

Original Article

FORMULATION AND EVALUATION OF ATORVASTATIN CALCIUM NANOCRYSTALS CONTAINING P-GLYCOPROTEIN INHIBITORS FOR ENHANCING ORAL DELIVERY

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ABSTRACT

Objective: The main objective of this study was to develop atorvastatin calcium (ATR) as an oral drug delivery system for a P-glycoprotein (P-gp) substrate drug using different pharmaceutical excipients that inhibit P-glycoprotein and evaluate the influence of nanocrystals on the dissolution characteristics and bioavailability compared to the plain drug.

Methods: A nanosuspension was prepared by Solvent-antisolvent precipitation method using a solvent containing stabilizer that act as a p-gp inhibitor dissolved in distilled water as polyethylene glycol 300, polyethylene glycol 400 (PEG 300, PEG 400), tween 20 and tween 80 while the solvent selected for atorvastatin calcium was methanol. The concentrations were as follows: PEG 300 and 400 = 0.25% w/v, tween 20 and 80 = 0.75% v/v. Nanocrystals were extracted from the suspension and characterized.

Results: Particle size of the drug was 1307±127.79 nm while the formulas prepared ranged from 223±17.67 to 887±58.12 nm. Pure ATR had a saturated solubility of 0.059±0.005 mg/ml and the prepared nanocrystals ranged from 0.32±0.021 to 0.88±0.019 mg/ml. The Percentage of drug released of plain atorvastatin calcium reached 41.49% while the formula ranged from 44.32 to 61.5%. Both XRD and SEM discussed the degree of crystallinity as follows: F1<F2<F4<F3<ATR.

Conclusion: 0.3% of PEG 300 and PEG 400 were not enough to formulate proper nanocrystals while 0.75% tween 20 and tween 80 achieved acceptable formulas. F4 which is prepared with tween 80 exhibited the highest enhancement in saturated solubility, dissolution rate and subsequently expected to have improved oral bioavailability.

Keywords: Atorvastatin Calcium, Nanocrystals, Antisolvent Precipitation Method, Solubility, Bioavailability, P-glycoprotein

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INTRODUCTION

40% of pharmaceutical compounds are poorly water-soluble which affect the absorption and bioavailability of the drug [1]. Therefore enhancement of the extent of absorption for poorly aqueous soluble drugs intended for oral use is still one of the most critical and challenging approaches in the improvement of dosage forms [2].

One of the approaches to improve the solubility of the drug is to formulate it into nanocrystals which are crystalline particles with at least one dimension measuring less than 1000 nanometers [3]. Nanocrystal formulations can be either partially or completely crystalline depending on the method of formulation and those designed for oral administration have several advantages as the high rate of absorption and oral bioavailability, rapid action, improved dose proportionality, lower required dose and being compatible with all routes of administration in any dosage form [4].

The drug chosen for this study was atorvastatin calcium which is one of HMG CoA reductase inhibitors or statins that can reduce the levels of low-density lipoprotein and triglycerids in the blood while elevating the level of high-density lipoprotein [5]. Atorvastatin is used to treat high cholesterol and to lower the risk of stroke, heart attack and other cardiac complications [5]. It is a class II drug with low aqueous solubility and high intestinal permeability but it is a p-gp substrate drug, therefore it has a low bioavailability of 14% [6, 7].

Permeability glycoprotein (p-gp) is an ATP-dependent efflux pump with broad substrate specificity extensively distributed and expressed in the intestinal epithelium, liver cells, and the capillary endothelial cells composing the blood-brain barrier and blood-testis barrier [8]. As a consequence of its tissue localization and its broad substrate specificity, P-gp plays a key role in the absorption, distribution, and elimination of many drugs thus reducing the

bioavailability and explaining how a drug of high permeability like atorvastatin has a reduced oral bioavailability [9].

The objective of this study is to improve the oral bioavailability of atorvastatin calcium by two means. The first is enhancing the solubility by decreasing the particle size to the nano range and formulation of nanocrystals while the second is augmenting the intestinal absorption through preparing nanocrystals using stabilizers that act as p-gp inhibitors to decrease or eliminate the effect of intestinal efflux on the absorption.

MATERIALS AND METHODS

Atorvastatin Calcium was kindly gifted by Amoun Pharmaceuticals Co., Egypt. Tween 80 and tween 20 were purchased from Lab-scan analytical sciences, Poland. Polyethylene 300 and polyethylene 400 were obtained from Loba Chemie. Methanol HPLC grade was purchased from Sigma-Aldrich co., Germany.

