localized, segmental, indeterminate and multifocal hemangiomas [5]. Vasculogenesis and angiogenesis are the important mechanisms underlying the pathophysiology of Infantile Hemangioma. Equilibrium between proangiogenic and angiogenic factors are disturbed by hypoxia and acidosis and result in endothelial proliferation, thus increases the growth rate of lesions. In addition to the proliferation of endothelial cells, acidosis and perinatal hypoxia increases the secretion of vascular endothelial growth factor (VEGF) by stimulating angiogenesis [6]. The angiogenic factors H1F1-alpha plays an important role in the induction of gene transcription of VEGF. Several theories are illustrated to give a brief idea about the pathogenesis of IH, including the placental hypothesis, vasculogenesis theory and hormonal theory [7]. The treatment options included in the current treatment strategy of Infantile Hemangioma includes the use of systemic or topical beta-blockers, systemic or intralesional corticosteroids, Interferons, pulsed dye laser therapy, surgical excision etc. The first line agent that is preferred in the treatment of Infantile Hemangioma is propranolol hydrochloride because of its rapid onset of action and

good drug tolerability [8]. The orally and intralesionally available therapies are associated with various types of adverse effects, so it is necessary to develop a topical formulation to treat this disease condition. Various advancements in the novel drug delivery system provide a wide opportunity for these limitations. Formulation of topical gels by using the first-line agent like propranolol hydrochloride is considered as efficient for the treatment of Infantile Hemangioma. Gels are more advantageous when compared to other topical formulations because of its easy application and increased patient compliance. The usage of polymers such as Carbapol 934 and HPMC in the formulation of gels can improve drug permeation and drug release properties of gels. The transdermal route of drug administration provides systemic delivery of drugs by applying the drug to unbroken and healthy skin, thus ensuring a sustained release of drugs and bypasses the Hepatic first-pass metabolism. Transdermal delivery of drugs significantly delivers an appropriate amount of drugs, thus overcoming conventional problems of oral dosing [9]. Hence the current study aims to formulate and evaluate topical gel containing propranolol hydrochloride for treating Infantile Hemangioma.

MATERIALS AND METHODS

Materials and excipients

The drug of choice, propranolol hydrochloride, was provided by Research fine chemicals Industries, Mumbai. Other ingredients used in this study were of standard grade.

Preformulation studies

Fourier transform infrared (FTIR) spectroscopy

The FTIR spectra of drug and excipients were obtained to ascertain the compatibility between propranolol hydrochloride and selected polymers using FTIR spectrophotometer by Potassium Bromide (KBr) pressed pellet method [10].

Solubility studies

Solubility profile of the drug was performed in various solvents such as chloroform, propylene glycol, distilled water, methanol, acetone and Phosphate Buffer Saline (PBS) pH 5.8 [11].

Melting point of the drug

Open capillary tube method was used to determine the melting point [12].

Lambda max of propranolol hydrochloride in phosphate buffer solution (PBS) pH 5.8

Absorption maxima of propranolol hydrochloride were determined in PBS pH 5.8 [13]. Standard stock solution was prepared by dissolving 10 mg of propranolol hydrochloride in 30 ml PBS pH 5.8 followed by sonication for 10 min and volume was made upto 100 ml using PBS pH 5.8. The concentration of the standard stock solution was 100 µg/ml. This was scanned between 400-200 nm.

Drug compatibility with excipients

The compatibility of drug with excipients is determined using FTIR spectral analysis [14].

Calibration curve of propranolol hydrochloride in PBS pH 5.8

Dissolved 2.712g of potassium dihydrogen orthophosphate in 100 ml distilled water and 0.8g of sodium hydroxide in 100 ml distilled water separately. From the prepared solution fixed volume of potassium dihydrogen orthophosphate and sodium hydroxide was taken into 100 ml standard flask and volume was made up to 200 ml mark using distilled water [15, 16].

Preparation of stock solution

10 mg of propranolol hydrochloride in 30 ml phosphate buffer was sonicated for 10 min and the volume was made up to 100 ml mark using PBS pH 5.8 solution to get a concentration of 100 µg/ml.

Preparation of standard graph

From the above solution, different concentrations were withdrawn and diluted to 10 ml with PBS pH 5.8 separately to prepare a series of concentrations from range 20-100 µg/ml. The standard stock solution was scanned in the range of 400-200 nm against PBS pH 5.8 as blank. Absorbance was plotted against concentration to obtain the standard graph.

