ABSTRACT

Objective: The objective of this study was to formulate and evaluate the poorly soluble drug, azilsartan medoxomil into nanosuspension to increase the solubility and enhance the dissolution rate and then improve its bioavailability.

Methods: Nanosuspension of azilsartan medoxomil was prepared using solvent-antisolvent precipitation method using PVP-K30 as a stabilizer. Eight formulations were prepared to show the effect of different parameters in which four formulations show the effect of stabilizer concentration, three formulations show the effect of stirring speed and two formulations prepare to show the effect of the addition of co-stabilizer such as sodium lauryl sulphate (SLS) and tween 80. All these formulation are evaluated for their particle size and entrapment efficiency. The selected one was evaluated for zeta potential, scanning electron microscope (SEM), saturation solubility, and in vitro drug release.

Results: All the prepared formulations were in the nano size. The optimum concentration of the stabilizer was in the formulation when the drug: stabilizer ratio 1:1 and optimum stirring speed was 300 rpm. Dramatic effect on the particle size reduction was found by the addition of co-stabilizer (SLS) in formulation F3 that has P. S 157±0.0 nm. The selected formula F3 showed an enhanced dissolution profile compared to the pure drug at all-time intervals.

Conclusion: The results show that the formulation that contain drug: PVP-K30: SLS in ratio 1:0.75:0.25 is the best one and can be utilized to formulate azilsartan medoxomil nanosuspension.

Keywords: Azilsartan medoxomil, Solubility, Bioavailability

INTRODUCTION

Drug solubility refers to the maximum amount of solute dissolved in the solvent under the specific condition of temperature, pressure and pH. It has been known that solubility, dissolution and gastrointestinal permeability are important parameters that control its bioavailability [1]. The water solubility of a drug plays an important role in the absorption of the drug after oral administration. It is also useful in manipulating and testing of drug properties during the drug design and development process. It is critically important when the dissolution time is limited [2]

There are several formulation approaches are available to solve the problems of low aqueous solubility and increase the dissolution rate of hydrophobic drugs. Some of the conventional approaches are micronization, use of penetration enhancer or co-solvents, surfactant dispersion method, salt formation, etc., but the major problems of these techniques are limited advantages in solubility enhancement for poorly soluble drugs. Also precipitation, toxicity and altered pharmacological activity are another disadvantages of the conventional strategies [3-5].

Other additional approaches are vesicular systems like liposomes, dispersion of solids, emulsion and micro emulsion methods, and complexes with cyclodextrins; these methods show the beneficial effect as drug delivery system but they are not applicable to all the drugs molecules which consider the major problem to all these techniques [6].

Nanotechnology can be used as an alternative method to enhance drug solubility and solve the problems associated with various approaches of the conventional methods described earlier [7, 8]. A pharmaceutical nanosuspension is biphasic systems consisting of Nano sized drug particles stabilised by surfactants for either oral and topical use or parenteral and pulmonary administration. This technology is used for poorly soluble drugs that are insoluble in both water and oils. Particle size distribution in nanosuspensions is usually less than one micron with an ideal average particle size ranging between 200 and 600 nm [9].

Nanosuspensions are considered to be the best dosage form in the formulation of BCS class-II drugs since this technology results in the formulation that is having high dissolution velocity and increased saturation solubility [10]. Other advantages of nanosuspension are that it can be easy fabrication into a tablet or a capsule or dried nanosuspension form which can easily be redispersible [11].

Azilsartan medoxomil is [(5-methyl-2-oxo-1, 3-dioxol-4-yl) methyl 2-ethoxy-1-\{2’-(5-oxo-4,5-dihydro-1,2,4-oxadiazol-3-y) biphenyl-4-yl\}[methyl]-1'H-benzimidazol-7-carboxylate] with a molecular weight of 568.5 g/mol. Fig. (1) Shows the chemical structure of azilsartan medoxomil [12].