Preparation and extraction of nanocrystals

A nanosuspension was prepared by Solvent-antisolvent precipitation method using a solvent: antisolvent ratio of 25:75 followed by extraction of nanocrystals [10]. The solvent selected to dissolve atorvastatin calcium (ATR) was methanol and supersaturation was achieved at a concentration of 60 mg/ml. The antisolvent contained a hydrophilic stabilizer that act as a p-gp inhibitor dissolved in distilled water. The stabilizers chosen for this study were polyethylene glycol 300, polyethylene glycol 400 (PEG 300, PEG 400), tween 20 and tween 80 [11]. Each one of them was used to prepare an antisolvent with different concentrations and four formulas were evaluated in this study. The concentrations were as follows: PEG 300 and 400 = 0.3% w/v, tween 20 and 80 = 0.75% v/v. The antisolvent was cooled in an ice bath and homogenized

using a mechanical stirrer then the solvent containing the drug was added drop wise. The blend was homogenized for 1 hour. Extraction of the nanocrystals was achieved by solvent evaporation after being left for 24 h to dry at room (25 °C).

Characterization of formulas

Particle size analysis

The mean particle size and polydispersity index (Pdi) were measured at 25±0.5 °C at a measuring angle of 90 ° to the incident beam using Zeta Sizer Nano-ZS, Malvern, UK. ATR powder and nanocrystals were prepared in triplicate by dispersing in deionized water, sonicated for 10 min and filtered before assessment [12].

Scanning electron microscopy (SEM)

A scanning electron microscope (JEOL JSM-5500 LV-JEOL Ltd, Japan) was used to obtain images of the drug and formulas to study their morphology by using high vacuum mode at an accelerating voltage of 20kV. The samples were coated by a gold sputter coater (SPI-Module) and fixed on brass stub using adhesive tape prior to observation [13].

Powder X-ray diffractometry (PXRD)

For further confirmation of the physical state of the drug and formulas, X-ray diffraction patterns were obtained using the X-ray diffractometer (X'Pert-PRO Diffractometer, PANalytical, the Netherlands) with Cu as tube anode. The following conditions were used to record the diffractograms, the voltage was 45 kV, steps were 0.02 ° of (2θ), data were collected from 0 to 70 °2θ, and the counting rate was 0.5 s/step at room temperature [14].

Saturated solubility

Saturated solubility was achieved by adding an excess amount of samples to 50 ml phosphate buffer solution (pH 6.8). The solutions were fixed on a shaking water bath for 48 h at 37±0.5 °C until

equilibrium was attained [15]. The equilibrated samples were centrifuged at 5,000 rpm for 5 min. After decantation, the supernatants were filtered through 0.45µm membrane filter, diluted and assayed using a UV-visible spectrophotometer against a blank at 246 nm [16]. Every sample was analyzed in triplicate and the mean values and standard deviations were reported

In vitro dissolution test

The dissolution studies were performed according to the paddle method (USP) operated at 100rpm using Hanson dissolution apparatus (Hanson Research, California, USA). The dissolution medium was 900 ml of phosphate buffer (pH 6.8), maintained at 37 °C±0.5 °C [17]. Samples containing the equivalent of 20 mg ATR were dispersed in the dissolution medium. 3 ml were withdrawn at different time intervals, filtered through a 0.45µm membrane filter, suitably diluted, and analyzed using a spectrophotometer for ATR content at 246 nm [18]. Withdrawn samples were compensated by fresh medium. The dissolution experiments were conducted in triplicate and calculated mean values of cumulative drug release were used to plot the release curve.

RESULTS AND DISCUSSION

Particle size analysis

Particle size of the drug was 1307±127.79 nm while the formulas prepared ranged from 223±17.67 to 887±58.12 nm. According to the results mentioned in table 1, nanoparticles were formed and their particle size was significantly reduced relative to that of the drug (P 0.05), which proves that the method of preparation and extraction of this study was successful. Samples formulated using tween 80 and 20 had smaller particle size and lower PDI than PEG 300 and PEG 400. PDI of F1 and F2 is lower than 0.5 indicating that the nanoparticle formulation has a high level of distribution homogeneity unlike F3 and F4 [19]. according to both parameters, F1 and F2 are more promising.