Formulation of propranolol hydrochloride topical gel

Polymers carbapol 934 (0.15%w/v) and HPMC (0.25-0.30%w/v) in distilled water was taken in a glass beaker, soaked for 24 h [17]. Methanol was added to dissolve the drug. Then the drug was added to the above solution and made upto to the required quantity using remaining distilled water, which was then continuously stirred using a mechanical stirrer. The polymeric mixture with drug was neutralized using triethanolamine, followed by the addition of other ingredients like glycerine and ethylparaben with slow continuous stirring. Then the prepared formulation was transferred to collapsible tube and stored in a cool place. Prepared formulation was subjected to homogeneity study. Required quantity of the prepared gel was diluted with distilled water. The resulting solution, pH was determined, which was previously calibrated using PBS at pH 5.8 [18, 19].

Mean spreadability

0.5 gm gel was pressed between two glass slides and then left for some time. The extent to which gel spreaded was determined [20].

Mean extrudability

The gel formulations were filled into a collapsible metal tube or aluminium collapsible tube. The tube was pressed to extrude the material and the extrudability of the formulations was checked [21].

Mean drug content estimation

Series of dilutions of the drug in methanol was made and transferred into 10 ml volumetric flask. The drug content was estimated on UV-visible spectrophotometer at 289 nm using methanol as blank [22].

In vitro drug release study

A soaked cellophane membrane was fixed on an open tube. In donor compartment, 1 gm of gel was taken and dipped in a 100 ml beaker containing drug-free PBS pH 5.8 (90 ml) as a receptor compartment

and a temperature was maintained. Fixed volume of samples was taken at various intervals of time over a period of 7.5 h and the absorbances were recorded at 289 nm. The volume withdrawn at each time was replaced with drug-free PBS. The percentage of cumulative amount of drug released at various time intervals of time was calculated and plotted against time [23-25]. The kinetic models of *in vitro* drug release studies were plotted [26].

Ex vivo permeation comparison study

The pigskin collected was fitted to the receptor compartment and 1 gm of optimised gel (G2) containing 3 mg drug was taken in the cell and the cell was immersed in a beaker (100 ml) containing PBS pH 5.8 (90 ml) as receptor compartment. The cell was dipped in between the 90 ml pH 5.8 [27, 28]. Fixed volume of sample was taken and determined the absorbance. Fresh PBS pH 5.8 solution was introduced at each withdrawal and the graph was plotted. Similarly the *ex vivo* permeation comparison study was done for the prepared topical propranolol hydrochloride solution, control drug solution (drug in PBS pH 5.8) by adding 1 ml each of formulation (containing 3 mg drug) in the donor compartment and the study was performed for a maximum period of 8 h [29, 30].

Steady-state flux determination

From the above data steady-state flux (J) and enhancement ratio were found out [31, 32].

The steady-state values were then calculated from the slope value and was tabulated and statistical analysis by Student t-test was also done [33].

Histopathological examination

The histopathological study was done for optimised propranolol hydrochloride topical gel (G2) formulation, topical propranolol hydrochloride solution, control drug solution (drug in PBS pH 5.8). The porcine skin was collected from the slaughterhouse and was proceeded to 6 h of *ex vivo* permeation study [34]. After 6 h, the skin mucosa was taken and immersed in 10% formalin solution and the preserved live tissues were equally cut into 5 µm containing sections and further stained with hemotoxylin and eosin and analysed using light microscope [35, 36].

Stability study

The optimised topical Propranolol Hydrochloride gel formulation (G2) was subjected to stability studies [37].

