DESIGN ZOLMITRIPTAN LIQUISOLID ORODISPERSIBLE TABLETS AND THEIR IN VITRO EVALUATION

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ABSTRACT

Objective: The objective of present study is to develop orodispersible tablets (ODTs) of zolmitriptan by liquisolid technique using different types of super disintegrants to enhance the disintegration and dissolution of zolmitriptan to improve the bioavailability of the drug.

Methods: Liquisolid ODTs of zolmitriptan were prepared from; microcrystalline cellulose (Avicel PH-102) as carrier, colloidal silicon dioxide (Aerosil 200) as a coating material, croscarmellose sodium (CSS), sodium starch glycolate (SSG), and crospovidone (CP) as super disintegrants, and propylene glycol as liquid vehicle. The ratio of carrier to coating material was kept constant in all formulations at 35:1, this ratio was chosen after testing the ratios 10:1, 15:1, 20:1, 25:1, 30:1, and 35:1. The ratio 35:1 give optimal results relative to other ratios. The pre-compression evaluation includes: flow properties were measured using the angle of repose and the compressibility index and FT-IR. The prepared liquid-sold system compacts were evaluated for their post-compression evaluation which includes: hardness, friability, wetting time, in vitro disintegration time, drug content and in vitro drug release.

Results: The tabletting properties of the liquid-solid ODTs were within the acceptable limits. Among the three super disintegrants, CP found to be the best in term of showing the fastest disintegration time. The optimized selected formula (F11) was prepared using 5% w/w crospovidone, by direct compression showed the shortest disintegration time (24 s), superior drug release profile [ the time required for 80% of the drug to be released (T 80%) and percent drug dissolved in 2 min (D 2 min) 1.84 min and 87.59%, respectively]. In addition to that, the selected formula had an acceptable hardness and friability, so it was selected as the best formula.

Conclusion: The overall results showed that CP was the best super disintegrant of showing the shortest disintegration time while loading factor of 0.125 was the best in the preparing of zolmitriptan liquid-solid ODTs, and this suggested the possibility of utilizing the selected best formula (F11) in the preparation of zolmitriptan ODTs as a new dosage form for oral administration.

Keywords: Orodispersible tablet, Zolmitriptan, Liquisolid technique

INTRODUCTION

Many newly developed drugs are poorly water soluble compounds, which lead to problems in the development of dosage forms with sufficient bioavailability [1]. Solubility is the most important parameter to achieve the desired concentration of the drug in the systemic circulation for therapeutic response to be shown [2]. The majority of the hydrophobic drugs are sparingly soluble, slightly soluble, very slightly soluble and practically insoluble drugs. For each drug substances mentioned above, the dissolution is the rate-limiting step, so, the challenges for absorption of poorly water-soluble drugs are to improve the dissolution rate. This lead to enhancement of the absorption and bioavailability of these drugs [3].

The term liquid-solid system refers to the powdered forms of liquid drugs formulated by changing liquid lipophilic drugs, drug suspensions or solutions of water-insoluble solids in suitable non-volatile vehicle systems into dry, non-adherent, freely flowing and readily compressible powder mixtures by simple mixing with selected powder excipients known as the carrier and coating materials. Generally, microcrystalline cellulose (Avicol) is utilised as the carrier material and amorphous silicon dioxide (colloidal silica) as a coating material [4].

Many patient groups like elderly, children and mentally retarded patients who are uncooperative, nauseated or on decreased liquid intake/diets have difficulties in swallowing the solid dosage forms. Those who are travelling or have little water access are evenly affected [5]. To accomplish these medical needs, pharmaceutical technologists have developed a patient-friendly novel oral dosage form known as “Orally Disintegrating Tablets” which disintegrate rapidly in saliva, usually within seconds, without needing for water. Drug dissolution, absorption, the onset of therapeutic effect and drug bioavailability may be significantly better than those obtained from conventional dosage forms [6].