Fig. 1: Chemical structure of azilsartan medoxomil [12]

Azilsartan medoxomil appear like a white crystalline powder which is practically insoluble in water, freely soluble in methanol, soluble
in acetic acid, slightly soluble in acetone and acetonitrile while it is very slightly soluble in 1-octanol. Azilsartan medoxomil has melting point 212-214°C, pKa 6.1 and log P 5.70. It is more lipophilic than candisartan [13, 14].

Azilsartan medoxomil (AZL-M) is a prodrug that it is rapidly hydrolyzed to the active metabolite, azilsartan, during the gastrointestinal absorption phase. It is a selective AT1 subtype angiotensin II receptor blocker (ARB) and is indicated for the treatment of mild to moderate essential hypertension [15]. Azilsartan reach its peak plasma concentration in about 1.5 to 3 h after oral administration, with bioavailability from 50-55%, the non-absorbable drug leads to diarrhea and gastric disturbances. It has a half-life of approximately 11 h and volume of distribution is 16L [16].

The starting dose in adults is 40 mg taken orally once daily and this may be increased to 80 mg once daily when it is required [17]. AZL-M has shown pharmaceutical problems of water solubility. Because it is practically insoluble in water, the dissolution of AZL-M from its available dosage form after oral administration which is an important factor for its bioavailability is usually the rate-limiting step in the absorption process [18].

The aim of present study is to the formulation of azilsartan medoxomil as nanosuspension in order to improve its solubility and enhance in vitro dissolution rate.

**MATERIALS AND METHODS**

**Materials**

Azilsartan medoxomil (99 % pure) was purchased from Hangzhou Hyper Chemical Limited, China. Sodium lauryl sulfate (SLS) was purchased from S. D Fine-Chem limited Mumbai, India. Poly vinyl pyrrolidone k-30 was provided by Hangzhou Sunflower Technology Development Co., Ltd, China. All other chemicals and solvents were of analytical reagent grade, and deionized water also was used in this study.

**Method**

**Determination of λmax**

Ten milligrams of azilsartan medoxomil was dispersed in 100 ml 0.1N HCl pH 1.2 to prepare 0.1 mg/ml stock solution. From this stock solution, a dilute (10 μg/ml) solution was prepared and scanned by UV spectrophotometer at the range of 200-400 nm. The same steps were repeated with phosphate buffer pH 6.8, water and methanol to obtain the λ max of azilsartan medoxomel in these medium [19].

**Preparation of calibration curves**

Calibration curves of azilsartan medoxomil in 0.1 N HCl, phosphate buffer pH 6.8, water and methanol were constructed by preparing serial dilutions of the drug from 0.1 mg/ml stock solution for each medium. The prepared samples were analyzed spectrophotometrically at λ max in these media. The plot of absorbance vs. concentration is done and beer's range was determined [20]. The results were analyzed in triplicate and standard division was represented.

**Determination of saturation solubility of azilsartan medoxomil**

Saturation solubility of azilsartan medoxomil was determined in (water, methanol, 0.1N HCl, pH 1.2 and phosphate buffer (pH 7.4 and 6.8 solution). Excess amount of azilsartan medoxomil was added to 10 ml of each media and kept in an incubator shaker at 25±0.5 °C and after 48 h, solution was centrifuged at 5000 rpm for 15 min.

**Preparation of azilsartan medoxomil nanosuspension by precipitation method**

Nanosuspension precipitation method is used to prepare oral nanosuspension of azilsartan medoxomil using different concentration of stabilizer and co-stabilizer. In brief, 40 mg of azilsartan medoxomil was dissolved in an organic solvent (3 ml methanol). Deionized water containing stabilizer (PVP K30) alone in different concentration or in combination with co-stabilizer (tween 80 or SLS), which acts as the antisolvent system. This was followed by the addition of the organic solution into the antisolvent solution at a very slow rate (1 ml/min) by the help of a syringe pump, under mechanical agitation of different speeds using homo disperser. Then transfer to hot plate magnetic stirrer (Stuart U. K) for 60 min at 50±1 °C to allow organic solvent to evaporate and get the desired nanosuspension [23]. The batches were prepared according to the formulation design (table 1).