RESULTS AND DISCUSSION

Preformulation studies

Fourier transform infrared (FTIR) spectroscopy

FTIR spectrum of propranolol hydrochloride showed broad peak at 3302.13 cm⁻¹, indicating the presence of alcoholic OH group of propranolol hydrochloride. A characteristic peak at 2981 cm shows the presence of aromatic CH group. A peak at 2819.93 cm⁻¹ represents the presence of aliphatic CH. An absorption band in the range of 2031.04 cm⁻¹ indicates the presence of C-C stretching of alkane. A peak at the range 1099.43 cm⁻¹ represents C-O stretching. FTIR spectrum of carbapol 934 showed an absorption band in the region of 2956.87 cm⁻¹ represents the presence of C-H stretching of alkane. A characteristic peak in the range of 1172.72 cm⁻¹ indicates the presence of C-O stretching. FTIR spectrum of HPMC showed a characteristic peak in the range of 2889.37 cm⁻¹ represents the presence of C-H stretching of alkane. A peak at 1045.20 cm⁻¹ indicates the presence of C=O functional group. FTIR spectrum of optimised topical propranolol hydrochloride gel formulation (G2) showed a broad peak at 3300.2 cm⁻¹ indicating the presence of alcoholic O-H group of propranolol hydrochloride. A characteristic peak in the region of 2034.90 cm⁻¹ indicates C-C stretching of alkane. A peak present in the range of 1597 cm⁻¹ represents the presence of C=O group. A characteristic peak in the range of 1099.43 cm⁻¹ indicates the presence of C-O stretching. No additional peaks were observed indicating good compatibility between drug and excipients when formulating it as a topical gel. The FTIR spectrum of the above compounds was shown in fig 1(A, B, C, D) [38, 39].

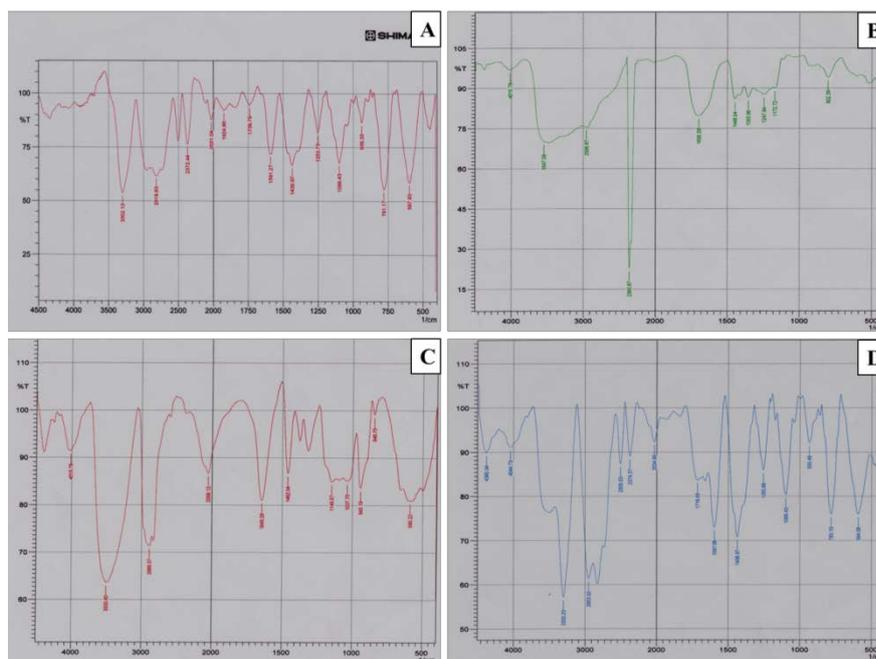


Fig. 1: (A) FTIR spectrum of Propranolol Hydrochloride, (B) FTIR spectrum of carbapool 934, (C) FTIR spectrum of HPMC, (D) FTIR spectrum of optimized propranolol hydrochloride topical gel

Solubility study

The pure drug was partially insoluble in chloroform and propylene glycol and soluble in distilled water, acetone, methanol Phosphate Buffer Saline (PBS) pH 5.8 [40].

Melting point

The melting point of the drug ranges from 160-168 °C [41, 42].

Lambda max of propranolol hydrochloride in phosphate buffer solution (PBS) pH 5.8

The absorption maxima of propranolol hydrochloride in PBS pH 5.8 was found to be 289 nm as shown in fig. 2(A)

Calibration curve of propranolol hydrochloride in PBS pH 5.8

The Standard calibration curve of drug was linear as shown in fig. 2(B)

Formulation of propranolol hydrochloride topical gel

The topical gel was formulated using the drug propranolol hydrochloride, which is the first-line agent for treating superficial Infantile Hemangioma and the polymer combination-carbapool 934 and Hydroxy Propyl Methyl Cellulose (HPMC) were also used [43, 44]. 0.15-0.20% w/v of carbapool 934, a synthetic polymer was used in formulating topical gel, which possesses effective gelling property and HPMC, a semisynthetic polymer used in this formulation, also enhance the gelling property. Triethanolamine act as an acid neutralizer [45, 46]. Glycerine (5 ml) acts as a permeation enhancer for topical drug delivery. Ethylparaben acts as a preservative. The topical gel is shown in fig. 2(C).