Zolmitriptan (4S)-4-[[2-dimethylamino ethyl]-1Hindol-5-yl] methyl oxazolidinone, is a white to almost white powder, slightly soluble in water. It has a pKa value of 9.6. The bioavailability of zolmitriptan is about 40% from oral and nasal dosage forms and problem arises from its low water solubility and dissolution rate. Zolmitriptan used for patients with migraine attacks, with or without an aura, and cluster headaches. It acts selectively on serotonin (5-HT1B/1D) receptors. It is presently available as a conventional tablet, an oral disintegrating tablet and a nasal spray (2.5 mg and 5 mg per dose) [7, 8]. Patients with a migraine generally suffer from nausea and vomiting. Furthermore, in migraine attack there is delayed gastric emptying with a resulting delayed absorption during attacks; therefore, oral treatment could be inconvenient or could fail. Therefore, zolmitriptan given as ODT might provide rapid-acting, non-invasive delivery system for anti-migraine drugs to enhance patient compliance [9]. The aim behind this study is to prepare and evaluate zolmitriptan as an ODTs by liquid solid systems technique to enhance the disintegration and dissolution of zolmitriptan to improve the bioavailability of the drug.

MATERIALS AND METHODS

Materials

Zolmitriptan, microcrystalline cellulose (Avicel PH-102), silicon dioxide (Aerosil 200), croscarmellose sodium, crospovidone, sodium starch glycolate are obtained by Hangzhou Hyper Chemicals Limited, China. Propylene glycol (PG) was purchased from Fluka Chemi AG,
Switzerland. Sodium saccharin, vanillin, disodium hydrogen orthophosphate and potassium dihydrogen orthophosphate were purchased from BDH chemical LTD, UK.

**Methods**

**Solubility studies**

Solubility studies of zolmitriptan were carried out in PG, PEG 400 and tween 80 to select the best non-volatile solvent for the dissolving of zolmitriptan in a liquid vehicle. Also simulated gastric fluid (SGF), pH 1.2 and simulated intestinal fluid (SIF), pH 6.8 were utilised to study solubility behaviour of zolmitriptan. Saturated solutions were prepared by adding much of zolmitriptan to the vehicles and shaking with the shaker for 48 h with a constant vibration. Then the solutions were filtered through a 0.45 mm millipore filter, diluted and analysed by UV-spectrophotometer. The sample was analysed in triplicate to calculate the solubility of zolmitriptan [10].

**Use of a mathematical model to design solid-liquid systems**

The flowability and compressibility of liquid solid compacts are addressed simultaneously in the new formulation mathematical model of liquid solid systems, which was used to calculate the appropriate quantities of the carrier and coating materials required to produce acceptably flowing and compressible powders based on new fundamental powder properties called the flowable liquid retention potential (Φ-value) and compressible liquid retention potential (Ψ-number) of the constituent powders. The flowable liquid retention potential of powder is defined as the maximum amount of a given non-volatile liquid that can be retained inside its bulk (w/w) while maintaining acceptable flowability [11].

The compressible liquid retention potential (Ψ) of powder is the maximum amount of liquid; the powder can retain inside its bulk (w/w) while maintaining acceptable compact ability, to produce compacts of suitable hardness and friability, with no liquid squeezing out phenomenon during the compression process. The Φ value of powders may be determined using a new procedure, the liquid solid flowability (LSF) test. The Φ number of powders may be determined using a new method termed the liquid solid compressibility (LSC) test which employs the 'pactisity theories' to evaluate the compaction properties of liquid/powder admixtures. According to the new theories, the carrier and coating powder materials can retain only certain amounts of liquid while maintaining acceptable flow and compression properties [12]. Depending on the excipients ratio (R) or the carrier: coating ratio of the powder system used, where,

\[ R = \frac{Q}{q} \]  

As R represents the ratio between the weights of carrier (Q) and coating (q) materials present in the formulation. An acceptably flowing and compressible liquid solid system can be prepared only if a maximum liquid on the carrier material is not exceeded; such a characteristic amount of liquid is termed the liquid load factor (Lf) and defined as the ratio of the weight of liquid medication (W) over the weight of the carrier powder (Q) in the system, which should be possessed by an acceptably flowing and compressible liquid solid system.

