

Original Article

FORMULATION OPTIMIZATION AND EVALUATION OF MOUTH DISSOLVING FILM OF RAMOSETRON HYDROCHLORIDE

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ABSTRACT

Objective: Ramosetron Hydrochloride is found to be more potent and having a longer duration of action with the least side effects, but the major drawback is it undergoes hepatic first-pass metabolism so our aim is to prepare mouth dissolving film (MDF) of Ramosetron hydrochloride for rapid relief in emesis.

Methods: The mouth dissolving films of Ramosetron Hydrochloride were prepared by using the solvent casting method. Films were formulated using HPMC E5 (Hydroxy Propyl Methyl Cellulose) as a film-forming agent, PEG400 (Polyethylene glycol) as a plasticizer and Aspartame as the sweetening agent. A 3² full factorial design was applied considering the concentration of HPMC E5 (X₁) and concentration of PEG400 (X₂) as independent variables and % cumulative drug release (Y₁) (CDR), disintegration time (Y₂) (DT) and tensile strength (Y₃) (TS) as dependent variables. The prepared films were evaluated for thickness, folding endurance, tensile strength, disintegration time, drug content uniformity and taste masking by E-tongue. The results indicated that factors X₁ and X₂ were found to be having a positive effect on DT and TS and negative effects on CDR.

Results: The optimized formulation was found to be the best with 94.00±0.85% *in vitro* drug release, 33.22±0.75 sec DT and 1.359±0.005 g/mm² tensile strength. Concentration of aspartame was optimized with E-tongue taking into consideration increased electric potential with decreasing bitterness.

Conclusion: Thus, a rapidly dissolving oral film of Ramosetron Hydrochloride with successful taste masking and immediate *in vitro* drug release was prepared using a solvent casting technique.

Keywords: Ramosetron Hydrochloride, Rapidly dissolving oral film, E-tongue, HPMC E5

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INTRODUCTION

Amongst the different routes, the most agreeable route for the patients is an oral route. But some patients, particularly pediatrics and geriatrics have complications in swallowing or chewing certain oral solid dosage forms like tablets and hard gelatin capsules [1]. Mouth dissolving film (MDF) are a most advanced form of solid dosage form due to various reasons like flexibility, enhanced effectiveness of active pharmaceutical ingredient, dissolution and disintegration within a minute with the help of less amount of saliva as compared to dissolving tablet [2].

Ramosetron Hydrochloride is a white crystalline powder soluble in water and methanol. Ramosetron is a 5-HT₃ receptor antagonist. It exerts its antiemetic property by blocking of serotonin to 5-HT₃ receptors present in the afferent vagal nerve-endings in the GI mucosa. Ramosetron hydrochloride is a new selective 5 hydroxytryptamine type 3 (5-HT₃) receptor antagonists that reportedly has more potent antiemetic effects compared with other 5-HT₃ receptor antagonists [3]. It undergoes hepatic first-pass metabolism. It is found to be more potent and various studies have shown that it is having longer duration of action and least unwanted side effects when compared to other antiemetics [4]. Its conventional tablets are available in the market but the major drawback of that is, tablet does not show the faster onset of action, which is required in case of emesis. Emesis is one of the side effect of cancer treatment and may happens with pregnant women hence our aim is to prepare rapidly dissolving film of Ramosetron hydrochloride for rapid relief in emesis.

MATERIALS AND METHODS

Materials

Ramosetron Hydrochloride was a gratis sample from Cadila Healthcare Kundam, Goa. HPMC E3, HPMC E5, HPMC E15 (Chemdyes), PEG 400, Propylene Glycol, Glycerol (Krishna-Chem Industry), Aspartame (Chemdyes), Methanol (Chemdyes), Ethanol (Chemdyes). All chemicals and reagents used were of AR grade.

Drug polymer compatibility study

Fourier transform infrared spectroscopy (FTIR)

Compatibility studies were performed using the FT-IR spectrophotometer. The IR spectrum of the physical mixture of drug and polymer was studied by making a KBr disc and it was compared with the spectrum of pure drug. The peak in the spectra of physical mixture correlates with the peaks of the drug spectrum. This indicates the drug is compatible with the formulation component.