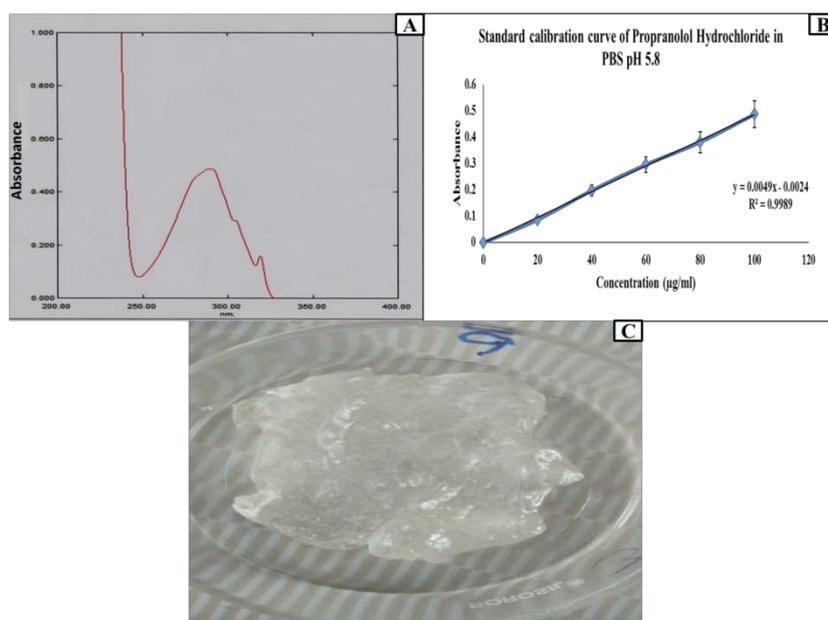


Fig. 2: (A) Lambda max of propranolol hydrochloride in PBS pH 5.8, (B) Calibration curve of propranolol hydrochloride, (C) Formulation of propranolol hydrochloride topical gel, (values are expressed as mean±standard deviation, n=3)

Characterization

Characterisation of topical gel

Homogeneity study

All the prepared topical gels were uniform in appearance [47].

Mean surface pH

The surface pH value ranges from 6.3±0.04 to 6.6±0.08, suitable for the topical application shown in fig. 3(C) [48].

Mean spreadability

The spreadability of the topical gel formulation ranges from 2.11±0.12gcm/min to 2.83±0.07 gcm/min and found to be suitable for the application shown in fig. 3(A)

Mean extrudability

The extrudability of the topical gels from the collapsible tube were also observed of which G2 formulation was easily extrudable when compared to the other formulation [49, 50].

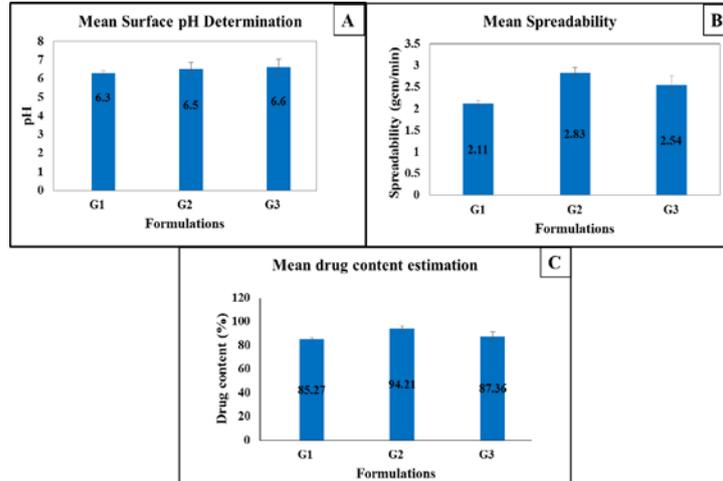


Fig. 3: (A) Mean spreadability, (B) Mean drug content estimation, (C) mean surface pH, (Values are expressed as mean±standard deviation, n=3)