\[ Lf = \frac{W}{Q} \]  

The powder excipients ratios R and liquid load factors Lf of the formulations is related as follows:

\[ \Psi Lf = \Psi Lf = \Phi(1/R) \]  

In order to calculate the required ingredient quantities, the flowable liquid retention potentials (Φ-values) of powder excipients were utilised. So to calculate the required weights of the excipients used, first, from Eq. (3), Φ and Φ are constants, therefore, according to the ratio of the carrier/coat materials (R), Lf was calculated from the linear relationship of Lf versus 1/R. Next, according to the used liquid vehicle concentration, different weights of the liquid drug solution (W) will be used. So, by knowing both Lf and W, the appropriate quantities of the carrier (Q) and coating (q) powder materials required to convert a given amount of liquid medication (W) into an acceptably flowing and compressible liquid solid system could be calculated from equations (1) and (2).

**Formulation of liquid solid ODTs of zolmitriptan**

Various liquid solid ODTs formulas denoted (F1 to F11) as shown in table (1) containing 2.5 mg of zolmitriptan were prepared by dispersing the drug in the non-volatile vehicle (PG). Then a bindery mixture of carrier (Avecil PH 102) and coating material (Aerosil 200) was prepared at a ratio of 35:1 (trial and error methods were used, i.e. changing the carrier; coating material ratio (R) from 10, 15, 20, 25, 30, and 35:1 until get good result (flow properties) is obtained. R 35 was used in all formulations since it gave the optimal flow property. This binary mixture was added to the admixture of drug and vehicle. Finally, super disintegrant and other excipients were added to the above powder blend and mixed thoroughly. The final powder blend was subjected to direct compression [13]. The formulas F1-F9 were prepared using different types and concentrations (2.5%, 5%, and 7.5%) of super disintegrants namely CSS, SSg, and CP. The loading factor was kept constant in the above formulations which equal to 0.25; this loading factor was decreased to 50% from its original value in formula F10 to become 0.175, while in formula F11, the loading factor 0.25 was decreased to 100% to become 0.125.

<table>
<thead>
<tr>
<th>Code</th>
<th>CSS (mg)</th>
<th>SSg (mg)</th>
<th>CP (mg)</th>
<th>Avicel PH-102 (mg)</th>
<th>Aerosol 200 (mg)</th>
<th>Na saccharin 1% (mg)</th>
<th>Vanillin 1% (mg)</th>
<th>Mg stearate 1% (mg)</th>
<th>Total weight (mg)</th>
</tr>
</thead>
<tbody>
<tr>
<td>F1</td>
<td>3.5</td>
<td>104.5</td>
<td>101</td>
<td>7 (5%)</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F2</td>
<td>2</td>
<td>104.5</td>
<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F3</td>
<td>7 (5%)</td>
<td>104.5</td>
<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F4</td>
<td>3.5</td>
<td>104.5</td>
<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F5</td>
<td>7 (5%)</td>
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<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F6</td>
<td>10.5</td>
<td>104.5</td>
<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F7</td>
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<td>104.5</td>
<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F8</td>
<td>7 (5%)</td>
<td>104.5</td>
<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F9</td>
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<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F10</td>
<td>9.3</td>
<td>104.5</td>
<td>97.5</td>
<td>140</td>
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<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>F11</td>
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<td>104.5</td>
<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>140</td>
</tr>
<tr>
<td>DCT</td>
<td>12.5</td>
<td>104.5</td>
<td>97.5</td>
<td>140</td>
<td>2.8</td>
<td>1.4</td>
<td>1.4</td>
<td>1.4</td>
<td>250</td>
</tr>
</tbody>
</table>

*Each formula contains 2.5 mg zolmitriptan*
Preparation of directly compressible ODTs (DCT) of zolmitriptan