Differential scanning calorimetric (DSC)

The samples (2-4 mg) were heated in hermetically sealed flat-bottomed aluminum pans under nitrogen flow (20 ml/min) at a scanning rate of 10 °C/min from 25 °C to 200 °C. Empty aluminum pan was used as the reference standard. The instrument was calibrated with the reference standard and scanned over a melting point range.

Preparation of film

Mouth dissolving film of Ramosetron Hydrochloride was prepared by the solvent casting method. The aqueous solution was prepared by dissolving the water-soluble polymer in water. The other ingredients were dissolved in Ethanol 95% solution. Both mixtures were mixed to form homogenous viscous solution. The entrapped air was removed by putting it into sonicator. The resulting solution was casted as a film on a petridish and was allowed to dry. Prepared films were carefully removed from the petridish, checked for any imperfections and then cut into the 2×2 cm², each containing 5 mg Ramosetron Hydrochloride. The films were stored in airtight plastic container till further use.

Preliminary trials

Optimization of film former and plasticizer

The placebo films were prepared using different polymer like HPMC E3, HPMC E5, HPMC E15 and plasticizer in range of 10 to 20 % w/v by the solvent-casting method. Selection of polymer was done on the

basis of appearance, folding endurance, film disintegration time and stickiness. Composition of preliminary batches are shown in table 1.

Optimization of sweetener [5, 6]

Optimization of sweetener was carried out by using different concentration of aspartame and mint flavor. The mouth dissolving films were dissolved in 50 ml of distilled water. The reference electrode, working electrode and counter electrode (sensor array) were dipped in to beaker containing test solution. Potentiometric difference between each individually coated sensor with the Ag/AgCl reference electrode was measured and recorded by the e-tongue software. Each sample was analyzed for 20 sec. The sensor array and reference electrode were then rinsed with distilled water. Using well-conditioned sensor, each sample was usually tested five times by the rotation procedure. The composition of batches is shown in table 2.

Experimental design [7]

In order to investigate the effect of formulation variables on the responses, and to predict an optimized formulation, a 3² factorial design was adopted. Nine batches were prepared as per the design layout shown in table 3. In the present work, a 3² full factorial design was adopted to find out the optimum combination of independent variables, the concentration of HPMC E5 (X₁) and PEG-400 (X₂) to obtain desired values of % Cumulative Drug Release (Y₁), Disintegration Time (Y₂) and Tensile Strength (Y₃). Optimization study was performed using Design-Expert software (version 10). Polynomial models, including interaction terms, were generated for all the three responses. The statistical validity of the mathematical models was established on the basis of Analysis of Variance (ANOVA).

Evaluation parameter

Tensile strength [8]

Tensile strength is the maximum stress applied to a point at which the strip specimen breaks. It was calculated by the applied load at rupture divided by the cross-sectional area of the strip as given in the equation below:

$$\text{Tensile strength} = \frac{\text{Load at failure} \times 100}{\text{Strip thickness} \times \text{Strip width}}$$

Folding endurance [9]

Folding endurance was determined by repeated folding of the strip at the same place till the strip breaks. The number of times the film is folded without breaking was computed as the folding endurance value

Weight variation

For weight variation films were weighed individually on digital balance, then the average weight will be calculated.

Thickness measurement [10]

The thickness of the film (2×2 cm²) was measured by micrometer screw gauge at three different places; averages of three values can be calculated.

In vitro disintegration time [10]

Disintegration time was visually determined by dipping the film (2×2 cm²) in 25 ml water in a beaker. The beaker was shaken gently and the time when the film starts to breaks or disintegrates was recorded.

In vitro dissolution studies [10]

In vitro dissolution time was performed using the USP basket type apparatus. The dissolution studies were carried out at 37±0.5 °C; with a stirring speed of 50 rpm in 300 ml phosphate buffer pH 6.8. Five ml aliquots of dissolution media were collected at predetermined time intervals of 0, 0.3,1,1.3,2,2.3,3,3.4,4,4.4,5,5.5,6 min and replaced with the equal volume of fresh dissolution medium. The collected samples were filtered and the drug release was analyzed spectrophotometrically at 249 nm using UV-Visible spectrophotometer.

Drug content

Fast dissolving film of size (2×2 cm²) was cut into small pieces and transferred into a graduated glass stoppered flask containing about 100 ml of 6.8 pH phosphate buffer. This solution was shaken properly till complete drug dissolves. It was filtered and the amount of drug present was determined after appropriate dilution using a UV-Visible spectrophotometer.