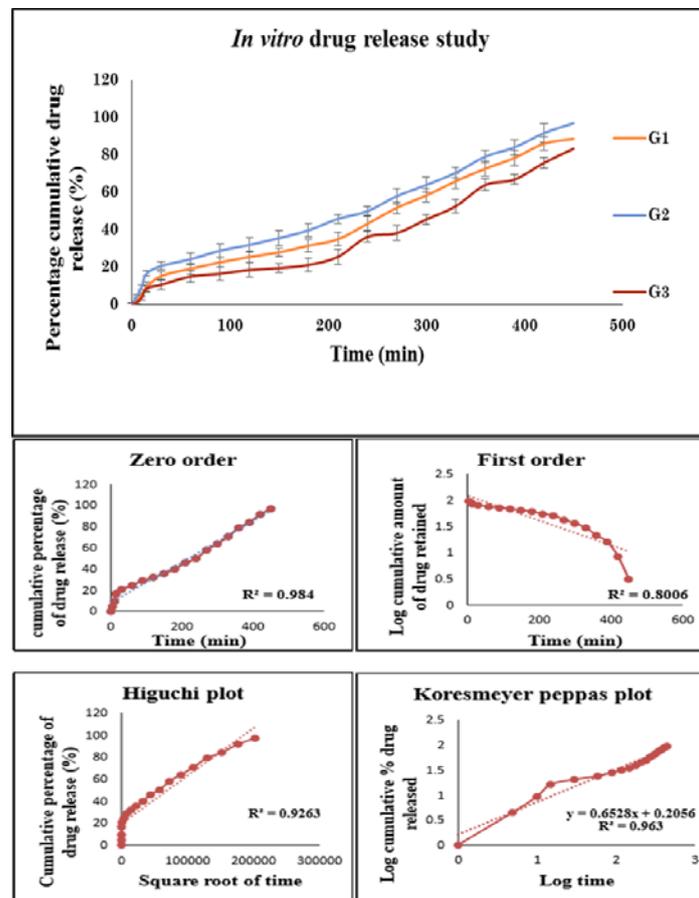


Fig. 4: *In vitro* drug release study and its kinetic modelling (values are expressed as mean±standard deviation, n=3)

Mean drug content estimation

Drug content values ranges from $85.27 \pm 0.23\%$ to $94.21 \pm 0.41\%$ for all the formulations. The drug content value was high in G2 formulation shown in fig. 3(B)

In vitro drug release study

The *in vitro* drug release study of different gel formulations were carried out for 7.5 h in pH 5.8 solution [52]. pH 5.8 solution resembles the normal skin pH. Temperature was maintained. The cumulative percentage drug release of various gel formulations (G1-G3) ranges from 88.90 ± 0.14 to 95.55 ± 0.15 at the end of 7.5 h. Selection of polymer is important in drug release study. The G2 gel showed highest cumulative percentage drug release that is, 95.55 ± 0.15 at the end of 7.5 h. The drug release profile of topical propranolol hydrochloride gel with the highest drug release pattern, (G2) was attributed to various kinetic models. The drug release kinetics fitted to zero order as the R^2 regression coefficient of the

model was found to be 0.984 [53, 54]. This was best fitted with korsmeyer peppas plot ($n=0.628$) and follows non fickian diffusion were shown in fig. 4

Ex vivo permeation comparison study

The *ex vivo* permeation comparison study was carried out for optimised topical propranolol hydrochloride gel formulation (G2), topical Propranolol Hydrochloride solution and control drug solution (drug in PBS pH 5.8) by open-end tube method using normal pig skin [55, 56]. The pigskin was tied on one side of open end tube and 1 gm optimised topical propranolol hydrochloride gel formulation (G2) containing 3 mg drug was placed on top of the skin mucosa and carried out the *ex vivo* permeation study. Fixed volume of samples was taken and analysed [57, 58]. The result of *ex vivo* permeation study indicated that the optimised propranolol hydrochloride topical gel formulation (G2) showed maximum permeation (i.e. $2345 \mu\text{g}/\text{cm}^2$) than topical propranolol hydrochloride solution ($1001 \mu\text{g}/\text{cm}^2$) and control drug solution ($789.61 \mu\text{g}/\text{cm}^2$) as shown in fig. 5