Directly compressible ODTs (DCT) of zolmitriptan were prepared by direct compression using single tablet punch machine, each containing 2.5 mg zolmitriptan, 221.2 mg Avicel PH 102, 6.31 mg Aerosil 200 (ratio of Avicel PH-102 to Aerosil 200 was set at 35:1), 5% w/w CP as super disintegrant, and 1% w/w of magnesium stearate, sodium saccharin, and vanillin, respectively. These tablets were prepared by mixing the drug with Avicel PH-102 and Aerosil 200 for a period of 10 min. The blend was mixed with CP and other additives for 10 min then magnesium stearate was added and mixed for 2 min. After that, the final mixture was directly compressed using a single punch tabletting machine 8 mm die size [14].

Pre-compression evaluation of zolmitriptan liquid solid ODTs

The flow properties of the liquid, solid systems were of critical importance in the production of pharmaceutical dosage forms in order to get a uniform feed, as well as the reproducible filling of tablet, dies otherwise high dose weight variations will occur. The flow properties of the liquid solid powders were estimated by determining the angle of repose and Carr’s index. The angle of repose was measured by the fixed funnel method. The bulk density and tap density were determined for the calculation of Carr’s index [15, 16].

Post-compression evaluation of zolmitriptan liquid solid ODTs

Hardness test

A hardness tester apparatus (Monsanto) was used to determine the tablet hardness. Three tablets were randomly selected from each batch of ODTs tablets for determination of hardness. The mean of three determination±SD was recorded. The hardness was expressed as a force in kg/cm² required to crush the tablets [17].

Friability test

Friability test was performed to evaluate the effect of friction and shocks, which may often cause tablets to chip, cap or break. Roche friabilator apparatus was used for this purpose. It is expressed as a percentage (%). Ten tablets were initially weighed (W initial) and put in the friabilator. The friabilator was operated at up to 100 revolutions. The tablets were weighed again (W final). The percentage friability was then calculated using the following equation:

\[
\% \text{ Friability} = \frac{W \text{ initial} - W \text{ final}}{W \text{ initial}} \times 100 \% \quad (6)
\]

Content uniformity test

Ten tablets from each batch were grounded in a mortar to a fine powder then powder mass equivalent to 2.5 mg of zolmitriptan was transferred into 100 ml volumetric flask, then the volume was completed to 100 ml with phosphate buffer (pH 6.8). The solution was sonicated and shaken intermittently for 1 h sonication and filtered. After the desired dilution, the solution was analysed for drug content at λ max 222 nm with a UV-Visible spectrophotometer using phosphate buffer (pH 6.8) as blank [19].

Wetting time test

The wetting time of tablets was measured using a simple procedure. A piece of sponge (0.5 cm thickness) was placed in a small Petri dish (internal diameter =12 cm) containing 10 ml of artificial saliva containing methylene blue (a water soluble dye). The dye solution is utilized to recognize the complete wetting of the tablet surface. The method was performed by maintaining artificial saliva at 37 °C. A tablet was placed on the sponge surface carefully and the time required for the complete wetting of the tablet was recorded as a wetting time as shown in fig. [1]. The mean of three determinations was used±SD. The artificial saliva used was composed of NaCl (8 g/l), KH₂PO₄ (0.19 g/l) and Na₂HPO₄ (2.38 g/l) [20].

Conventional disintegration tests show not to be reflective of the disintegration time in the human mouth. To overcome this problem, a new modified apparatus represented as a suitable method to determine the disintegration time of ODTs was developed. A modified apparatus fig. (2) Consisting of a glass beaker of 10 ml capacity contained 6 ml of salivary phosphate buffer pH 6.8 as a disintegration medium placed on the magnetic stirrer. A very small magnetic bead was put at the bottom of a beaker and temperature was maintained at 37±2 °C. Disintegration time was determined at 50 rpm. The disintegration test was performed on six tablets [21, 22].