Stability studies [10]

The selected formulation was packed and sealed in aluminum packaging coated inside with polyethylene, they were then stored at 40 °C and 75 % Relative Humidity (RH) for 1 mo and evaluated for their physical appearance, drug content, disintegration time, and *In vitro* % drug release at specified intervals of time and results were reported.

RESULTS AND DISCUSSION

Drug polymer compatibility study

Fourier transform infrared spectroscopy (FTIR)

Compatibility studies were performed using FT-IR spectrophotometer. FTIR spectra of drug and physical mixture is shown in fig. 1a and b. The peak in the spectra of physical mixture correlates with the peaks of the drug spectrum. This indicates the drug is compatible with the formulation component. Also, all the characteristics peaks of drug remain intact in the physical mixture.

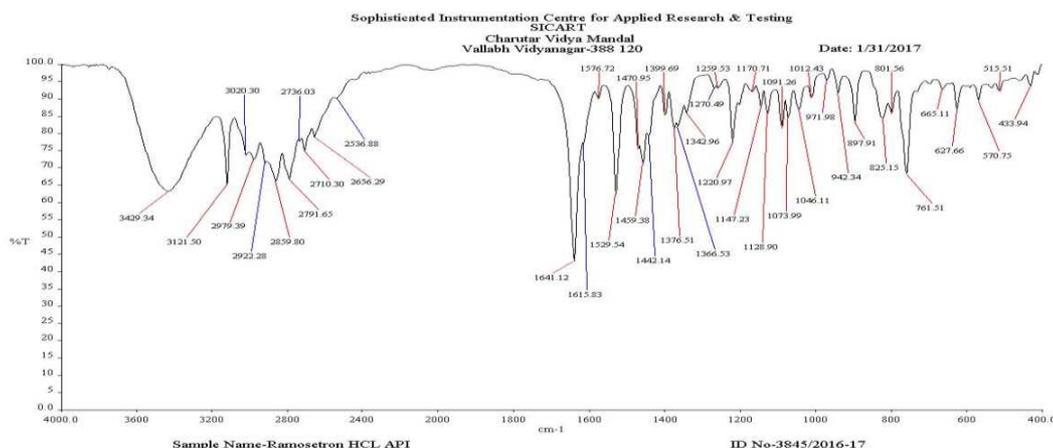


Fig. 1a: FTIR spectra of ramosetron hydrochloride

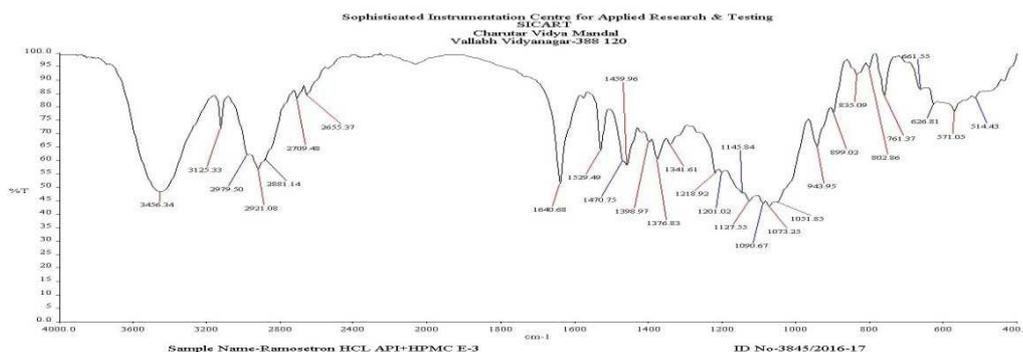


Fig. 1b: FTIR of ramosetron hydrochloride+HPMC5 polymer

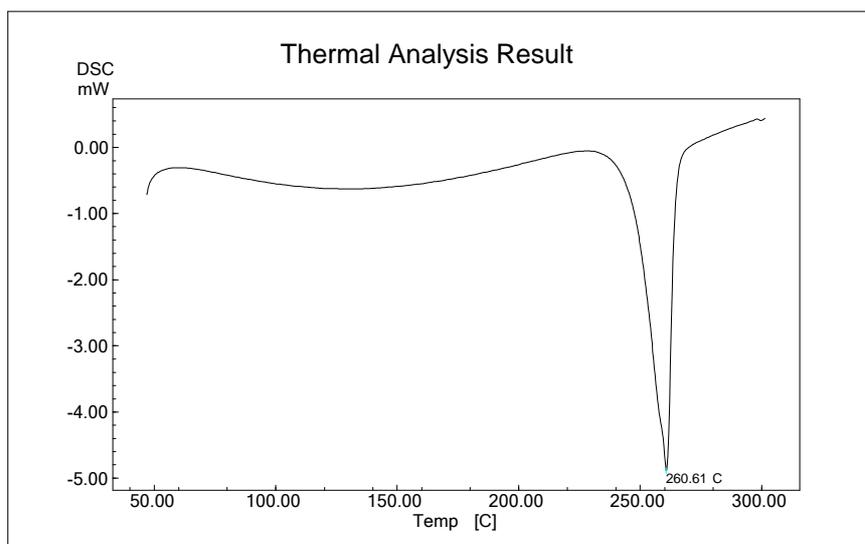


Fig. 2: DSC thermogram of ramosetron hydrochloride

Differential scanning calorimetric (DSC)

Ramosetron Hydrochloride showed sharp endothermic peak at 260.61 °C that corresponds to its melting range as shown in fig. 2.

Preliminary screening studies