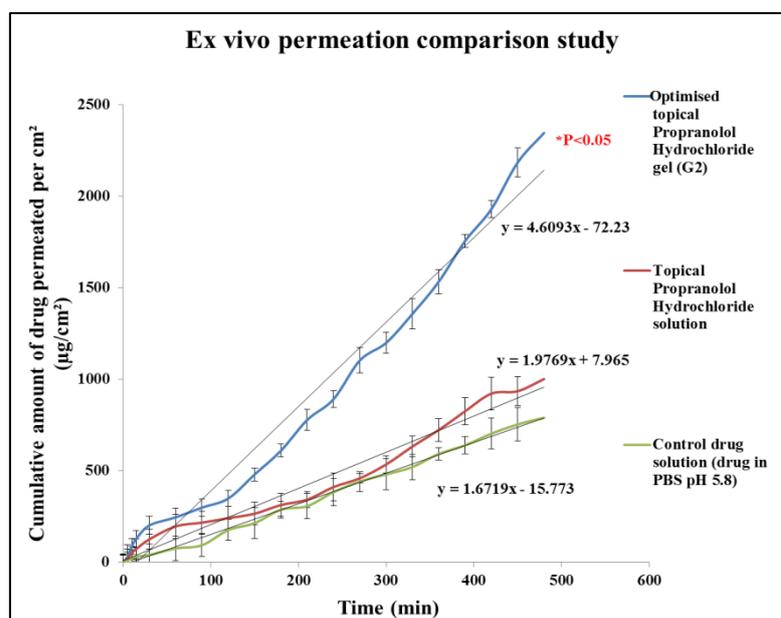


Fig. 5: *Ex vivo* permeation comparison study, (values are expressed as mean±standard deviation, n=3)

Table 1: Representation of flux, enhancement ratio parameters

S. No.	Parameters	Optimised topical propranolol hydrochloride gel (G2)	Topical propranolol hydrochloride solution	Control drug solution (drug in PBS pH 5.8)
1	Steady state flux-J ($\mu\text{g}/\text{cm}^2/\text{h}$)	4.61 ± 0.31	1.97 ± 0.22	1.67 ± 0.35
2	Enhancement ratio	2.8	1.1	-

(Values are expressed as mean±standard deviation, n=3)

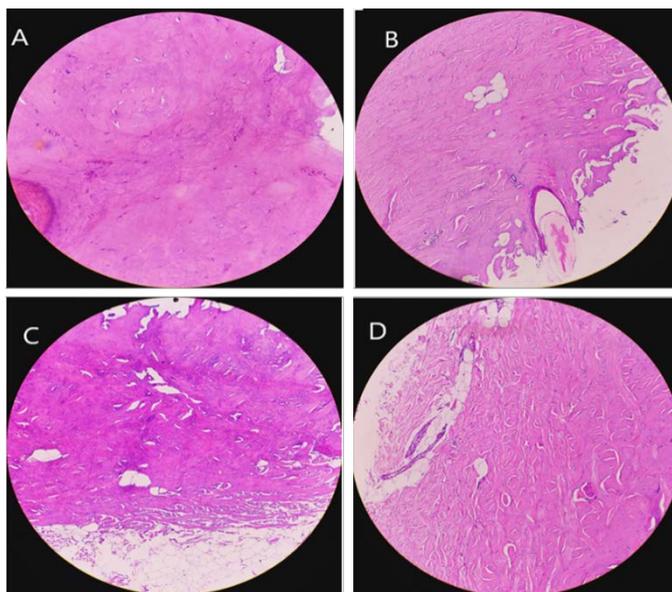
The flux value obtained for optimised propranolol hydrochloride topical gel formulation (G2) was found to be $4.61 \mu\text{g}/\text{cm}^2/\text{h}$. These values depicts that the optimised propranolol hydrochloride topical gel (G2) showed greater steady-state flux value ($4.61 \pm 0.31 \mu\text{g}/\text{cm}^2/\text{h}$) when compared to topical propranolol hydrochloride solution ($1.97 \mu\text{g}/\text{cm}^2/\text{h}$) and control drug solution ($1.67 \mu\text{g}/\text{cm}^2/\text{h}$). The enhancement ratio of optimised propranolol hydrochloride gel was found to be 2.8 and oral propranolol hydrochloride solution as 1.1 when compared with that of the control drug solution. The *ex vivo* permeation parameters confirmed that the permeation of propranolol hydrochloride across the pig skin layer was significantly higher when compared to topical propranolol hydrochloride solution and control drug solution which were shown in table 1 [59].