In vitro disintegration time test

One of the most important characteristics of the ODT is the disintegration time in the oral cavity; yet, the disintegration time of ODTs is measured using the conventional tests (for tablets) that were described in the Pharmacopoeias. However, it is hard to determine the disintegration time for the ODT with these tests due to its rapid disintegration rate even in a small amount of water. Further, the conventional tests use a volume of 800-900 ml of the test solution compared to the volume of saliva in humans, which is less than 6 ml. Thus, the disintegration time obtained from the conventional disintegration tests show not to be reflective of the disintegration time in the human mouth. To overcome this problem, a new modified apparatus represented as a suitable method to determine the disintegration time of ODTs was developed. A modified apparatus fig. (2) Consisting of a glass beaker of 10 ml capacity contained 6 ml of salivary phosphate buffer pH 6.8 as a disintegration medium placed on the magnetic stirrer. A very small magnetic bead was put at the bottom of a beaker and temperature was maintained at 37±2 °C. Disintegration time was determined at 50 rpm. The disintegration test was performed on six tablets [21, 22].
In vitro dissolution studies of zolmitriptan liquisolid ODTs

The release profile of selected formula of zolmitriptan liquisolid orodispersible tablets was performed in 500 ml phosphate buffer pH 6.8 maintained at 37±0.5 °C using the USP Dissolution Tester Apparatus II, at a rotation speed of 50 rpm. Also, dissolution study was performed for DCT. Aliquots from the dissolution medium (5 ml) were withdrawn at 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 12.5, 15, 20, 25 and 30 min time intervals. The samples were replaced with fresh dissolution medium of same quantity in order to maintain the volume in the vessels constant. Samples were filtered using 0.45 millipore filter and drug content was determined spectrophotometrically at λ max 222 nm. The percentage of drug dissolved in 2 min (D 2 min) and the time required for 80% of drug to be released (T 80%) were considered for comparing the dissolution results for the prepared zolmitriptan liquisolid ODTs formula and DCT. Each preparation was tested in triplicate and the mean value was calculated [23].

Fourier transform infrared spectroscopy (FT-IR)

This study was achieved to identify any sign of complexation and interaction between zolmitriptan and other excipients used in the preparation of zolmitriptan liquisolid ODTs. The samples are ground and mixed with potassium bromide. The spectrum was obtained between the wave number of 4000-400 cm⁻¹

<table>
<thead>
<tr>
<th>Solvents</th>
<th>Solubility (% w/w) meansSD*</th>
</tr>
</thead>
<tbody>
<tr>
<td>Distilled water</td>
<td>0.122±0.0546</td>
</tr>
<tr>
<td>(0.1 N HCl)</td>
<td>1.873±0.1162</td>
</tr>
<tr>
<td>(phosphate buffer pH 6.8)</td>
<td>0.235±0.0972</td>
</tr>
<tr>
<td>PG</td>
<td>7.721±0.6553</td>
</tr>
<tr>
<td>PEG 400</td>
<td>0.737±0.0475</td>
</tr>
<tr>
<td>Tween 80</td>
<td>0.132±0.0126</td>
</tr>
</tbody>
</table>

*SD standard deviation from mean. n=3

Application of new mathematical model for design of liquisolid systems

In order to calculate the required ingredient quantities, the flowable liquid retention potentials (Φ-values) of powder excipients were utilised. The values of the flowable liquid retention potentials for Avicel PH-102 and Aerosil 200 in PG were (0.16) and (3.33), respectively [11,12]. The loading factor (Lf) was calculated from the following equation:

Lf = 0.16 + 3.33 (1/35) for PG ........... (7)

The optimal R-value was 35:1, the corresponding optimal liquid load factor of a given excipients ratio was established. The appropriate quantities of Avicel PH 102 (Q) and Aerosil 200 (q) required to convert a given amount of liquid medication (W) into an acceptably flowing and compressible liquisolid system, were calculated using Eqs. (1) and (2), and it was equal to 0.25. A reasonable flow was achieved when the liquid loading factors (Lf) equal to or lower than 0.25, this is in agreement with what was stated in literature that it is hard to prepare formulation with good flowability and compactibility when loading factor is above 0.25, because fewer amounts of carrier and coating materials are used during preparation of these formulations, and excess liquid is not completely absorbed, leading to the formation of agglomerates [27].