Preliminary studies were carried out to optimize the suitable film former polymer, plasticizer and concentration of sweetener, which is capable of producing film of desirable mechanical property and dissolution characteristics.

Optimization of film former and plasticizer

The films formed using HPMC E3 and E15 as a film former and Propylene glycol and Glycerol as plasticizer lacked suitable strength, were fragile having less folding endurance. However, the films with HPMC E5 and PEG 400 (B5) were found to be good in appearance with an acceptable physical characteristic. The films were easy to separate from petridish due to its non-sticky nature. It possessed good folding endurance and disintegration time within a minute. Films prepared using different film former and plasticizer is shown in fig. 3. Composition of preliminary batches and its results are shown in table 1.

Table 1: Preliminary screening MDF batches

Batch	Film forming polymer	Plasticizer	Film former conc. (% w/v)	Plasticize conc. (%w/v)	Appearance	Folding endurance	DT (sec)	Stickiness
1.	HPMC E3	Propylene Glycol	3	10	Good	78	55	Slightly Sticky
2.		Propylene Glycol	5	15	Good	95	61	Sticky
3.		Propylene Glycol	7	20	Good	80	70	Sticky
4.	HPMC E5	PEG 400	3	10	Good	89	47	Not Sticky
5.		PEG 400	5	15	Very Good	102	54	Not Sticky
6.		PEG 400	7	20	Good	99	68	Not Sticky
7.	HPMC E15	Glycerol	3	10	Good	75	53	Slightly Sticky
8.		Glycerol	5	15	Good	92	59	Sticky
9.		Glycerol	7	20	Good	89	75	Very Sticky