The statistical analysis by Student t-test was performed for the data obtained from the values of different formulations. The steady state

flux value of the optimized topical propranolol hydrochloride gel formulation (G2) compared to the prepared topical propranolol hydrochloride solution and control drug solution. Hence the difference is statistically significant ($P < 0.05$) as shown in fig. 5.

Histopathological examination

The pig skins subjected to 6 h permeation study were assessed for histopathological changes. The optimised topical propranolol hydrochloride gel formulation (G2), topical propranolol hydrochloride solution and control drug solution (drug in PBS pH 5.8) showed no significant changes in the histological pattern when compared to normal skin tissue [60]. Hence, it was found that optimised topical propranolol hydrochloride gel does not cause any irritation and was found to be safe for topical application as shown in fig. 6.



(Scale bar = 35 microns with 10x magnifications)

Fig. 6: Histopathological evaluation of pigskin treated with various formulations, (A) Normal pig skin, (B) Pig skin treated with optimised topical propranolol hydrochloride (G2) gel formulation, (C) Pig skin treated with topical propranolol hydrochloride solution (D) Pigskin treated with control drug solution (drug in PBS pH 5.8)

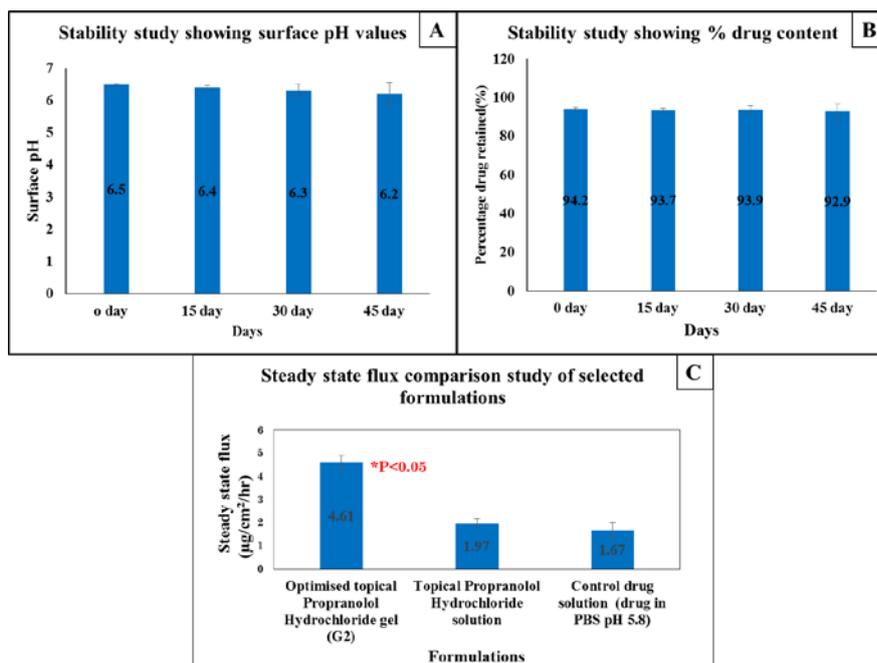


Fig. 7: (A) Stability study showing mean surface pH, (B) Mean drug content estimation, (C) Steady-state flux determination, (Values are expressed as mean±standard deviation, n=3)

Stability study

Parameters like pH and drug content were evaluated from 0 d to 45 d at regular intervals in room temperature condition [61]. The optimised propranolol hydrochloride topical gel (G2) formulation was found to be stable at room temperature condition as shown in fig. 7(A, B)

CONCLUSION

Infantile Hemangioma (IH) is a benign vascular tumour of childhood characterized by endothelial cell proliferation. The main purpose of this study was to formulate a topical gel drug delivery system for

treating IH that can bypass first-pass metabolism and nullify systemic side effects by delivering the drug directly in to the site of action. So by formulating the drug as topical gel, enhanced skin permeation was obtained. The steady-state flux were found to be higher for optimized topical propranolol hydrochloride gel formulation (G2) when compared to topical propranolol hydrochloride solution and control drug solution. Hence the formulated topical propranolol hydrochloride gel seems to be advantageous for enhanced skin delivery of first line agent propranolol hydrochloride for the treatment of Infantile Hemangioma, which could be further studied using suitable *in vivo* animal models.

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Nil

AUTHORS CONTRIBUTIONS

All the authors have contributed equally.

CONFLICT OF INTERESTS

Declared none

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