Pre-compression studies of the prepared liquisolid orodispersible powder system

The data obtained for pre-compression parameters for formulas F1-F11 and DCT such as carr’s index and angle of repose are shown in table (3) and was within acceptable limits according to USP [28].

<table>
<thead>
<tr>
<th>Formula no.</th>
<th>Angle of repose*</th>
<th>Carr’s index*</th>
<th>Flow-compression character</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>3.4±0.22</td>
<td>19.6±0.47</td>
<td>Good to fair</td>
</tr>
<tr>
<td>2</td>
<td>3.4±0.179</td>
<td>18.4±0.79</td>
<td>Good to fair</td>
</tr>
<tr>
<td>3</td>
<td>2.6±0.194</td>
<td>19.4±0.85</td>
<td>Good to fair</td>
</tr>
<tr>
<td>4</td>
<td>3.3±0.70</td>
<td>18.8±1.62</td>
<td>Good to fair</td>
</tr>
<tr>
<td>5</td>
<td>3.3±0.206</td>
<td>16.7±1.42</td>
<td>Good to fair</td>
</tr>
<tr>
<td>6</td>
<td>3.2±0.55</td>
<td>16.6±2.12</td>
<td>Good to fair</td>
</tr>
<tr>
<td>7</td>
<td>3.0±0.69</td>
<td>15.7±2.39</td>
<td>Excellent to Good</td>
</tr>
<tr>
<td>8</td>
<td>3.0±0.65</td>
<td>14.3±0.56</td>
<td>Excellent to Good</td>
</tr>
<tr>
<td>9</td>
<td>2.9±0.47</td>
<td>12.6±0.91</td>
<td>Excellent to Good</td>
</tr>
<tr>
<td>10</td>
<td>2.7±0.87</td>
<td>14.3±0.94</td>
<td>Excellent to Good</td>
</tr>
<tr>
<td>11</td>
<td>2.5±1.80</td>
<td>15.1±0.91</td>
<td>Excellent to Good</td>
</tr>
<tr>
<td>DCT</td>
<td>3.2±0.57</td>
<td>19.2±0.219</td>
<td>Good to Fair</td>
</tr>
</tbody>
</table>

*SD standard deviation from mean. n=3.
Post-compression evaluation of zolmitriptan liquidosil ODTs: hardness, friability, and content uniformity

Post-compression parameters like hardness, friability and content uniformity were mentioned in table (4). The tablets measured hardness was found to be in the range of 3.03 to 4.75 kg/cm². The percentage of friability was less than 1% for all formulations ensuring the optimum mechanical stability of the formulated tablets. The percentage of the drug content for all formulas was found in the range of 97.4-100.6% which comply with the USP limits [28].

Table 4: Hardness, friability, content uniformity percentage, wetting time and disintegration time of zolmitriptan liquidosil orodispersible tablets