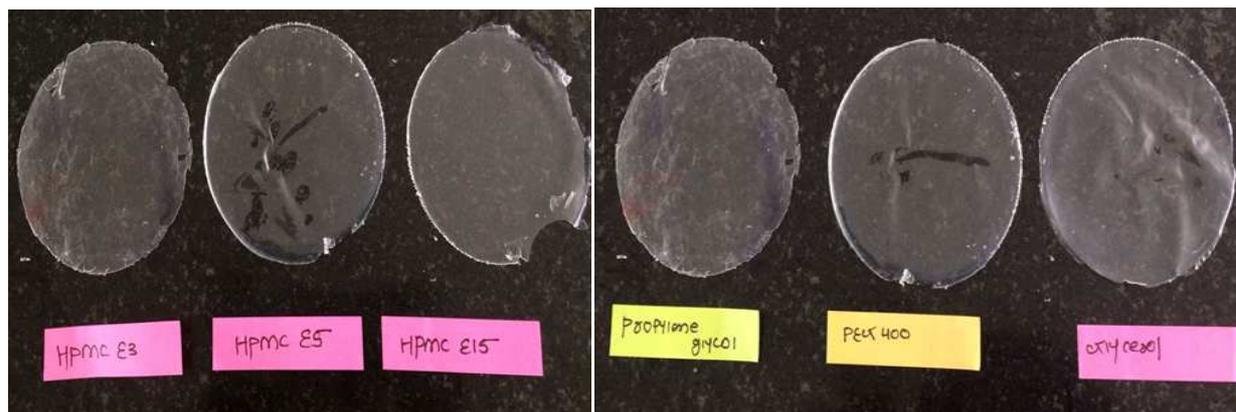


Fig. 3: Films prepared using different film former and plasticizer

Table 2: Batch composition for screening of aspartame concentration

Ingredient	F1	F2	F3	F4
Ramosetron hydrochloride (mg)	73.075	73.075	73.075	73.075
HPMC E5 (mg)	500	500	500	500
PEG 400 (%)	15	15	15	15
Aspartame (mg)	10	20	30	40
Menthol (mg)	40	40	40	40
Ethanol (ml)	7	7	7	7
Distilled Water (ml)	5	5	5	5

Optimization of sweetener

To mask the bitter taste of formulations, sweetener and flavor were incorporated. Aspartame was added as a sweetener in a different concentration (10 to 40 mg) and the mint flavor was added to fulfill the need of flavor. The prepared batches were evaluated for taste masking using E-tongue. The composition of batches is shown in table 2.

The effect of a sweetener, aspartame, on masking Ramosetron Hydrochloride bitterness was evaluated by e-Tongue and a Principal Component Analysis (PCA) map (fig. 4) was configured to determine the system discrimination power between the samples using the data generated. E-Tongue works on the principle that as the bitterness decreases, the electric potential increases. From the PCA map generated, it can be seen that F4 formulation showed the

highest electric potential, hence minimum bitterness value thus sufficiently masking the bitter taste of the drug. F4 was considered as an optimized concentration of sweetener.

Experimental design

3² Factorial designs have often been applied to optimize the formulation variables with basic requirement of understanding the interaction of independent variables. Preliminary investigations of the process parameters revealed that factors like the concentration of HPMC E5 (X₁) and concentration of Plasticizer PEG 400(X₂) showed significant influence on % Cumulative drug release (% CDR) (Y₁), Disintegration time (Y₂) and Tensile strength (Y₃) of drug-loaded mouth dissolving film. Hence, they were utilized for further systematic studies. Composition of the nine batches and its results are shown in table 3a.

Table 3a: 3²Factorial design batches

Batch code	Independent variables		Dependent variable		
	X ₁	X ₂	% Cumulative drug release (%)	Disintegration time (sec)	Tensile strength (g/mm ²)
F1	-1	-1	98.05±0.4	31.04±0.81	0.835±0.003
F2	-1	0	97.43±0.7	33.83±0.53	0.862±0.003
F3	-1	+1	97.03±0.8	36.28±0.65	0.882±0.003
F4	0	-1	96.18±0.6	36.90±0.68	1.531±0.008
F5	0	0	95.48±0.5	38.20±0.91	1.562±0.009
F6	0	+1	94.85±0.7	42.93±0.18	1.678±0.007
F7	+1	-1	90.81±0.7	62.23±0.63	1.893±0.04
F8	+1	0	89.26±0.8	71.08±1.95	2.132±0.006
F9	+1	+1	86.77±0.6	77.12±0.85	2.283±0.01
Independent variables		Low (-1)		High (+1)	
X ₁ -HPMC E5		3%		7%	
X ₂ -PEG 400		10%		20%	

Mathematical relationships, generated using multiple linear regression analysis, gives an insight into the effect of independent variables on the dependent variables. A positive sign of coefficient indicates a synergistic effect, while a negative sign indicates an antagonistic effect

upon the response. For estimation of the significance of the model, ANOVA was performed as per the provision of a Design Expert using 5 % significance level. A model is considered as significant if p<0.05. ANOVA analysis is shown in table 3b.