<table>
<thead>
<tr>
<th>Substance</th>
<th>F1</th>
<th>F2</th>
<th>F3</th>
<th>F4</th>
<th>F5</th>
<th>F6</th>
<th>F7</th>
<th>F8</th>
</tr>
</thead>
<tbody>
<tr>
<td>AZL-M (mg)</td>
<td>40</td>
<td>40</td>
<td>40</td>
<td>40</td>
<td>40</td>
<td>40</td>
<td>40</td>
<td>40</td>
</tr>
<tr>
<td>PVP-K30 (mg)</td>
<td>20</td>
<td>30</td>
<td>30</td>
<td>30</td>
<td>30</td>
<td>40</td>
<td>40</td>
<td>60</td>
</tr>
<tr>
<td>SLS (mg)</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
</tr>
<tr>
<td>Tween 80 (ml)</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
<td>-</td>
</tr>
<tr>
<td>Methanol (ml)</td>
<td>3 ml</td>
<td>3 ml</td>
<td>3 ml</td>
<td>3 ml</td>
<td>3 ml</td>
<td>3 ml</td>
<td>3 ml</td>
<td>3 ml</td>
</tr>
<tr>
<td>Water (ml)</td>
<td>40 ml</td>
<td>40 ml</td>
<td>40 ml</td>
<td>40 ml</td>
<td>40 ml</td>
<td>40 ml</td>
<td>40 ml</td>
<td>40 ml</td>
</tr>
<tr>
<td>Stirring speed (rpm)</td>
<td>3500</td>
<td>3500</td>
<td>3500</td>
<td>3500</td>
<td>3500</td>
<td>3500</td>
<td>3500</td>
<td>3500</td>
</tr>
</tbody>
</table>

**Lyophilization of selected nanosuspension**

The selected formulation of the prepared azilsartan medoxomil nanosuspension was lyophilized (vacuum freeze dryer, Labconco, USA) using mannitol as a cryoprotectant (1:5 ratio-total solid content: Mannitol). Briefly, (five times the quantity of total solid content in nanosuspension). The nanosuspension was then kept in the freezer for a suitable time. Afterwards, the frozen nanosuspension was directly placed in the freeze dryer chamber and allowed to be lyophilized over 48 h at 20°C and 0.03 mbar pressure [24].

**Preparation of nanosuspension**

**Particle size and size distribution**

Particle size determination was done by using Nano Brook 90Plus particle size analyzer (Brookhaven instruments. USA) which is a dynamic light scattering, works by measuring the intensity of light scattered by the molecules in the sample as a function of time, at scattering angle 90° and a constant temperature of 25°C. The Nano Brook 90Plus particle size analyzer provides different choices. The important one is the determination of an average diameter (Eff. Dia.) and a measure of the polydispersity which are sufficient for many applications [25].

**Determination of entrapment efficiency (EE) of nanosuspension**

10 ml of nanosuspension was centrifuged at 5000 rpm for 20 min. The supernatant solution was filtered and separated. 1 ml of this filtrate was diluted with water and the absorbance at maximum λ max was measured by UV spectrophotometer using water as blank [26]. The amount of free drug in the formulations was measured and the entrapment efficiency is then calculated from Eq.1

\[
E.E\% = \frac{(Total\ drug\ in\ formula-free\ drug)\times100}{Total\ drug\ in\ formula} \quad (1)
\]
The results were analyzed in triplicate and standard deviations are reported.

**Zeta potential**

Zeta potential of the selected formulation of azilsartan medoxomil nanosuspension was measured using The Nano Brook 90Plus zeta seizer (Brookhaven Instruments USA). Before analysis, the samples were diluted 10 times with solvent. A zeta potential value of ±30mV is required as a minimum for physically stable nanosuspension stabilised by electrostatic repulsion only. While zeta potential of about ±20 mV is sufficient to stabilise the nanosuspension system stabilized by a combination of steric and electrostatic stabilisation [27, 28].