<table>
<thead>
<tr>
<th>Formula code</th>
<th>Hardness kg/cm² mean±SD, n=3</th>
<th>% Friability (w/w) Mean, n=10</th>
<th>% content uniformity mean±SD, n=10</th>
<th>Wetting time Mean (s)±SD, n=3</th>
<th>Disintegration time Mean(s)±SD, n=6</th>
</tr>
</thead>
<tbody>
<tr>
<td>F1</td>
<td>4.20±0.20</td>
<td>0.72</td>
<td>95.4±2.07</td>
<td>288±7.45</td>
<td>185±3.97</td>
</tr>
<tr>
<td>F2</td>
<td>4.13±0.05</td>
<td>0.86</td>
<td>98.6±3.20</td>
<td>253±5.54</td>
<td>201±7.52</td>
</tr>
<tr>
<td>F3</td>
<td>3.90±0.26</td>
<td>0.46</td>
<td>99.6±4.15</td>
<td>217±8.61</td>
<td>221±7.78</td>
</tr>
<tr>
<td>F4</td>
<td>3.70±0.17</td>
<td>0.40</td>
<td>100.2±2.16</td>
<td>246±7.57</td>
<td>126±6.22</td>
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<tr>
<td>F5</td>
<td>3.36±0.11</td>
<td>0.89</td>
<td>97.8±2.68</td>
<td>207±5.72</td>
<td>101±3.09</td>
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<tr>
<td>F6</td>
<td>3.03±0.15</td>
<td>0.73</td>
<td>100.6±2.70</td>
<td>167±9.45</td>
<td>118±5.33</td>
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<tr>
<td>F7</td>
<td>4.00±0.00</td>
<td>0.21</td>
<td>97.4±3.50</td>
<td>76±3.31</td>
<td>79±2.40</td>
</tr>
<tr>
<td>F8</td>
<td>4.23±0.20</td>
<td>0.75</td>
<td>100.8±2.03</td>
<td>68±3.12</td>
<td>48±1.63</td>
</tr>
<tr>
<td>F9</td>
<td>4.75±0.25</td>
<td>0.28</td>
<td>99.8±3.91</td>
<td>53±5.34</td>
<td>61±3.73</td>
</tr>
<tr>
<td>F10</td>
<td>4.10±0.42</td>
<td>0.70</td>
<td>98.8±2.38</td>
<td>54±2.74</td>
<td>33±2.43</td>
</tr>
<tr>
<td>F11</td>
<td>4.11±0.39</td>
<td>0.35</td>
<td>100.2±1.30</td>
<td>40±1.41</td>
<td>24±1.53</td>
</tr>
<tr>
<td>DCT</td>
<td>4.29±0.29</td>
<td>0.66</td>
<td>100.2±2.23</td>
<td>71±2.37</td>
<td>44±3.17</td>
</tr>
</tbody>
</table>

Wetting time (WT) and In vitro disintegration time (DT)

The wetting and disintegration behaviour of the prepared zolmitriptan liquidosil ODTs in salivary phosphate buffer pH 6.8 were shown in the table (4). It was observed that the WT and DT for F1-F9 formulas were influenced by the type and concentration of super disintegrant. Table (4) shows that the best super disintegrant type was CP among the other super disintegrants CCS and SSg; this is due to the fact that CP rapidly wicks water into the tablet to create the volume expansion and hydrostatic pressure required to provide rapid disintegration. The results are in agreement with those reported in the literature [29]. Concerning the concentration of the super disintegrant, a rational concentration should be utilized in the formulation of ODTs, because increasing the concentration over an optimum one lead to an increase in the DT of the tablet. From data in table (4), as the concentration of the super disintegrant increase, the DT consistently increase. This increase in DT was more marked in formulas F3, F6 and less in F9. The reason behind this increase may be due to the formation of viscous gel layer on the surface of the tablet which prevents the penetration of water to the core of the tablet especially for super disintegrant CCS and SSg [30], as shown in fig. (3). More gel was formed with CCS than with SSg. This makes DT of tablets with super disintegrant CCS more than that of tablets with SSg (DT of tablets prepared with CCS 7.5% (F3) and SSg 7.5% (F6) were 221 and 118 s, respectively). In contrast, CP has less tendency to gelling [29]. In F9 which contains 7.5% CP there is a slight increase in DT, because the quick expansion of the largest capillaries isolates other areas of fine pores structure in which air cannot escape. These areas make no role to the overall uptake of liquid [31]. Moreover, it can be concluded that as the concentration of the super disintegrant increase, the WT decrease.

The formulas F10 and F11 were prepared with the loading factors 0.175 and 0.125, respectively, and their WT and DT were compared to the formula F8 with a loading factor of 0.25. From the results shown in table (4), a significant (p<0.05) decrease in the WT and DT was seen as the loading factor was decreased. This is due to that as the loading factor decrease, the amount of Avicel PH-102 will decrease. This is due to that as the loading factor decrease, the amount of Avicel PH-102 will increase according to the equation L=W/Q, where Q is the weight of Avicel PH-102. Microcrystalline cellulose (Avicel PH-102) has a very high intraparticle porosity. This high porosity support is swelling and disintegration of ODTs, due to the penetration of water into the hydrophilic tablet matrix by capillary action which generates pressure for fast and complete disintegration of the tablets. So, microcrystalline cellulose acts as auxiliary tablet disintegrant because of its high water absorption capacity [32].