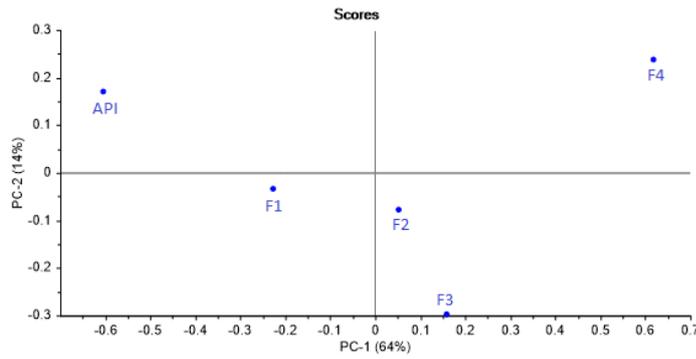


Fig. 4: PCA map of ramosetron hydrochloride in the presence of a different concentration of aspartame

Table 3b: ANOVA Analysis for the 3² experimental design

Source	Y ₁ % cumulative drug release (%)		Y ₂ disintegration time (sec)		Y ₃ tensile strength (g/mm ²)	
	F value	P value	F value	P value	F value	P-value
X ₁	130.62	0.0010	50.75	0.0042	123.79	<0.0001
X ₂	551.11	0.0002	202.30	0.0008	241.65	<0.0001
X ₁₂	11.43	0.0431	2.80	0.1928		
X ₁ ²	57.76	0.0047	32.08	0.0109		
X ₂ ²	0.50	0.5276	2.83	0.1910		
PRESS	7.25		303.10		0.16	
R square	0.9954		0.9883		0.9763	
Adjusted R Square	0.9878		0.9688		0.9685	
Predicted R Square	0.9448		0.8579		0.9345	

The statistically insignificant terms (p>0.05) were omitted to generate the reduced model. Reduced model for each response are shown below:

% Cumulative drug release (%CDR) (Y₁) = +95.77-4.28X₁-1.06X₂-0.76X₁₂-2.40X₁²

Disintegration Time (Y₂) = +36.62+16.74X₁+4.36X₂+11.54X₁²

Tensile Strength (Y₃) = +1.52+0.62X₁+0.097X₂

% Cumulative drug release (%CDR) (Y₁)

Both the independent variables X₁ and X₂ had a negative effect on %CDR. As the concentration of X₁ and X₂ increases from -1 to +1, %CDR was found to be decreasing. This can be clearly seen in the contour plot as shown in fig. 5. In general, it was found that the presence of hydrophilic additive (PEG 400) in HPMC E5 resulted in a rise in the release rate of the drug.

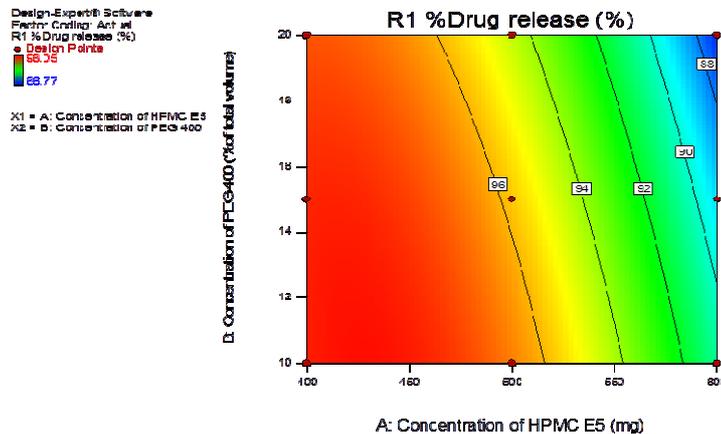


Fig. 5: Contour plot of % CDR

Disintegration time (Y₂)

Disintegration time was found to be increasing with the increasing concentration of X₁ and X₂ as shown in the contour plot (fig. 6). Thus the lower concentration of both the variables are preferred to obtain the fast disintegration of film. The delay in the disintegration time may be the result of increased tensile strength.

Tensile strength (Y₃)

The mechanical properties of cast films were examined by tensile testing. Linear model was suggested showing that tensile strength increased with the increased concentration of PEG 400 and HPMC

E5 as seen from the contour plot (fig. 7). No interaction effect or second-order interaction affected the mechanical strength of the casted films. This might be due to the penetration of PEG chains into HPMC E5, leading to crosslinking and an increase in mechanical strength.

Evaluation parameter

Weight variation

The weight variation for all the formulation is tabulated in table 4. It was found to be in the range of 46.21±0.1 to 70.28±0.5 mg. The weight of all the films was found to be uniform.