Table 1: Particle size, polydispersity index and saturated solubility

Formulas code	Stabilizer used	Mean particle size (nm±SD,n=3)	PDI	Saturated solubility in mg/ml (mean±SD,n=3)
ATR	Pure drug	1307±127.79	0.985	0.059±0.005
F1	PEG 300	887±58.12	0.756	0.31±0.036
F2	PEG 400	753±67.51	0.732	0.42±0.021
F3	T20	341±29.34	0.389	0.59±0.050
F4	T80	223±17.67	0.204	0.88±0.019

Saturated solubility

Results of the saturated solubility studies are indicated in table 1. Pure ATR had a saturated solubility of 0.059±0.005 mg/ml and the prepared nanocrystals ranged from 0.32±0.021 to 0.88±0.019 mg/ml. The saturated solubility of all formulas increased significantly (P<0.05) compared to plain drugs. This result may be due to the significant particle size reduction [20]. F4 showed the lowest particle size and highest saturated solubility (0.88±0.019 mg/ml) compared to the other formulas which confirm that particle size is inversely proportional to solubility [21].

Scanning electron microscopy (SEM)

The shape and surface characteristics of ATR and nanocrystals were visualized using SEM as in fig. 1. Plain Atorvastatin calcium, F3 and F4 have uniform rod-shaped crystals which confirm the success of the antisolvent precipitation method while F1 and F2 showed irregular aggregated particles especially F1, also high degree of tackiness was observed after extraction from nanosuspension, unlike F3 and F4 that yielded free-flowing fine powder. The aggregation and tackiness of F1 and F2 may be caused by the low affinity of PEG 300 and PEG 400 to the newly formed crystal surface or their concentration of (0.3%) was not sufficient to form a protective layer on the crystal surface reduce or prevent stickiness of the crystals formed [14]. This finding suggest that The higher particle size of both F1 and F2 might be attributed to the aggregation rather than to the crystal growth [22]. Also, possible transformation into an amorphous form is suspected in F1, it might be confirmed or denied by the XRD analysis.

In vitro dissolution test

10 samples of each formula were taken in different time intervals in the course of 120 min and the percentage of drug released was calculated. All formulas exhibited higher dissolution characteristics than atorvastatin calcium in phosphate buffer PH (6.8) as shown in table 2. the plain atorvastatin calcium reached 41.49% while the formula ranged from 44.32 to 61.5%.

It was also observed that the cumulative percentage of drug released in F1 and F2 were not significantly higher than drug (P<0.05) and they took a longer time to dissolve completely proofing that the aggregation hindered the dissolution [23]. These findings indicate that 0.3 % of PEG 300 and PEG 400 were not sufficient to achieve better formulas. The dissolution profiles of F3 and F4 showed a significantly improved percentage of drug release and rapid dissolving of powder in the medium [24]. According to this data, F4 is the best formula.

Powder X-ray diffractometry (PXRD)

In fig. 3 X-ray diffraction patterns of drug and formulas were discussed to investigate the presence of any polymorphic transformation. The diffractogram of pure atorvastatin calcium shows sharp characteristic peaks of high intensity which proofs its crystalline nature. Characteristic peaks were spotted at intensity reflection counts of 310.46, 433.3, 750.5 and 358.77 at diffraction angles of (2θ) 16.8739°, 19.2897°, 21.4145° and 23.5345° respectively. These peaks are present in the diffractograms of F3 and F4 at the same diffraction angles but with the decrease in the reflections counts revealing a reduction in

their crystallinity. In F3 peaks are sharp like the drug with a slight decrease in intensity while in F4 the sharpness decreased more as well as their intensity indicating that F3 is slightly lower in crystallinity while F4 is even lower. Drugs with lower crystallinity and smaller particle size have a higher dissolution rate and bioavailability which explains why F4 has the highest solubility and dissolution rate [25, 26]. Distinct decrease in peaks intensity was observed in F2 and some peaks were absent which is attributed to the partial transformation into amorphous form and could be due to the tackiness and

aggregation present in the formula as observed in the SEM image. The characteristic crystalline peaks in F1 appeared broadened and almost distorted as compared to the pure drug confirming the possible transformation into an amorphous form which was suspected from the SEM image and the aggregation that occurred during the preparation of the formula [26]. Despite having a lower level of crystallinity the dissolution wasn't significantly higher which gives further confirmation that aggregation hinders and lowers the solubility and dissolution of formulas.