The disintegration time and wetting time of DCT orodispersible tablet of zolmitriptan were compared to F11. The results showed that F11 had significantly (p<0.05) lower WT and DT compared to DCT formula table (4). This is due to that solubilization of the drug in the nonvolatile liquid by liquidosil technique results in enhancing the wettability of the formulation (F11) compared to the DCT orodispersible tablet of zolmitriptan [33]. From the result shown in table (4), it can be concluded that formula F11 complies with USP specification of the disintegration time which is less than 30 s [28].

The liquidosil ODTs of zolmitriptan F11 was the best formula among all the formulas of the liquidosil ODTs tablets; in terms of rapid in vitro disintegration and acceptable tablet properties. The dissolution of the zolmitriptan from formula F11 was compared to the DCT of zolmitriptan as in fig. (4). From the data in table (5), it was found that F11 showed significant (p<0.05) faster dissolution compared to DCT of zolmitriptan, this attributed to the fact that zolmitriptan is already in solution form in PG, at the same time, it is hold by the powder particles (Avicel PH-102 and Aerosil 200). When the drug within the liquidosil system is completely dissolved in the liquid vehicle, it is located in the powder substrate still in a solubilized state. The accelerated release in zolmitriptan liquidosil ODTs (F11) is due to its markedly increased wettability and surface area available to the dissolution medium [34].

Fig. 3: The process of disintegration time test for F3 with 7.5% CSS as super disintegrant: (A) beginning (B) at 30th s and (C) at 60th s
Compatibility studies

FT-IR of zolmitriptan showed three main characteristic absorption bands of strong absorbance at 1738 cm$^{-1}$ due to C = O stretching vibrations of amino ester functional group OCONHR, N-H stretching band of secondary and tertiary amine appears at 3350 cm$^{-1}$ as a single sharp band and C-O (stretching) of ester group at 1252 cm$^{-1}$ [22] as in fig. (5). It was noted that the peaks of major functional groups of zolmitriptan, which are present in the spectrum of pure drug, were present in zolmitriptan liquisolid formula fig. (6) (C = O stretching vibrations and C-O stretching of ester group except N-H stretching of pure drug at 3350 cm$^{-1}$ was overshadow with OH stretching of Avicel PH-102 this due to the amount of the drug is too low compared to Avicel PH-102 (the ratio of the drug Avicel PH-102 was 1:80 in the selected formula F18, also might be attributed to the formation of hydrogen bonding between the drug and liquid vehicle; this indicated lack the possibility of interaction between zolmitriptan and polymers used in the preparation of the liquisolid orodispersible tablets.

Accelerated stability study (effect of humidity)

Stability studies of the selected formula (F11) showed no significant difference (p>0.05) in tablet hardness, % friability, drug content, disintegration time, wetting time and release profile after storage at 40±2 °C/75±5% RH for the duration of four months.
CONCLUSION

The orodispersible tablets of zolmitriptan were prepared by liquisolid technique method using different super disintegrants such as CP, SSG, and CSS. Among all super disintegrant, a formulation containing CP as a super disintegrant is fulfilling all the parameters satisfactorily compared to another super disintegrant. The relative efficiency of this super disintegrant to improve the disintegration time in order of CP>SSG>CSS. In vitro release studies revealed that almost 95.2% drug was released from the formulation were within 2 min. The physicochemical properties and stability of the prepared liquisolid tablets were satisfactory. This study indicates the possibility of using the selected best formula (F11) in the preparation of zolmitriptan ODTs for oral administration because of desired properties of the prepared tablets concerning sufficient hardness, low friability, fast disintegration and dissolution.

CONFLICT OF INTERESTS

Declared none

REFERENCES


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