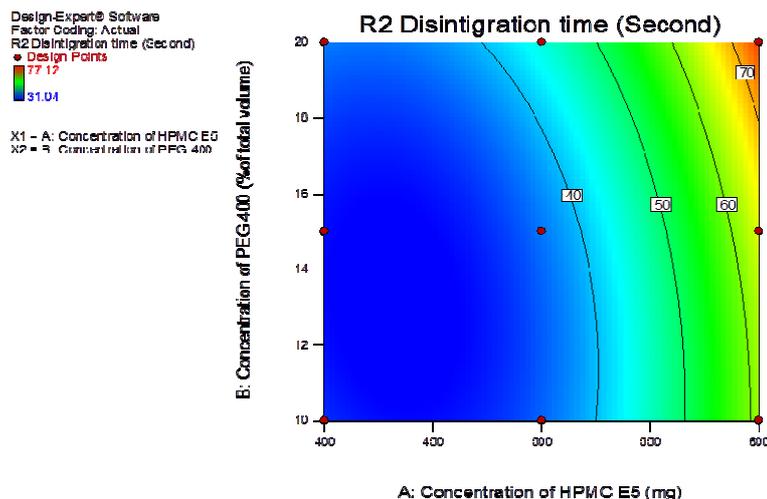


Fig. 6: Contour plot of disintegration time

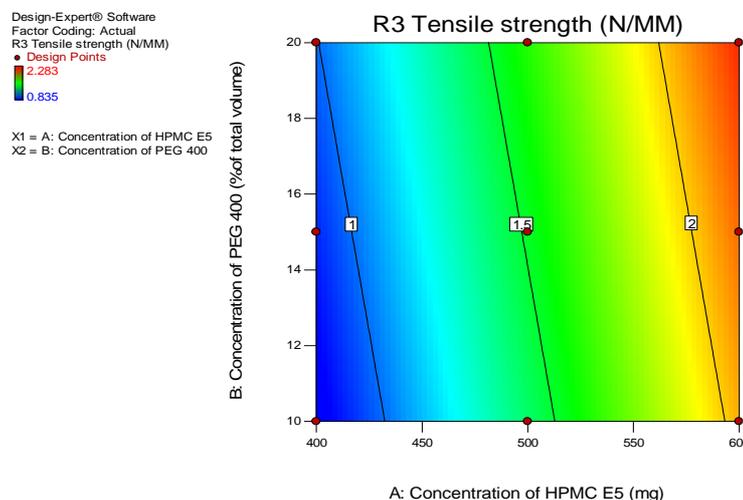


Fig. 7: Contour plot of tensile strength

Thickness

The thickness of the formulated films was found to be in the range of 0.204±0.003 to 0.195±0.002 mm. The mean values are tabulated in table 4. The values indicate that as the concentration of polymer increases, the thickness was found to be gradually increasing. The values are almost uniform in all formulations.

Folding endurance

The folding endurance of formulated films was found to be in range of 95±4.24 to 221±16.26. The mean values are tabulated in table 4. The values indicated that as the concentration of polymer and plasticizer increases, folding endurance was found to be increasing.

Drug content

The drug content was determined to make sure uniform and accurate distribution of the drug. The drug content was performed for all the nine formulations and results are tabulated in table 4. Three trials from each formulation were analyzed spectrophotometrically. The mean value and standard deviation of all the formulations were calculated. The results specified that in all the formulations, the drug content was uniform. The percentage drug released by each film to the *in vitro* release studies was based on the mean content of the drug present in the respective film. The ranges of drug content in all the formulations were 94.63±1.2 % to 99.02±0.35 %.

Table 4: Evaluation of design batches of mouth dissolving films

Batch	Weight variation (mg)	Thickness (mm)	Folding endurance	Drug content (%)
F1	46.21±0.1	0.204±0.003	95±4.24	99.02±0.35
F2	47.98±0.3	0.202±0.003	102±3.53	98.52±0.70
F3	48.30±0.1	0.201±0.004	115±1.41	97.02±0.28
F4	58.02±0.0	0.198±0.002	162±9.89	97.38±1.0
F5	58.56±0.2	0.203±0.002	178±12.02	96.98±0.50
F6	58.98±0.1	0.196±0.004	192±7.77	96.57±0.12
F7	68.67±0.3	0.205±0.004	199±2.82	95.68±1.2
F8	69.33±0.4	0.197±0.003	211±6.36	93.73±0.86
F9	70.28±0.5	0.195±0.002	221±16.26	94.63±1.2