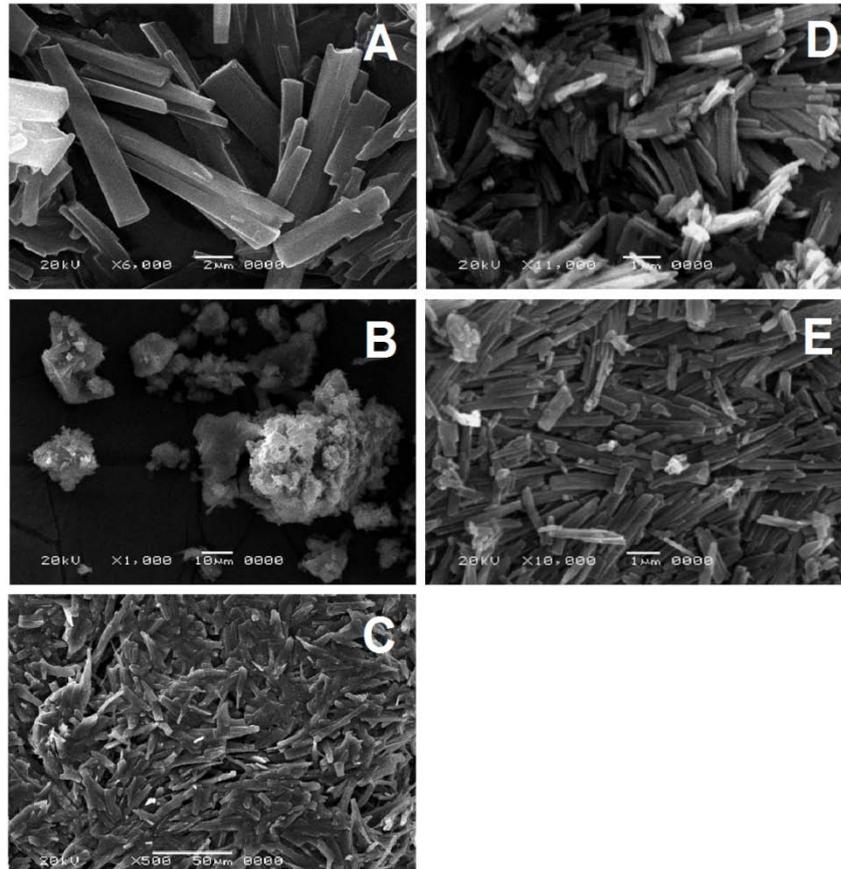


Fig. 1: SEM images of (A) plain atorvastatin, (B) F1, (C) F2, (D) F3, (E) F4

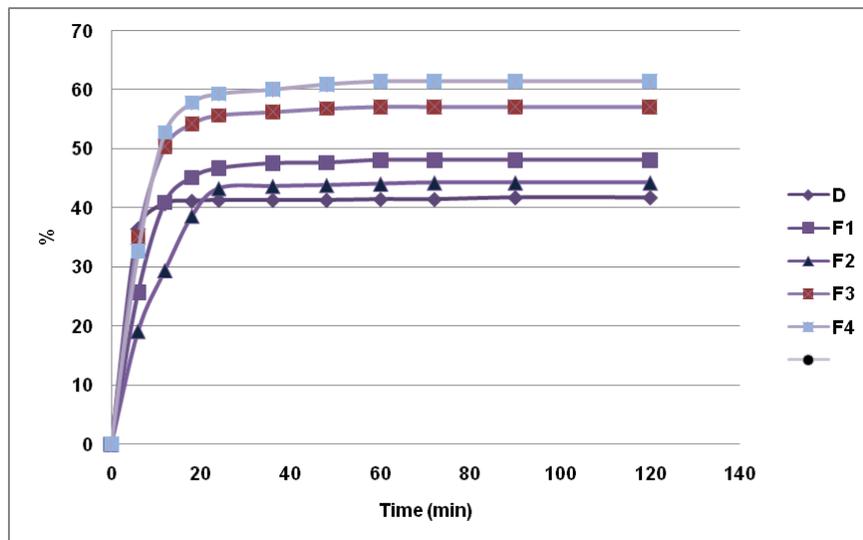


Fig. 2: In vitro drug release profiles of (D) drug and formulas in phosphate buffer pH 6.8

Table 2: *In vitro* drug release profiles of (D) drug and formulas in phosphate buffer pH 6.8

Cumulative % of drug released					
Time (min)	D	F1	F2	F3	F4
0	0	0	0	0	0
6	36.5	19.17	25.76	35.12	32.67
12	40.77	29.48	40.98	50.42	52.8
18	41.2	38.67	45.18	54.31	57.86
24	41.35	43.35	46.72	55.75	59.37
36	41.35	43.71	47.56	56.32	60.1
48	41.35	43.88	47.68	56.89	61
60	41.49	44.12	48.13	57.2	61.5
72	41.49	44.32	48.13	57.2	61.5
90	41.78	44.32	48.13	57.2	61.5
120	41.78	44.32	48.13	57.2	61.5