**In vitro dissolution profile of nanosuspension**

In vitro drug release for nanosuspension was done by dialysis bag method using himedia dialysis membrane (MWCO 12 KD). Volume containing 40 mg of azilsartan medoxomil of optimized formulations of nanosuspension was placed in pretreated dialysis bag and drug release was done using USP dissolution apparatus II containing 900 ml of dissolution medium at 37 ± 0.5°C. The speed of the paddle was 100 rpm. The optimized formulation of azilsartan medoxomil nanosuspension was subjected to the drug release studies in both media of 0.1N HCl (pH 1.2) and phosphate buffer (pH 6.8) in comparison with pure drug. Samples (5 ml) were withdrawn at regular intervals of 10 min for 90 min and replaced with fresh dissolution medium. Samples were filtered and assayed spectrophotometrically on UV spectrophotometer at 248 nm wavelength. For each formulation, the experiment was repeated in triplicate [26, 29].

**Scanning electron microscopy (SEM)**

The pure drug powder of azilsartan medoxomil was confirmed by direct deposition of powder as thin film on double-sided carbon tape, while SEM for the liquid of the selected formulation of the prepared nanosuspension was confirmed by the droplet evaporation technique and photographs were taken at different magnification [10]. A droplet of liquid was deposited on a double-sided carbon tape and dried at room temperature using a Vega/TESCAN scanning electron microscope operated with a secondary detector at different acceleration voltage and at different magnification [30].

**X-ray powder diffraction (XRPD)**

Powder X-ray diffraction can be used to confirm the crystalline nature of materials. So, this information is used to verify whether the substances are crystalline or amorphous. The diffractograms of azilsartan medoxomil and lyophilized powders of the selected formulation were obtained for analysis. The study was confirmed by using Shimadzu XRD-6000 powder X-ray diffractometer at continuous scan range of 10-80 degree. The operating voltage was 40 (kV) and current 30mA [31, 32].

**Fourier transforms infrared spectroscopy (FTIR)**

The FTIR spectra of pure azilsartan and lyophilized powder of the selected formula were obtained using FTIR spectrophotometer (FTIR-8300 Shimadzu, Japan) by potassium bromide (KBr) pellet method. This study was achieved to identify any sign of interaction between the drug and stabiliser used. The spectrum obtained was in between the wave number of 4000-400 cm⁻¹ [33].

**Statistical analysis**

The results were expressed as mean ± SD and were analysed statistically by one-way analysis of variance (ANOVA) using Graph Pad Prism V5.04 software (San Diego, CA, USA) at level of (p<0.05).

**RESULTS AND DISCUSSION**

**Determination of λ Max**

The analysis of UV spectra of azilsartan medoxomil in HCL buffer pH 1.2 and phosphate buffer (pH 6.8) in comparison with pure drug. Samples (5 ml) were withdrawn at regular intervals of 10 min for 90 min and replaced with fresh dissolution medium. Samples were filtered and assayed spectrophotometrically on UV spectrophotometer at 248 nm wavelength. For each formulation, the experiment was repeated in triplicate [34, 35].

**Calibration curves of azilsartan medoxomil**

The constructed calibration curves of azilsartan medoxomil in methanol, water, HCl buffer pH 1.2 with 0.5% Tween80, and Phosphate buffer pH 6.8 shows the same λmax 248 nm while it was 250 nm in methanol which similar to the published one as shown in fig. 2 [34, 35].

**Saturation solubility of azilsartan medoxomil**

The poor solubility of azilsartan medoxomil that determined is in agreement with published researches as shown in table 2, also the results shows that an increase in pH resulted in an increase in the solubility of azilsartan medoxomil as showing in the figure; this is because it is an acidic drug (pKa = 6.1).

**Table 2: Saturation solubility of azilsartan medoxomel in different media**

<table>
<thead>
<tr>
<th>Solvent</th>
<th>PH 1.2</th>
<th>PH 6.8</th>
<th>PH 7.4</th>
<th>Water</th>
</tr>
</thead>
<tbody>
<tr>
<td>Solubility(µg/ml) mean±SD*</td>
<td>20.305±0.11</td>
<td>374±0.5</td>
<td>1033±1.2</td>
<td>16.1±0.1</td>
</tr>
</tbody>
</table>

*SD standard deviation from mean, n=3
Particle size analysis and polydispersity index measurement
The effect of different parameters on the particle size and polydispersity index was studied using eight different formulations. All the prepared formulations were in the Nano size. The mean particle size (effective diameter) for formulations varied in the narrow range from 157±0.0 nm to 610.6±0.0 nm.