Optimized formulation

The optimized formula was selected based on criteria of maximum % drug release, minimum disintegration time and maximum tensile strength. The overlay plot (fig. 8) was constructed to obtain optimized batch by using Design-Expert version 10. Optimized batch containing HPMC E5 (494.5 mg) and PEG 400 (13.6 mg) was prepared experimentally using the same procedure and same

ingredients, which were utilized in the formulation of 3² full factorial designs. The result of % CDR, disintegration time and tensile strength was compared with that of computed values from the regression equations. When both (experimentally obtained and theoretically computed) values were compared, % error was found to be less than <5% for all responses. This endorsed utility of established contour plots and polynomial equations for all responses. Results of the optimized batch is shown in table 5.

Table 5: Optimized batch evaluation

Responses	Experimental value
% CDR (%)	94.00±0.85
Disintegration time (Sec)	33.22±0.75
Tensile strength (g/mm ²)	1.359±0.005
Thickness(mm)	0.209±0.009
Drug content (%)	97.02±0.742
Folding Endurance	81±5.68
Disintegration time (sec)	33.22±0.75

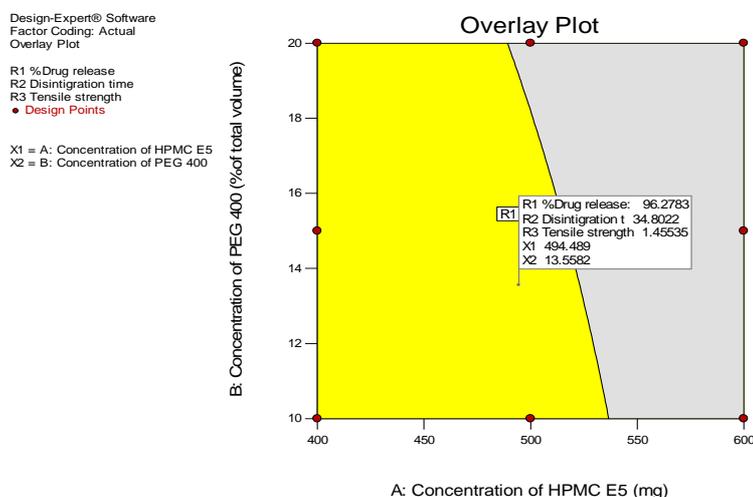


Fig. 8: Overlay plot for checkpoint batch analysis

Stability studies

The accelerated stability studies were carried for the optimized batch as per ICH guidelines. The optimized formulation was evaluated for accelerated stability studies at 40±2 °C/75±5% RH conditions for 1 mo using a stability chamber. The results of stability studies are shown in table 6. At the end of studies, the sample was analyzed for drug

content, disintegration time, tensile strength and folding endurance. Dissolution profile was found to be almost the same in both cases. The data, after the stability period of evaluation parameters were found nearly same as it was before the stability period. Hence stability study indicated that the formulation was quite stable at accelerated conditions. Thus, it can be concluded that the formulation is thermally stable as well as not affected by high humidity conditions.

Table 6: Result of accelerated stability studies

Evaluation parameter	Initial	After 1 mo
Drug content (%)	97.02±0.742	95.83±0.98
% CDR (%)	94.00±0.60	92.76±0.80
Disintegration time (sec)	33.22±0.75	39.27±0.4
Tensile strength(g/mm ²)	1.359±0.005	1.139±0.033
Folding endurance	81±5.68	75±0.65

CONCLUSION

In conclusion, the developed MDF was having enhanced dissolution and acceptable taste masking by the use of a combination of HPMC E5 and PEG 400 in the concentration of 5 % w/v and 15 %w/v respectively. Improved dissolution of the drug may be attributed to the presence of hydrophilic polymer PEG 400. Sufficient taste masking was confirmed by using the e-tongue sensor. The Ramosetron Hydrochloride film possesses adequate mechanical strength and desired rapid disintegration leading to rapid

therapeutic action and can be used as an alternate to the commercially available immediate-release tablets for controlling emesis, resulting in improved patient adherence.

FUNDING

Nil

AUTHORS CONTRIBUTIONS

All the authors have contributed equally.

CONFLICT OF INTERESTS

The authors declare that there is no Conflict of Interest regarding the publication of this paper.

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