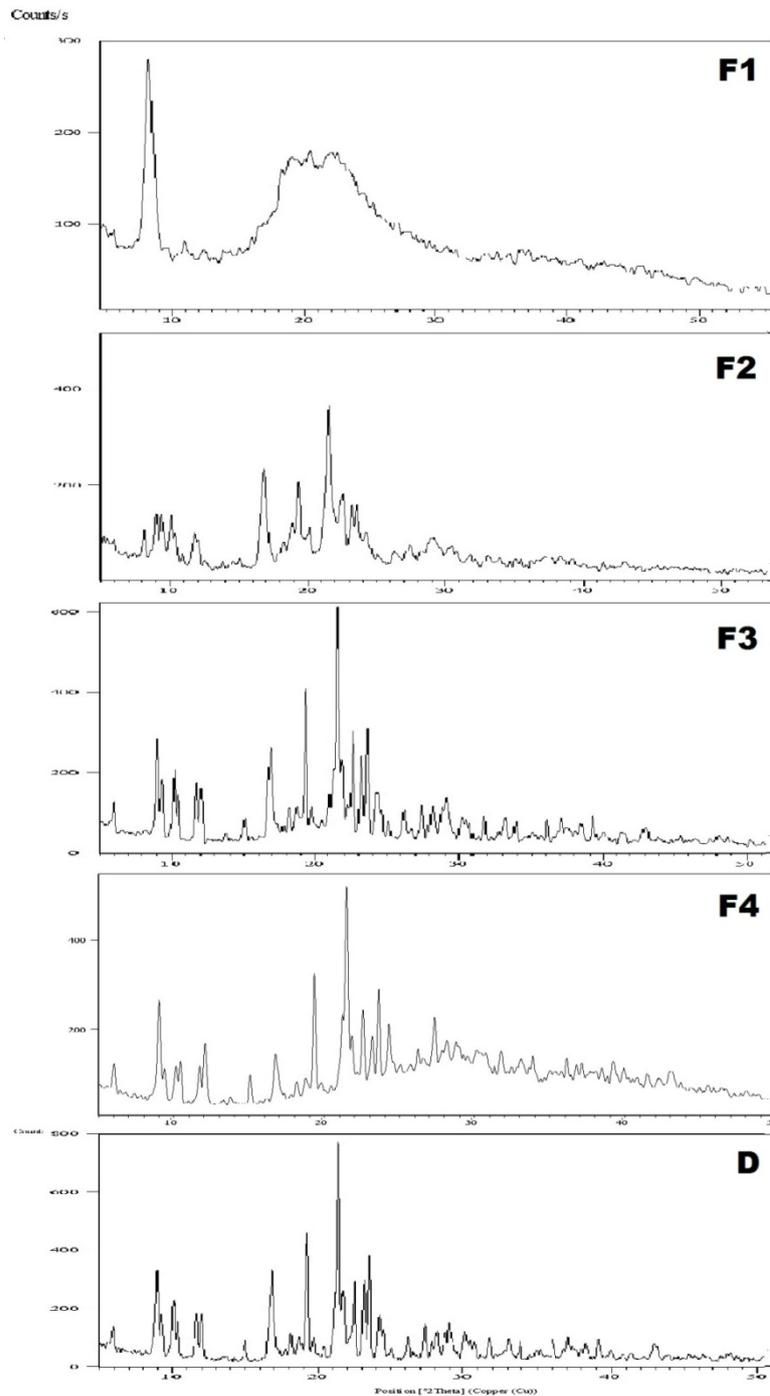


Fig. 3: XRD patterns of (D) plain drug, (F1) formula prepared PEG 300, (F2) by PEG 400, (F3) by tween 20, (F4) by tween 80

CONCLUSION

The method of preparation used was successful to form nanoparticles as shown in the particle size study but the formulas produced have different degrees of crystallinity. The XRD analysis illustrated that the degree of crystallinity was arranged as follows, F1<F2<F4<F3<ATR. Although lower crystallinity means higher solubility and dissolution, they were arranged as follows ATR<F1<F2<F3<F4. It was expected for F1 and F2 to have a higher dissolution rate but they were the least due to the tackiness and aggregation as well as the larger particle size. Both F3 and F4 were significantly enhanced but F4 was the best formula in terms of the degree of saturated solubility and dissolution. It may be attributed to the lower crystallinity of F4, the absence of aggregation and having the lowest particle size. To sum up, 0.3% PEG 300 and PEG 400 were not sufficient to form a protective barrier on the newly formed nanocrystals so preparing formulas with higher concentration was considered and the best formula selected from this study is F4 which is prepared using 0.75% tween 80 as a stabilizer as it showed a marked enhancement in dissolution and subsequently in bioavailability.

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Nil

AUTHORS CONTRIBUTIONS

All the authors have contributed equally.

CONFLICT OF INTERESTS

The authors report no conflicts of interest.

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