The particle size and PDI for different formulations of different parameters is showing in table 3.

Table 3: The particle size, PDI, free drug and % entrapment efficiency (E. E %) of different formulations

<table>
<thead>
<tr>
<th>Formula no.</th>
<th>Stabilizer</th>
<th>Drug:stabilizer:co-stabilizer ratio</th>
<th>Stirring speed</th>
<th>P. S±SD*</th>
<th>PDI</th>
<th>E. E%±SD*</th>
</tr>
</thead>
<tbody>
<tr>
<td>F1</td>
<td>PVP K30</td>
<td>1:0.5</td>
<td>3500</td>
<td>470.5±0.0</td>
<td>0.252</td>
<td>83±0.14</td>
</tr>
<tr>
<td>F2</td>
<td>PVP K30</td>
<td>1:0.75</td>
<td>3500</td>
<td>421.2±0.0</td>
<td>0.005</td>
<td>83.19±0.1</td>
</tr>
<tr>
<td>F3</td>
<td>PVPK30:0.75:SLS</td>
<td>1:0.75:0.25</td>
<td>3500</td>
<td>157±0.0</td>
<td>0.005</td>
<td>95.8±0.2</td>
</tr>
<tr>
<td>F4</td>
<td>PVPK30:0.75:SLS</td>
<td>1:0.75:0.25</td>
<td>3500</td>
<td>190.8±0.0</td>
<td>0.005</td>
<td>97.1±0.2</td>
</tr>
<tr>
<td>F5</td>
<td>PVP K30</td>
<td>1:1</td>
<td>3500</td>
<td>324.3±0.0</td>
<td>0.233</td>
<td>88.25±0.1</td>
</tr>
<tr>
<td>F6</td>
<td>PVP K30</td>
<td>1:1</td>
<td>1200</td>
<td>317.3±0.0</td>
<td>0.005</td>
<td>90.75±0.3</td>
</tr>
<tr>
<td>F7</td>
<td>PVP K30</td>
<td>1:1.5</td>
<td>300</td>
<td>293.1±0.0</td>
<td>0.315</td>
<td>90.97±0.1</td>
</tr>
<tr>
<td>F8</td>
<td>PVP K30</td>
<td>1:1.5</td>
<td>3500</td>
<td>610.6±0.0</td>
<td>0.182</td>
<td>91.37±0.2</td>
</tr>
</tbody>
</table>

*SD standard deviation, n=3

Effect of stabilizer concentration on the particle size and polydispersity index
Four formulations were used to show this effect F1, F2, F5 and F8. The optimum concentration was in the formulation of F5 which has particle size 324.2±0.0 nm. Also these formulation show PDI in the range of 0.05-0.252 and this low value will indicate good stability of the nanosuspension. The effect of the drug to stabilizer ratio show in the fig. 5. The choice of suitable stabilizers and its concentration are the most important factors to control the size and stability of the nanosuspension during nanoprecipitation methods [36, 37].
In our work; PVP-K30 was used at different concentration (table 1). The results showed that particle size is reduced with the increasing of stabilizer concentration as the particle size of formula F1 which contains 1:0.5 of drug: pvp-k30 ratio was 470.5±0.0 nm compared with 324.3±0.0 nm for F5 which contains 1:1 ratio of drug: stabilizer. The reason behind this is that high stabilizer concentration decreases surface tension and stabilizes newly developed surfaces during precipitation process and produce nanosuspension of smaller particles size [38]. Also, low or insufficient concentration of stabilizer will cause instability and recrystallization [39]. This could be attributed to the increase in the molar substitution ratio (MSR) of the polymer per drug. The increase of the hydrophilic corona surrounding the polymer to protect the nanoparticles enhances the stability and prevents particles from aggregation [40, 41].

On the other hand, the particle size increased with the high concentration of PVP-K30 which might be due to the higher viscosity of the resulting solution that might hinder particle movement during stirring as in formulation F8 which has particle size of 610.6±0.0 nm. The polydispersity index (PI) values were ranged from 0.05-0.356 which indicates acceptable uniformity level for all the prepared formulations [42]. Narrower range of particles size will minimizes the difference between active agent concentration and the surrounding environment. As a result, the Ostwald ripening phenomenon will be inhibited [43].

**Effect of stirring speed on the particle size and polydispersity index of prepared nanosuspension**

Three different speeds 3500, 1200 and 300 rpm were used to prepare three formulations F5-F7 to show this effect. In this study the optimum speed at a drug to stabilizer ratio 1:1 was found to be 300 rpm that produce mean particle size 293.1±0.0 nm. PDI of these formulations was in the range of 0.233-0.315. This effect is shown in fig. 6.

**Effect of addition co-stabilizer on particle size and polydispersity index**

Two different stabilizers (SLS and Tween 80) in the ratio of drug: stabilizer: co-stabilizer 1:0.75:0.25 in formulations F3 and F4 were used to show this effect. The effect of SLS was more prominent than the effect of tween 80 on particle size in this study which produce nanosuspension of particle size 157 nm as compared with formulation F2 without co-stabilizer 421.2 and F4 that contain tween 80 of 190.8 nm. Usually, a combination of homopolymer (PVP-K30) with ionic surfactant (SLS) is required to provide repelling forces and concomitant maintenance of particle stabilization and crystallization balance [44]. This effect is shown in figure 7. These findings are in accordance with Kumar et al. who had lower particle sizes and better stability when stabilized the formulation with surfactant mixtures compared with formulations with only one surfactant [45].

It could be inferred from the results that there was a significant impact of the drug to polymer ratio, stirring speed and addition of co-stabilizer on the mean particle size of the drug loaded nanosuspensions and PDI. The addition of the surfactant on the particle size and PDI will be the formula no F3 which has the lowest mean particle size (157.0±0.0 nm) and this formula is selected for lyophilization and further study. The mean particle sizes of the F3 formulation and their size distribution graph was shown in fig. 8.

**Drug entrapment efficiency**

The Percentage drug entrapment efficiency of all the formulations was calculated and the results were tabulated in table (3). The drug entrapment efficiency of F3 and F4 was high when compared to other formulations. This may be due to the presence of optimum polymer and optimum tween 80 and SLS concentrations, comparing the formulations F1, F2, F5 and F6, it is clear that increase in polymer concentration increased the drug entrapment efficiency. Fig. 9 show the drug entrapment efficiency of a different formulation of azilsartan medoxomil nanosuspension. The concentration of stabilizer used are the most effective factor on entrapment efficiency and this agree with that obtained by Patil et al. who formulate spry dried chitosan nanoparticles containing doxorubicin [46].

**Zeta potential**

The zeta potential for the selected formulation of azilsartan medoxomil nanosuspension was -127.17 mV as shown in fig. 10. The charge was negative due to adsorbed SDS and PVP-k30 on the drug particles; however the high zeta potential proposes that the nanosuspension was adequately stabilized. It reflects the electrical potential of particles and is influenced by the composition of the particle and the medium in which it is dispersed. Zeta potential gives certain information about the surface charge properties and further the long-term physical stability of the nanosuspensions. The obtained value for selected formulation indicates stable nanosuspension [47].

**Saturation solubility of freeze drying nanosuspension**

The batch F3 (AZL-M: PVP-K30: SLS 1:0.75:0.25) was selected for freeze drying since it had the small particle size and lowest polydispersity index. Using mannitol as the cryoprotectant resulted in the formation of a white spongy, cotton-like material upon lyophilization. Mannitol containing samples showed good redispersibility upon manual shaking. The saturation solubility of the lyophilized powder of the selected formula F3 was increased significantly. It increases to 11±0.2 folds in pH 1.2 and to 21±0.4 folds in pH 6.8
Fig. 8: particle size distribution of the selected formula (F3)

Fig. 9: Drug entrapment efficiency of the prepared formulation of azilsartan medoxomil nanosuspension (Results are expressed as mean, n=3)

Fig. 10: Zeta potential of the selected formula (F3)
In vitro drug release

In vitro drug release profiles of AZL-M pure drug, nanosuspension of selected formula (F3) are shown in fig. 11. The release of AZL-M from the nanosuspension of selected formulation was higher than the release profile of pure drug in 90 min. The %CDR of the selected formula F3 was more than 80% in less than 30 min in both 0.1N HCl and phosphate buffer pH 6.8 media as compare to less than 14% and 28% of pure drug in the same media respectively. This will indicate that the dissolution rate of the prepared nanosuspension is enhanced. Factors contributing to a fast release were large surface area due to small particle size, high diffusion coefficient (small molecular size), low matrix viscosity and short diffusion distance of the drug [45].

Scanning electron microscope

The SEM of pure azilsartan medoxomil is presented in fig. (12) at 100x and 500x magnification. The particles of azilsartan were large in size (from 50-350um) and has irregular shape and when the picture is closer at 500x and more of magnification it would illustrate the rough surface of azilsartan particles while the images of the SEM at different magnification for that of the selected formula of the nanosuspension (F3) is represent in fig. (13) and it indicate uniform submicron sized particles and results also show nearly spherical shaped nanoparticles and a size within the nano size and this micrograph was in agreement with those measured by particle size distribution [48].

Powder X-ray diffraction analysis (PXRD)

PXRD patterns of azilsartan medoxomil as a pure drug showed sharp diffraction peaks in the fig. (14) and this indicate the crystalline nature of the pure azilsartan medoxomil. azilsartan medoxomil show intense crystalline peaks at 2θ from 13 ° to 27 °, and the strongest three peaks were 23 °, 21 ° and 20 °. However, these characteristic peaks disappeared in the pattern of lyophilized powder of the selected formulations (F3) as seen in fig. (15) Producing a diffused pattern of very low intensity peaks and shifting to a lower degree and we characterized by the complete absence of any diffraction peak corresponding to crystalline azilsartan medoxomil. These results provide that the azilsartan medoxomil in the lyophilized powder is in an amorphous state [49].

Fourier transforms infrared spectroscopy (FTIR)

The FTIR spectra of pure azilsartan medoxomil is shown in fig. 16 and that of the lyophilized powder of the selected formula (F3) is shown in fig. 17. FTIR spectra of AZL-M nanosuspension show no change in shifting of the position of the major functional groups and this will indicate there is no major interaction between the drug and the stabilizer PVP K-30 and other excipients (SLS) used in the formulation [50].

![Fig. 12: SEM of pure azilsartan medoxomil A): 100X B): 500X](image)
Fig. 13: SEM of selected formula F3 A): 1kx B): 10kx

Fig. 14: PXRD of pure azilsartan medoxomil

Fig. 15: PXRD of the selected formula F3
CONCLUSION

It may be concluded from the results of this study that nanosuspensions of poorly soluble drug azilsartan medoxomil can be prepared using solvent antisolvent precipitation method and using PVP K30, Tween 80, and SLS as stabilizers. The process parameters, such as stabilizer concentration, stirring speed and combination of other stabilizer were investigated and optimized to produce the smallest drug nanoparticles. The dissolution rate of the nanosuspension significantly enhance as compare with the pure drug.

ACKNOWLEDGEMENT

We are very thankful to the presidency of nanotechnology and advance material center in the university of technology, Iraq; for providing necessary facilities utilized in carrying out parts of the work.

CONFLICT OF INTERESTS

Declared none

REFERENCES


Kesessoglou F, Amitava M. Crystalline nanosuspensions as potential toxicity and clinical oral formulations for BCS II/IV compounds. AAPS J 2012; 14:677-87.


How to cite this article